

Irregular Stimulus Timing: Analysis with 3dDeconvolve

- 3dDeconvolve is set up to calculate response functions $h(t)$ when stimuli occur locked to image acquisition TR interval
 - ◇ The -stim_nptr option allows stimuli to occur at intervals of TR/p , where p is a small integer
 - ◇ But it seems like there is no way to do deconvolution for a completely irregular stimulus pattern
- The key is to write the response function $h(t)$ as a linear sum of a small number of basis functions, and then use 3dDeconvolve to calculate (and test) the weighting factors in this sum:

$$h(t) = \sum_{a=0}^{N_a} \lambda_a \cdot \psi_a(t)$$

where each $\psi_a(t)$ is a fixed function and the unknown amplitudes λ_a are to be determined from data

- ◇ Must choose the $\psi_a(t)$ basis functions based on the duration and shape of response you expect

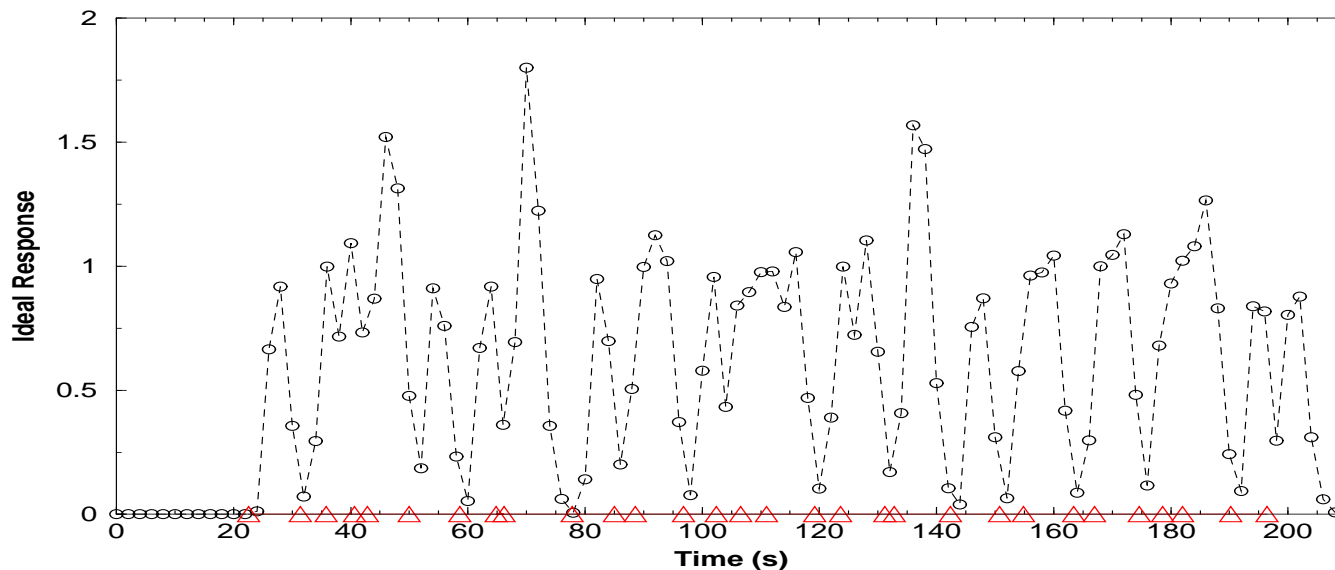
- Simulating a time series:

- ◇ `waver -dt 2.0 -GAM -peak 1 -tstim 'cat tstim.1D' > ideal.1D`

- ◇ File tstim.1D (30 stimulus times, averaging about 6 s apart):

22.6 31.4 35.8 40.6 42.8 50.0 58.6 66.2 64.8 77.8 85.0 88.6 96.8 102.4 106.6 111.0
119.2 123.6 131.2 132.8 142.4 150.8 154.8 163.4 167.0 174.6 178.6 182.0 190.2 196.4

- ◇ Graph of response ideal.1D (circles/dashed lines) with triangles \triangle at tstim.1D stimulus times, for 106 volumes to be simulated at TR=2 s:



- ◇ Despite appearances, this is without noise: fluctuations are just from different overlaps of gamma variate hemodynamic response, since stimuli are not evenly spaced in time
 - ◇ Goal of analysis is to retrieve hemodynamic response function (including amplitude) in each voxel, and test whether it is significantly different from zero

- Generate a simulated dataset with this ideal response time series in every voxel (with varying amplitude), a baseline, and some noise (with varying standard deviation):

- ◇ Make a 1 slice dataset from something handy, just to use as a template:

```
3dZcutup -prefix zcut -keep 10 10 epi07+orig
```

- ◇ Calculate a dataset with this geometry ($64 \times 64 \times 1$) with the ideal.1D function intensity and noise variance varying in 8×8 blocks across the image:

```
3dcalc -a 'zcut+orig[0]' \  
        -b ideal.1D          \  
        -datum float         \  
        -prefix sim:time     \  
        -expr '100+(int(i/8)+1)*0.25*b+int(j/8)*0.25*gran(0,1)'
```

↪ 3dcalc is a voxel-by-voxel dataset calculator program

↪ -a 'zcut+orig[0]' means to read in the #0 sub-brick of this dataset and call its voxel values by the symbol a

↪ -b ideal.1D means to read in this time series file and call its values by the symbol b (since this has no spatial dimension, each spatial voxel from b at a given time index will have the same value, unlike from a)

▷ Since the -a dataset doesn't have a time axis, the -b time series will be used to provide a time axis in the output of 106 points (same length as ideal.1D)

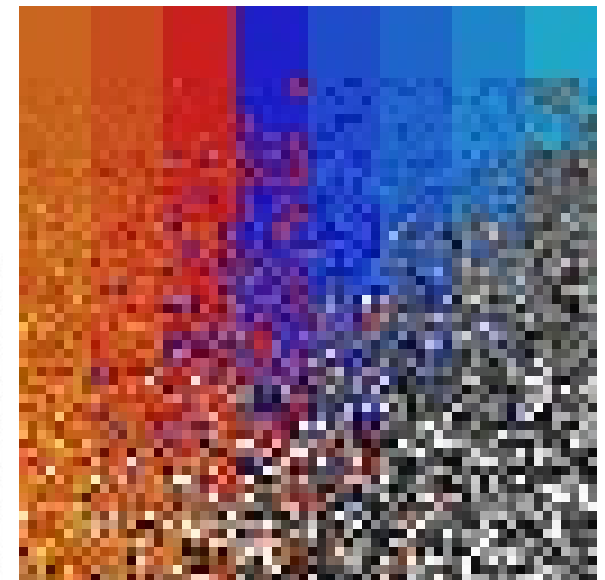
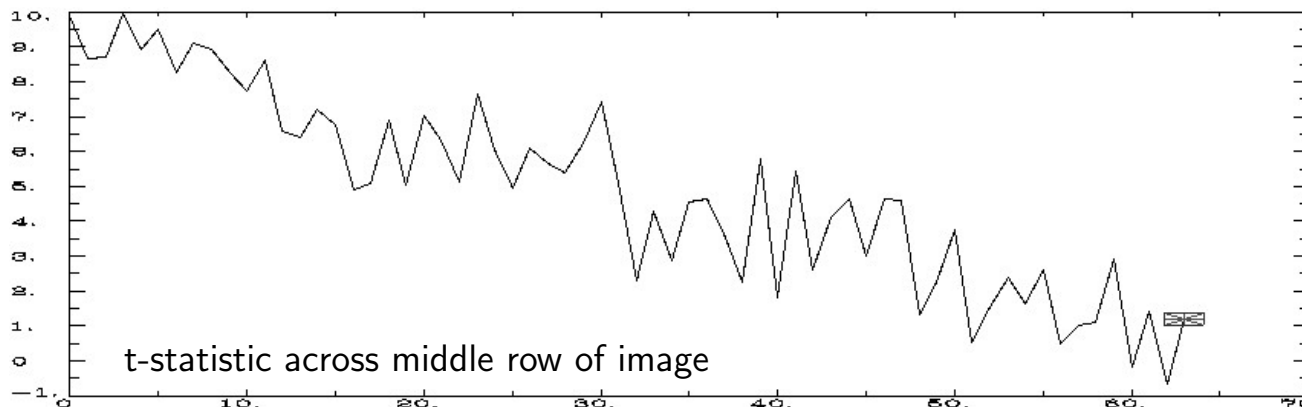
- ↪ -datum float means to write the output dataset in floating point format (don't need to deal with scaling issues then)
- ↪ -prefix sim:time is the prefix part of the output dataset filename
- ↪ -expr '100+(int(i/8)+1)*0.25*b+int(j/8)*0.25*gran(0,1)' is the mathematical expression that determines the output at each voxel
 - ▷ Symbols b, i, j are used
 - ▷ Dataset a was only read in to act as a template for the output dataset (i.e., to set up its spatial axes and dimensions)
 - ▷ Since there was no -i or -j option, 3dcalc assigns the x-axis voxel index to the symbol i (range=0..63) and the y-axis voxel index to the symbol j (range=0..63)
 - ▷ 100 is the baseline
 - ▷ (int(i/8)+1) ranges 1..8 across image horizontally, in blocks 8 voxels wide
 - (int(i/8)+1)*0.25*b gives signal from 0.25 to 2 times b
 - ▷ int(j/8) ranges 0..7 across image vertically, in blocks 8 voxels wide
 - int(j/8)*0.25*gran(0,1) gives noise increasing down image, in blocks
 - gran(0,1)=Gaussian deviate with mean=0, standard deviation=1
- ◇ Result is spatially square 3D+time dataset with varying amounts of signal and noise that we can use for testing

◇ Simple regression analysis with 3dDeconvolve:

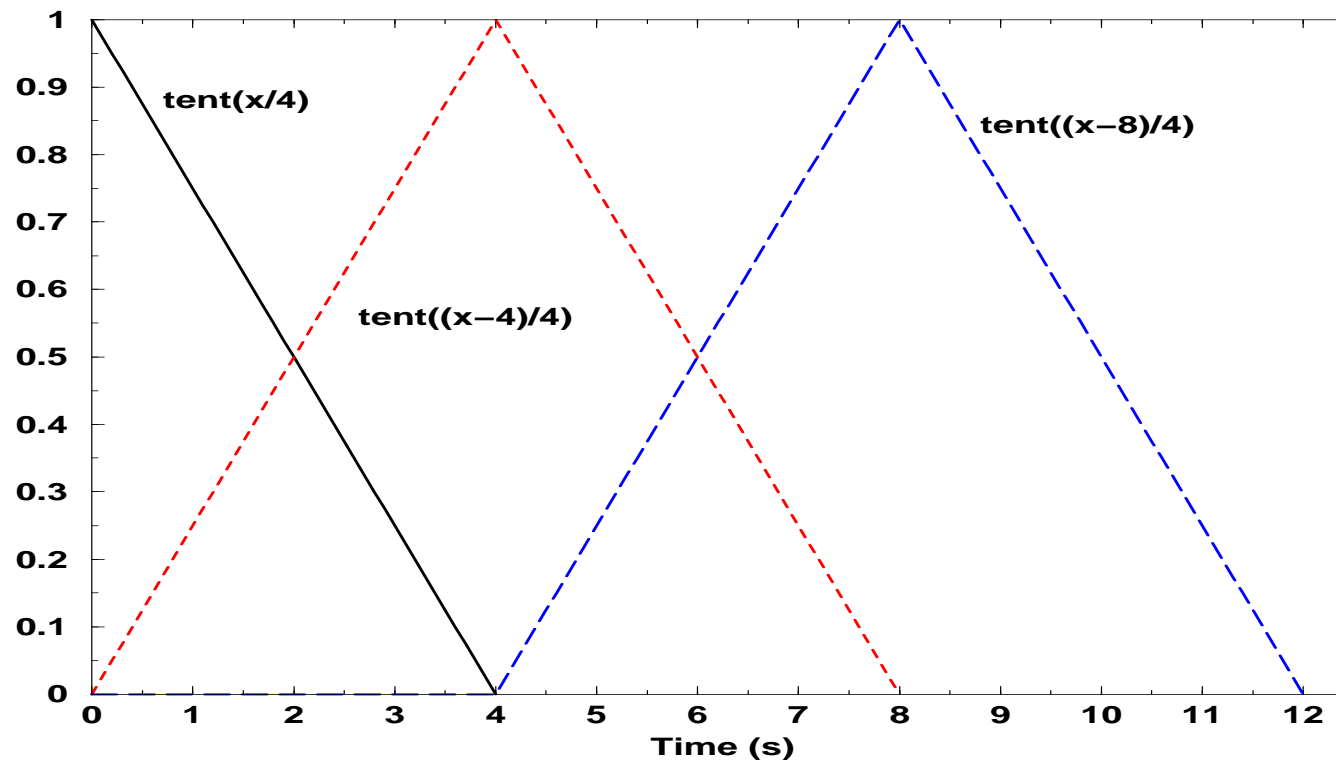
```
3dDeconvolve -input sim:time+orig \
             -num_stimts 1 \
             -stim_file 1 ideal.1D \
             -stim_label 1 Response \
             -stim_minlag 1 0 -stim_maxlag 1 0 \
             -fitts sim_regress_fitts \
             -tout -bucket sim_regress_stats \
```

↪ In AFNI:

- Set Function→Func to sub-brick #4 Response[0] Coef
- Set Function→Thr to sub-brick #5 Response[0] t-tstat
- Set Function→** to 1; slider to $p \approx 1.0 \cdot 10^{-4}$ ($t \approx 4$)
- Set Function→Pos ON; pbar # to 11
- Set Datamode→Misc→Voxel Coords ON
- Turn on See Function, open Axial Image
- Noise increases downwards; signal leftwards



- However, our goal is deconvolution analysis, not simple regression
 - ◇ Assume hemodynamic response to individual stimulus lasts no more than 12 s (depends on type of stimulus)
 - ↪ Actual waver -GAM function is significant only from 2..10 s post-stimulus
 - ◇ Model it as the sum of 3 “tent” functions:



↪
$$\text{tent}(x) = \begin{cases} 1 - |x| & \text{if } -1 < x < 1 \\ 0 & \text{if } |x| \geq 1 \end{cases}$$

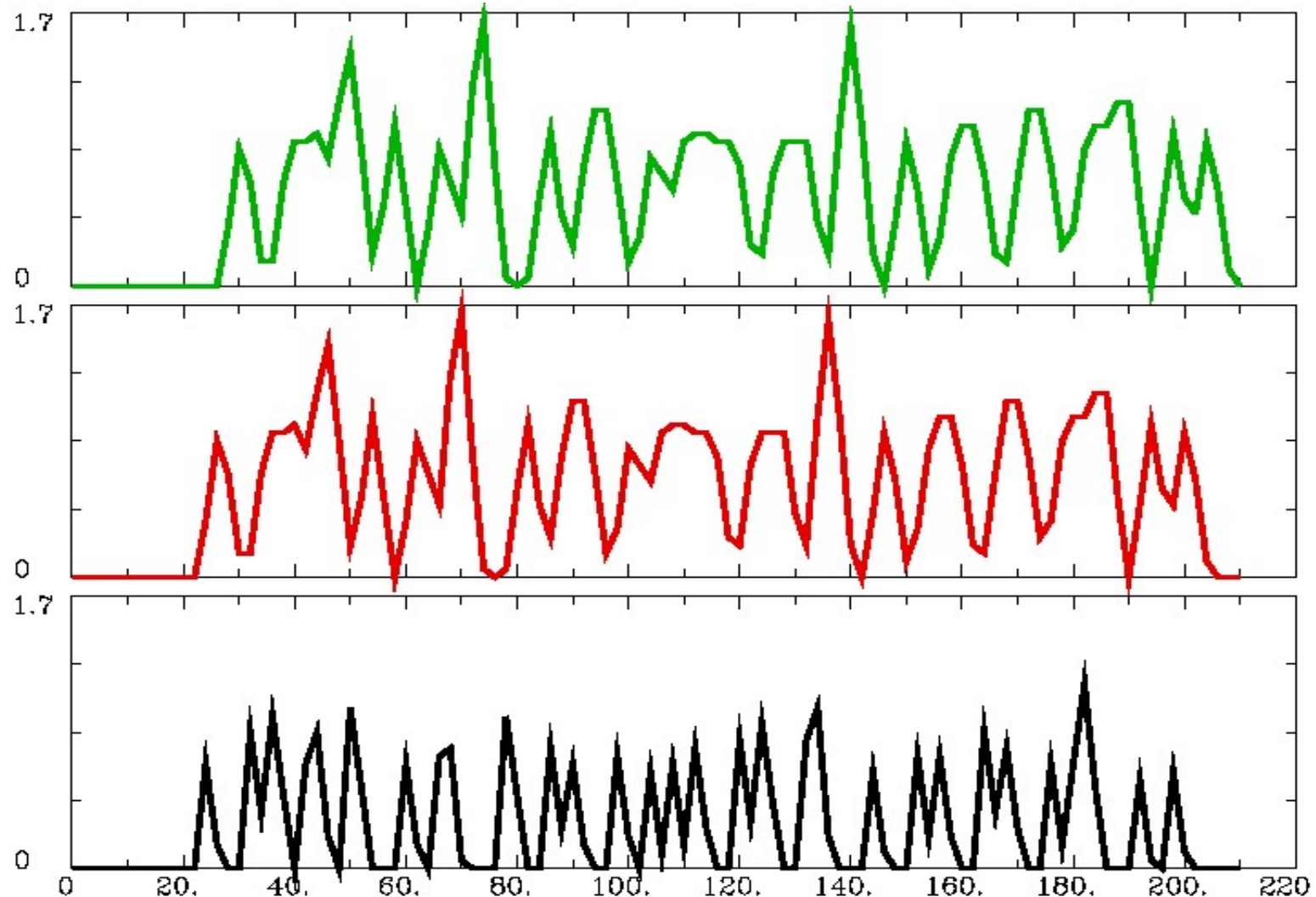
↪ Built in function in 3dcalc, waver, etc.

- ◇ We generate response time series for each of the 3 basis functions $\text{tent}(t/4)$, $\text{tent}((t-4)/4)$, and $\text{tent}((t-8)/8)$:

```
waver -dt 2.0 -EXPR 'tent(t/4)' -peak 1 -tstim 'cat tstim.1D' > tent0.1D
```

```
waver -dt 2.0 -EXPR 'tent((t-4)/4)' -peak 1 -tstim 'cat tstim.1D' > tent4.1D
```

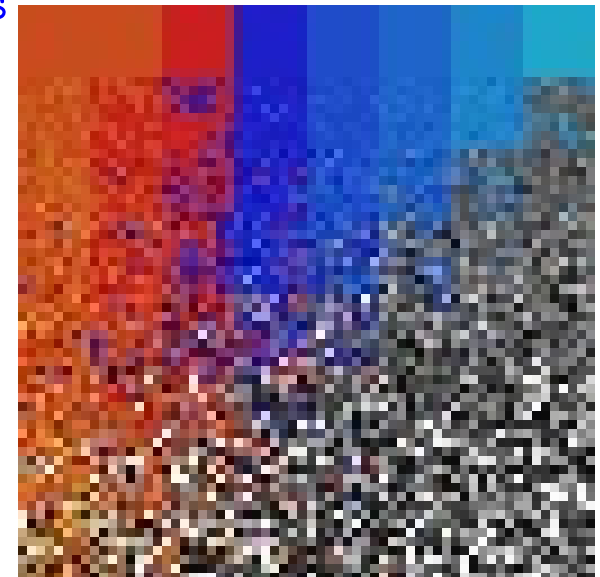
```
waver -dt 2.0 -EXPR 'tent((t-8)/4)' -peak 1 -tstim 'cat tstim.1D' > tent8.1D
```



◇ Then we run 3dDeconvolve with these 3 regressors:

```
3dDeconvolve -input sim:time+orig.HEAD \
             -num_stimts 3 \
             -stim_file 1 tent0.1D \
             -stim_file 2 tent4.1D \
             -stim_file 3 tent8.1D \
             -stim_label 1 tent0 \
             -stim_label 2 tent4 \
             -stim_label 3 tent8 \
             -stim_minlag 1 0 -stim_maxlag 1 0 \
             -stim_minlag 2 0 -stim_maxlag 2 0 \
             -stim_minlag 3 0 -stim_maxlag 3 0 \
             -fitts sim_decon_fitts \
             -fout -bucket sim_decon_stats
```

- Function→Func = #4 tent4[0] Coef
- Function→Thr = #8 Full F-stat
- Function→** = 1; slider $p \approx 1.0-4$ ($F \approx 7.8$)
- Function→Pos ON; # = 11



- ◇ To calculate hemodynamic response function in each voxel, need to combine basis functions with amplitudes from output dataset sim_decon_stats+orig:

```
3dcalc -a 'sim_decon_stats+orig[2]' \
      -b 'sim_decon_stats+orig[4]' \
      -c 'sim_decon_stats+orig[6]' \
      -d 121junk.1D \
      -dt 0.1 \
      -datum float \
      -prefix sim:hrf_fit \
      -expr 'a*tent(t/4)+b*tent((t-4)/4)+c*tent((t-8)/4)'  
3drefit -epan sim:hrf_fit+orig
```

- ↪ Symbols a, b, c are for 3D (no time) volumes
 - ↪ -d 121junk.1D is just to input a time series of length 121 points (contents don't matter, since symbol d isn't using in expression)
 - ↪ -dt 0.1 sets TR for manufactured 3D+time dataset to 0.1 s
 - ↪ Symbol t is time in -expr
 - ↪ 3drefit command is to make output an Anat type dataset (so can graph it in AFNI)
- ◇ Also make a 1D file with the true gamma deviate hemodynamic response function, for comparison: waver -GAM -dt 0.1 > gamma.1D

◇ In AFNI:

- ↪ Switch Anatomy to sim:hrf_fit; open Axial Graph
- ↪ FIM→Pick Ideal and choose gamma.1D timeseries
- ↪ Opt→Colors, Etc.→Ideal: Use Thick Lines ON
- ↪ Opt→Colors, Etc.→Grid color to lt-blue2 (say)
- ↪ Opt→Baseline→Global ON; Opt→Baseline→Set Global to -1
- ↪ Press h key to get horizontal line at $y=0$; press a to autoscale

