
FMRI Connectivity Analysis in AFNI

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Structure of this lecture

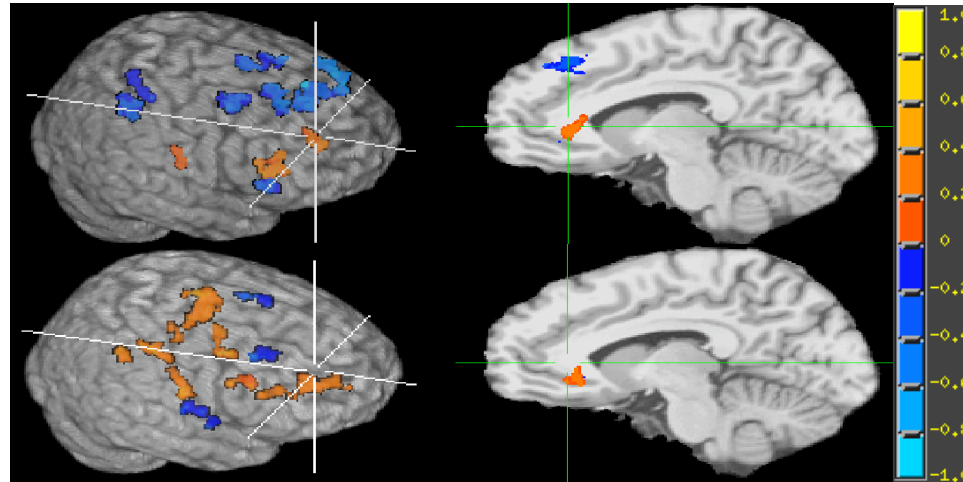
- Overview
- Correlation analysis
 - Simple correlation
 - Context-dependent correlation (PPI)
- Structural equation modeling (SEM)
 - Model validation
 - Model search
- Granger causality (GC)
 - Bivariate: exploratory - ROI search
 - Multivariate: validating – path strength among pre-selected ROIs

Overview: fMRI connectivity analysis

- All about fMRI
 - Not for DTI
 - Some methodologies may work for MEG, EEG-ERP
- Information we have
 - Anatomical structures
 - Exploratory: A seed region in a network, or
 - Validating: A network with all relevant regions known
 - Brain output (BOLD signal): regional time series
- What can we say about inter-regional communications?
 - Inverse problem: make inference about intra-cerebral neural processes from extra-cerebral/vascular signal
 - Based on response similarity (and sequence)

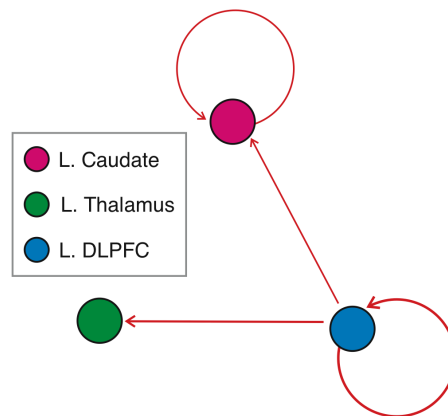
Approach I: seed-based; ROI search

- Regions involved in a network are unknown
 - Bi-regional/seed vs. whole brain (**3d***): brain volume as input
 - Mainly for ROI search
 - Popular name: functional connectivity
 - Basic, coarse, exploratory with **weak assumptions**
 - Methodologies: simple correlation, PPI, bivariate GC
 - **Weak interpretation**: may or may not indicate directionality /causality



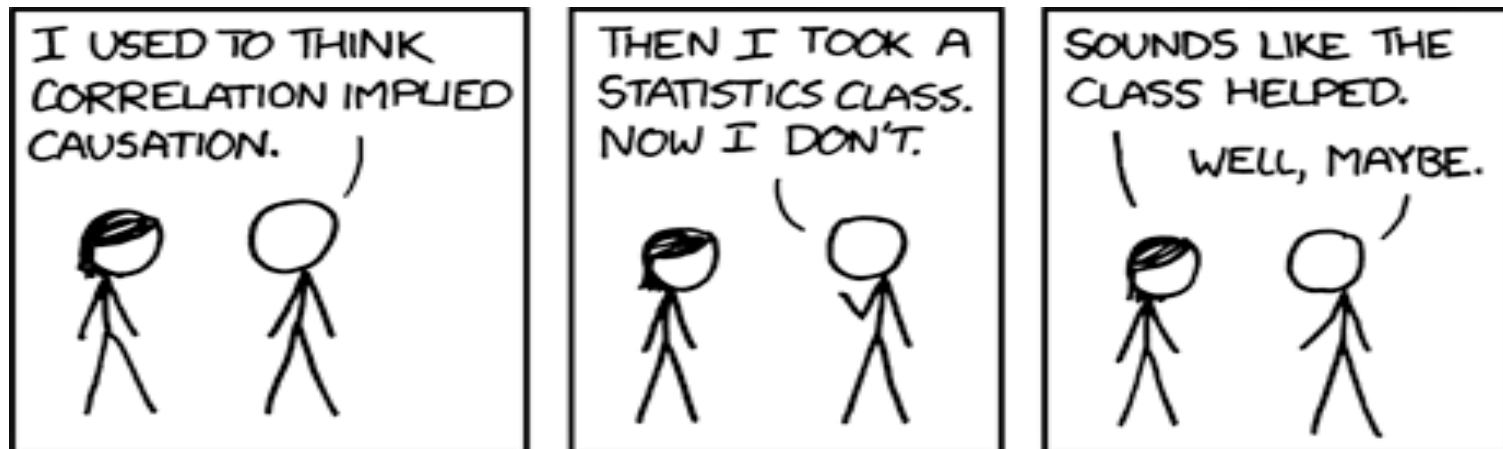
Approach II: ROI-based

- Regions in a network are known
 - Multi-regional (**1d***): ROI data as input
 - Model validation, connectivity strength testing
 - Popular name: effective or structural connectivity
 - Strong assumptions: specific, but with high risk
 - Methodologies: SEM, multivariate GC, DCM
 - Directionality, causality (?)



Interpretation Trap: Correlation vs. Causation!

- Some analyses require fine time resolution we usually lack
- Path from (or correlation btw) A to (and) B doesn't necessarily mean causation
 - Bi-regional approach simply ignores the possibility of other regions involved
 - Analysis invalid if a relevant region is missing in a multi-regional model
- Robust: connectivity analysis < regression analysis
- Determinism in academics and in life
 - Linguistic determinism: Sapir-Whorf hypothesis



Preparatory Steps

- Warp brain to standard space
 - **adwarp**, **@auto-tlrc**, **align_epi_anat.py**
- Create ROI
 - Sphere around a peak activation voxel: **3dUndump -master ... -srad ...**
 - Activation cluster-based (biased unless from independent data): localizer
 - Anatomical database
 - Manual drawing
- Extract ROI time series
 - Average over ROI: **3dmaskave -mask**, or **3dROIstats -mask**
 - Principal component among voxels within ROI: **3dmaskdump**, then **1dsvd**
 - Seed voxel with peak activation: **3dmaskdump -noijk -dbox**
- Remove effects of no interest
 - **3dSynthesize** and **3dcalc**
 - **3dDetrend -polort**
 - **RETROICORR/RetroTS.m**
 - **3dBandpass**

Simple Correlation Analysis

- Seed vs. rest of brain
- ROI search based on response similarity
 - Looking for regions with similar signal to seed
- **Correlation** at individual subject level
 - Usually have to control for effects of no interest: drift, head motion, physiological variables, censored time points, tasks of no interest, etc.
- Applying to experiment types
 - Straightforward for resting state experiment
 - With tasks: correlation under specific condition(s) or resting state?
- Program: **3dfim+** or **3dDeconvolve**
 - r : not general, but **linear**, relation; slope for standardized Y and X
 - β : slope, amount of **linear** change in Y when X increases by 1 unit
- Two interactive tools: AFNI and SUMA
 - InstaCor, GroupInstaCor

Simple Correlation Analysis

■ Group analysis

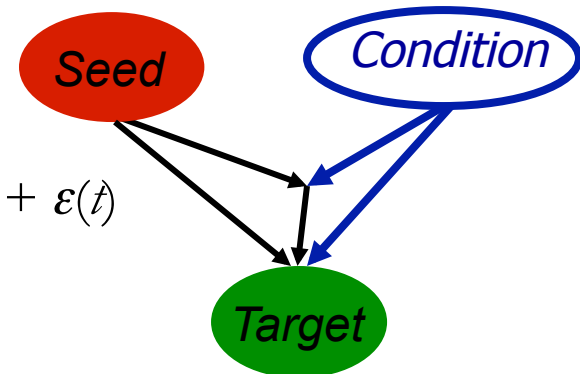
- Run Fisher-transformation of r to Z -score and t -test: **3dtttest**
- Take β and run t -test (pseudo random-effects analysis): **3dtttest**
- Take $\beta + t$ -statistic and run random-effects model: **3dMEMA**

■ **Caution:** don't over-interpret

- Not proof for anatomical connectivity
- **No golden standard procedure** and so many versions in analysis: seed region selection, covariates, $r(Z)/\beta$, bandpass filtering, ...
- Just Pearson correlation (information limited if other regions present in network)
- Be careful with group comparison (normal vs. disease): assuming within-group homogeneity, can we claim
 - No between-group difference → same correlation/connectivity across groups?
 - Between-group difference → different correlation/connectivity across groups?

Context-Dependent Correlation

- Popularized name: Psycho-Physiological Interaction (PPI)
- 3 explanatory variables
 - Condition (or contrast) effect: $C(t)$
 - Seed effect on rest of brain: $S(t)$
 - Interaction between seed and condition (or contrast): $I(C(t), S(t))$
 - **Directionality** here!
- Model for each subject
 - Original GLM: $y = [C(t) \text{ Others}] \beta + \varepsilon(t)$
 - New model: $y = [C(t) S(t) I(C(t), S(t)) \text{ Others}] \beta + \varepsilon(t)$
 - 2 more regressors than original model
 - **Others** NOT included in SPM
 - What we care for: r or β for $I(C(t), S(t))$



Context-Dependent Correlation

- How to formulate $I(C(t), S(t))$?
 - BOLD signal is an indirect measure of brain activity: Interaction occurs at neuronal, not BOLD, level
 - **Deconvolution**: derive “neuronal response” at seed based on BOLD response with **3dTfitter**
 - Impulse convolved with Neuronal events = BOLD response
 - A difficult and an inaccurate process!
 - Deconvolution matters more for event-related than block experiments
- Group analysis
 - Run Fisher-transformation of r to Z -score and t -test: **3dttest**
 - Take β and run t -test (pseudo random-effects analysis): **3dttest**
 - Take β and t -statistic and run random-effects model: **3dMEMA**

PPI Caution: avoid over-interpretation

- Not proof for anatomical connectivity
- Just Pearson correlation (interpretation weakened if other regions involved in the network)
- Neuronal response is hard to decode: Deconvolution is very far from reliable, plus we have to assume a shape-fixed HRF (same shape regardless of condition or regions in the brain)
- Doesn't say anything about interaction between seed and target on seed
- Doesn't differentiate whether modulation is
 - Condition on neuronal connectivity from seed to target, or
 - Neuronal connectivity from seed to target on condition effect
- Be careful with group comparison (normal vs. disease group): assuming within-group homogeneity, can we claim
 - No between-group difference => same correlation/connectivity across groups?
 - Between-group difference => different correlation/connectivity across groups?

Context-Dependent Correlation: hands-on

■ Data

- ❑ Downloaded from <http://www.fil.ion.ucl.ac.uk/spm/data/attention/>
- ❑ Event-related attention to visual motion experiment
- ❑ 4 conditions: fixation, stationary, attention motion (att), no attention motion (natt)
- ❑ TR=3.22s, 360 time points = 90 TR's/run × 4 runs, seed ROI = V2
- ❑ All steps coded in commands.txt: `tcsch -x commands.txt` (~5 minutes)

■ Should effects of no interest be included in PPI model?

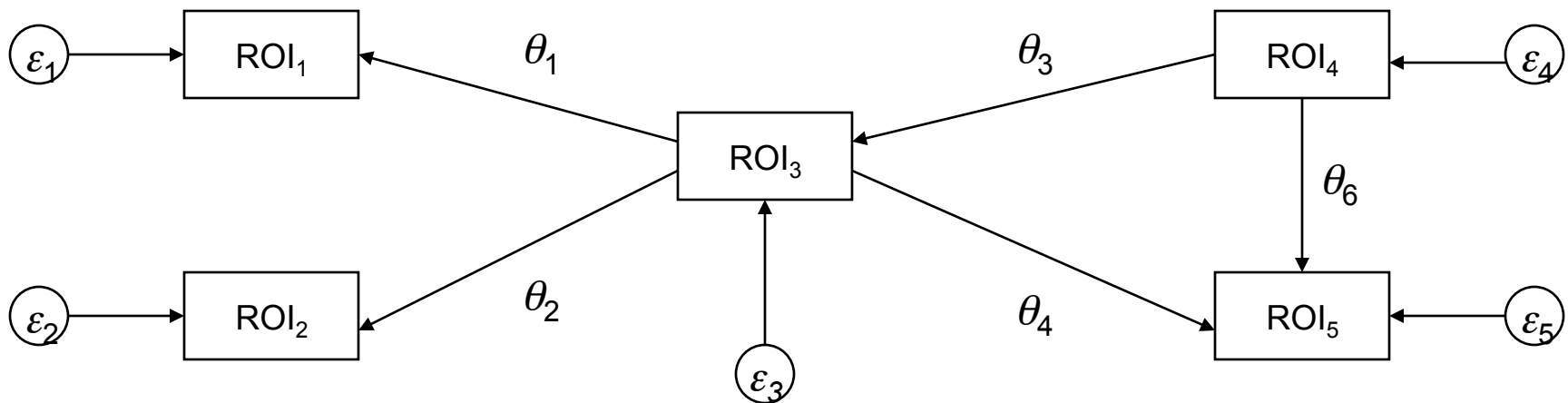
- ❑ Compare results between AFNI and SPM

■ If stimulus was presented in a resolution finer than TR

- ❑ Use **1dUpsample n** to interpolate ROI time series *n* times finer before deconvolution with **3dTffiter**
- ❑ Then downsample interaction regressor back to original resolution with **1dcat** + selector '{0..\$(n)}'

Structural Equation Modeling (SEM) or Path Analysis

- All possible regions involved in network are included
- All regions are treated equally as endogenous (dependent) variable
- Residuals (unexplained) are exogenous (independent) variables
- Analysis based on summarized data (not original ROI times series) with **model specification**, **covariance/correlation matrix**, **DF** and residual error variances (?) as input



SEM: theory

- Hypothetical model $X = KX + \varepsilon$
 - X : i -th row $x_i(t)$ is i -th ROI time series
 - K : matrix of path coefficients θ 's whose diagonals are all 0's
 - ε : i -th row $\varepsilon_i(t)$ is residual time series of i -th ROI

- Predicted (theoretical) covariance

$$\Sigma(\theta) = (I - K)^{-1} E[\varepsilon(t)\varepsilon(t)^T] [(I - K)^{-1}]^T \text{ as } X = (I - K)^{-1} \varepsilon$$

- ML discrepancy/cost/objective function btw predicted and estimated covariance (P : # of ROIs)

$$F(\theta) = \ln |\Sigma(\theta)| + \text{tr}[C\Sigma^{-1}(\theta)] - \ln |C| - P$$

- Input: model specification; covariance (correlation?) matrix C ; DF (calculating model fit statistic chi-square); residual error variances?
- Usually we're interested in a network under resting state or specific condition

SEM: 1st approach - validation

- Knowing directional connectivity btw ROIs, data support model?
- Null hypothesis H_0 : It's a good model
- If H_0 is **not** rejected, what are the path strengths, plus fit indices?
- Analysis for whole network, path strength estimates by-product
- 2 programs
 - **1dSEM** in C
 - Residual error variances as input (DF was a big concern due to limited number of time points)
 - Group level only; no CI and p value for path strength
 - Based on Bullmore *et al.*, How Good is Good Enough in Path Analysis of fMRI Data? NeuroImage 11, 289-301 (2000)
 - **1dSEMr . R** in R
 - Residual error variances not used as input
 - CI and p value for path strength
 - Individual and group level

SEM: 2nd approach - search

- All possible ROIs known with some or all paths are uncertain
- Estimate unknown path strengths
- Start with a minimum model (can be empty)
- Grow (add) one path at a time that lowers cost
- How to add a path?
 - **Tree growth**: branching out from previous generation
 - **Forest growth**: whatever lowers the cost – no inheritance
- Program **1dSEM**: only at group level
- Various fit indices other than cost and chi-square:
 - AIC (Akaike's information criterion)
 - RMSEA (root mean square error of approximation)
 - CFI (comparative fit index)
 - GFI (goodness fit index)

SEM: caution I

- **Correlation or covariance:** What's the big deal?
 - Almost **ALL** publications in fMRI use correlation as input
 - A path connecting from region A to B with strength θ
 - Not correlation coefficient
 - If A increases by one SD from its mean, B would be expected to increase by θ units (or decrease if θ is negative) of its own SD from its own mean while holding all other relevant regional connections constant.
 - With correlation as input
 - May end up with different connection and/or path sign
 - **Results are not interpretable**
 - Difficult to compare path strength across models/groups/studies,...
 - **Scale ROI time series to 1** (instead of 100 as usual)
- ROI selection very important
 - If one ROI is left out, whole analysis (and interpretation) would be invalid

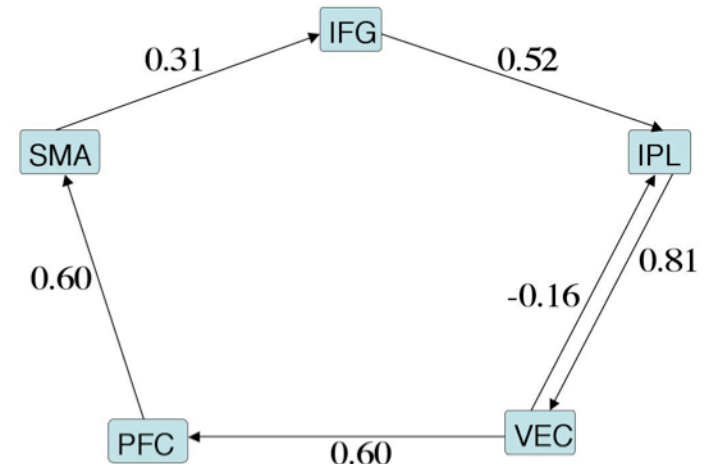
SEM: caution II

- Validation
 - It's **validation**, not proof, when not rejecting null hypothesis
 - Different network might be equally valid, or even with lower cost: model comparison possible if nested
- Search: How much faith can we put into final 'optimal' model?
 - Model comparison only meaningful when nested (tree > forest?)
 - Is cost everything considering noisy fMRI data? (forest > tree?)
 - Fundamentally SEM is about validation, not discovery
- Only model regional relationship at current moment
 - $X = KX + \epsilon$
 - No time delays

SEM: hands-on

■ Model validation

- ❑ Data: Bullmore *et al.* (2000)
- ❑ Correlation as input
- ❑ Residual error variances as input
- ❑ **SEMscript.csh** maybe useful
- ❑ **1dSEM**: `tssh -x commands.txt`
- ❑ **1dSEMr.R**: sequential mode



■ Model search

- ❑ Data courtesy: Ruben Alvarez (MAP/NIMH/NIH)
- ❑ 6 ROIs: PHC, HIP, AMG, OFC, SAC, INS
- ❑ Tree growth
- ❑ Covariance as input for **1dSEM**
- ❑ Shell script **SEMscript.csh** taking subject ROI time series and minimum model as input: `tssh -x commands.txt` (~10 minutes)

Granger Causality: introduction

- Classical univariate autoregressive model $AR(p)$
 - $y(t) = \alpha_0 + \alpha_1 y(t-1) + \dots + \alpha_p y(t-p) + \varepsilon(t) = \alpha_0 + \sum_{k=1}^p \alpha_k y(t-k) + \varepsilon(t)$, $\varepsilon(t)$ white
 - Current state depends linearly on immediate past ones with a random error
 - Why called autoregressive?
 - Special multiple regression model (on past p values)
 - Dependent and independent variable are the same
 - $AR(1)$: $y(t) = \alpha_0 + \alpha_1 y(t-1) + \varepsilon(t)$
- What we typically deal with in GLM
 - $y = X\beta + \varepsilon$, $\varepsilon \sim N(0, \sigma^2 V)$, σ^2 varies spatially (across voxels)
 - Difficulty: V has some structure (*e.g.*, $ARMA(1,1)$ in 3dREMLfit) and may vary spatially
 - We handle autocorrelation structure in noise ε
 - Sometimes called time series regression

Rationale for Causality in FMRI

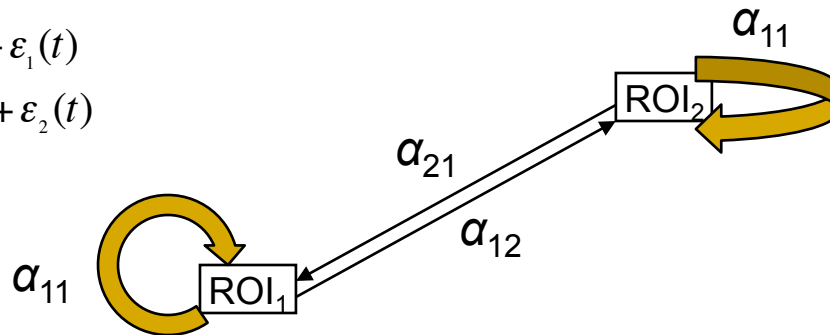
- Networks in brain should leave some signature (*e.g.*, latency) in fine texture of BOLD signal because of dynamic interaction among ROIs
- Response to stimuli does not occur simultaneously across brain: latency
- Reverse engineering: signature may reveal network structure
- **Problem:** latency might be due to neurovascular differences!

Start simple: bivariate AR model

- Granger causality: A Granger causes B if
 - time series at A provides **statistically significant** information about another at B at some time delays (order)
- 2 ROI time series, $y_1(t)$ and $y_2(t)$, with a VAR(1) model

$$y_1(t) = \alpha_{10} + \alpha_{11}y_1(t-1) + \alpha_{12}y_2(t-1) + \varepsilon_1(t)$$

$$y_2(t) = \alpha_{20} + \alpha_{21}y_1(t-1) + \alpha_{22}y_2(t-1) + \varepsilon_2(t)$$



Assumptions

- Linearity
 - Stationarity/invariance: mean, variance, and autocovariance
 - White noise, positive definite contemporaneous covariance matrix, and no serial correlation in individual residual time series
- Matrix form: $Y(t) = \alpha + AY(t-1) + \varepsilon(t)$, where

$$Y(t) = \begin{bmatrix} y_1(t) \\ y_2(t) \end{bmatrix} \quad \alpha = \begin{bmatrix} \alpha_{10} \\ \alpha_{20} \end{bmatrix} \quad A = \begin{bmatrix} \alpha_{11} & \alpha_{12} \\ \alpha_{21} & \alpha_{22} \end{bmatrix} \quad \varepsilon(t) = \begin{bmatrix} \varepsilon_1(t) \\ \varepsilon_2(t) \end{bmatrix}$$

Multivariate AR model

- n ROI time series, $y_1(t), \dots, y_n(t)$, with VAR(p) model

$$y_1(t) = \alpha_{10} + \sum_{k=1}^p \alpha_{11k} y_1(t-k) + \dots + \sum_{k=1}^p \alpha_{1nk} y_n(t-k) + \varepsilon_1(t)$$

⋮

$$y_n(t) = \alpha_{n0} + \sum_{k=1}^p \alpha_{n1k} y_1(t-k) + \dots + \sum_{k=1}^p \alpha_{nnk} y_n(t-k) + \varepsilon_n(t)$$

- Hide ROIs: $Y(t) = \alpha + A_1 Y(t-1) + \dots + A_p Y(t-p) + \varepsilon(t)$,

$$Y(t) = \alpha + \sum_{i=1}^p A_i Y(t-i) + \varepsilon(t) \quad \alpha = \begin{bmatrix} \alpha_{10} \\ \vdots \\ \alpha_{n0} \end{bmatrix} \quad Y(t) = \begin{bmatrix} y_1(t) \\ \vdots \\ y_n(t) \end{bmatrix} \quad A_i = \begin{bmatrix} \alpha_{11i} & \cdots & \alpha_{1ni} \\ \vdots & \ddots & \vdots \\ \alpha_{n1i} & \cdots & \alpha_{nli} \end{bmatrix} \quad \varepsilon(t) = \begin{bmatrix} \varepsilon_1(t) \\ \vdots \\ \varepsilon_n(t) \end{bmatrix}$$

VAR: convenient forms

- Matrix form (hide ROIs) $Y(t) = \alpha + A_1 Y(t-1) + \dots + A_p Y(t-p) + \varepsilon(t)$
- Nice VAR(1) form (hide ROIs and lags): $Z(t) = \mathbf{v} + BZ(t-1) + u(t)$

$$Z(t) = \begin{bmatrix} Y(t) \\ Y(t-1) \\ \vdots \\ Y(t-p+1) \end{bmatrix} \quad \mathbf{v} = \begin{bmatrix} \alpha \\ 0 \\ \vdots \\ 0 \end{bmatrix} \quad B = \begin{bmatrix} A_1 & \dots & A_{p-1} & A_p \\ I_n & \dots & 0 & 0 \\ \vdots & \ddots & \vdots & \vdots \\ 0 & \dots & I_n & 0 \end{bmatrix} \quad u(t) = \begin{bmatrix} \varepsilon(t) \\ 0 \\ \vdots \\ 0 \end{bmatrix}$$

- Even neater form (hide ROIs, lags and time): $Y = BZ + U$

$$Y = [Y(p+1), \dots, Y(T)], \quad B = [\alpha, A_1, \dots, A_p], \quad U = [\varepsilon(p+1), \dots, \varepsilon(T)],$$

$$Z = \begin{bmatrix} 1 & 1 & \dots & 1 \\ Y(p) & Y(p+1) & \dots & Y(T-1) \\ \vdots & \vdots & \vdots & \vdots \\ Y(1) & Y(2) & \dots & Y(T-p) \end{bmatrix}$$

- Solve it with OLS:

$$\hat{B} = YZ^+ = YZ'(ZZ')^{-1}$$

VAR extended with covariates

- **Standard VAR(p)** $Y(t) = \alpha + A_1 Y(t-1) + \dots + A_p Y(t-p) + \epsilon(t)$

- Covariates are all over the place!

- Trend, tasks/conditions of no interest, head motion, time breaks (due to multiple runs), censored time points, physiological noises, etc.

- **Extended VAR(p)**

$$Y(t) = \alpha + A_1 Y(t-1) + \dots + A_p Y(t-p) + BZ_1(t) + \dots + B_q Z_q(t) + \epsilon(t),$$

where Z_1, \dots, Z_q are covariates

- Endogenous (dependent: ROI time series)
- Exogenous (independent: covariates) variables
- Path strength significance: t -statistic (F in BrainVoyager)

Model quality check

- Order selection: 4 criteria (1st two tend to overestimate)
 - AIC: Akaike Information Criterion
 - FPE: Final Prediction Error
 - HQ: Hannan-Quinn
 - SC: Schwartz Criterion
- Stationarity: VAR(p) $Y(t) = \alpha + A_1 Y(t-1) + \dots + A_p Y(t-p) + \epsilon(t)$
 - Check characteristic polynomial $\det(I_n - A_1 z - \dots - A_p z^p) \neq 0$ for $|z| \leq 1$
- Residuals normality test
 - Gaussian process: Jarque-Bera test (dependent on variable order)
 - Skewness (symmetric or tilted?)
 - Kurtosis (leptokurtic or spread-out?)

Model quality check (continued)

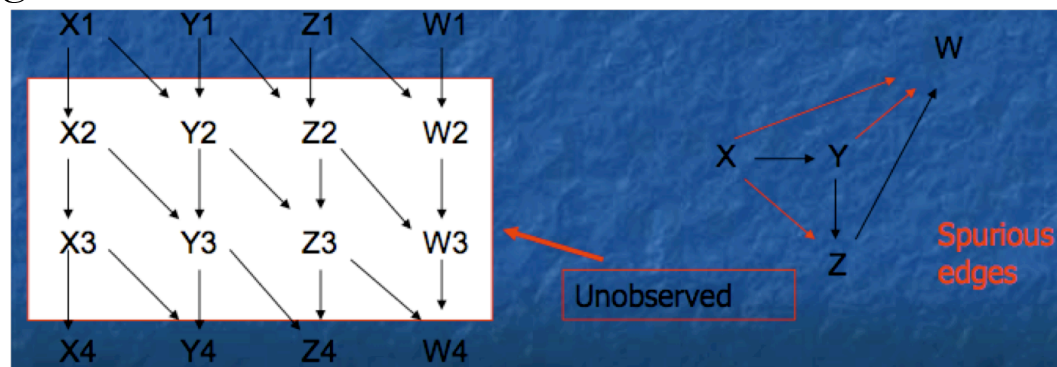
- Residual autocorrelation
 - Portmanteau test (asymptotic and adjusted)
 - Breusch-Godfrey LM test
 - Edgerton-Shukur F test
- Autoregressive conditional heteroskedasticity (ARCH)
 - Time-varying volatility
- Structural stability/stationarity detection
 - Is there any structural change in the data?
 - Based on residuals or path coefficients

GC applied to fMRI

- Resting state
 - Ideal situation: no cut and paste involved
 - Physiological data maybe essential?
- Block experiments
 - Duration ≥ 5 seconds?
 - Extraction via cut and paste
 - Important especially when handling confounding effects
 - Tricky: where to cut especially when blocks not well-separated?
- Event-related design
 - With rapid event-related, might not need to cut and paste (at least impractical)
 - Other tasks/conditions as confounding effects

GC: caveats

- Assumptions (stationarity, linearity, Gaussian residuals, no serial correlations in residuals, etc.)
- Accurate ROI selection
- Sensitive to lags
- Interpretation of path coefficient: slope, like classical regression
- Confounding latency due to vascular effects
- **No transitive relationship:** If $Y_3(t)$ Granger causes $Y_2(t)$, and $Y_2(t)$ Granger causes $Y_1(t)$, it does not necessarily follow that $Y_3(t)$ Granger causes $Y_1(t)$.
- Time resolution? Not so serious a problem? Not neuronal signal, but blurred through IRF



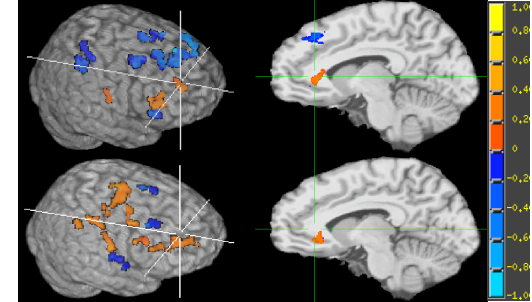
GC in AFNI

- Exploratory: ROI searching with **3dGC**
 - Seed vs. rest of brain
 - Bivariate model
 - 3 paths: seed to target, target to seed, and self-inflicted effect
 - Group analysis with **3dMEMA** or **3dttest**
- Path strength significance testing in network: **1dGC**
 - Pre-selected ROIs
 - Multivariate model
 - Multiple comparisons issue
 - Group analysis
 - path coefficients only
 - path coefficients + standard error
 - *F*-statistic (BrainVoyager)

GC: hands-on

■ Exploratory: ROI searching with **3dGC**

- Seed: sACC
- Sequential and batch mode (~5 minutes)
- Data courtesy: Paul Hamilton (Stanford)

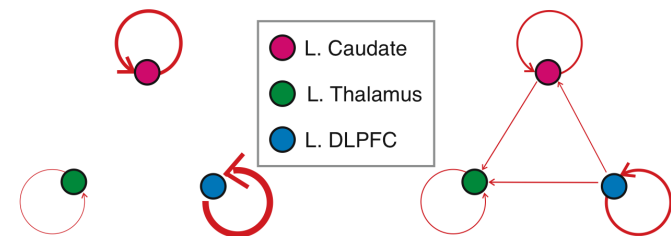


■ Path strength significance testing in network: **1dGC**

- Data courtesy: Paul Hamilton (Stanford)
- Individual subject
 - 3 pre-selected ROIs: left caudate, left thalamus, left DLPFC
 - 8 covariates: 6 head motion parameters, 2 physiological datasets

□ Group analysis

- path coefficients only
- path coefficients + standard errors



Summary: connectivity analysis

- 2 basic categories
 - Seed based method for ROI searching
 - ROI-based for network validation
- 3 approaches
 - Correlation analysis
 - Structural equal modeling
 - Granger causality
- A lot of interpretation traps
 - Over-interpretation seems everywhere
 - I may have sounded too negative about connectivity analysis
- Causality regarding the class: Has it helped you somehow?
 - Well, maybe?

Other approaches

- Multivariate (data-driven)
 - Techniques from machine learning, pattern recognition
 - Training + prediction
 - PCA/ICA
 - SVM: 3dsvm, plug-in
 - Kernel methods

Acknowledgments

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