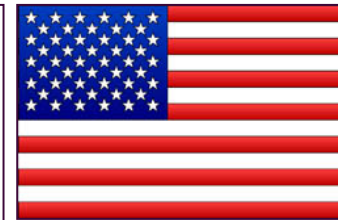


The Sources of Bias in Resting State FMRI

Ziad S Saad, PhD

SSCC / NIMH & NINDS / NIH / DHHS / USA /
EARTH

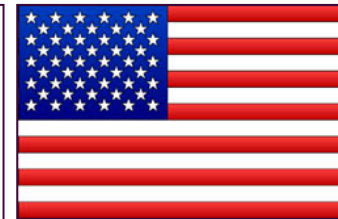


The Sources of Bias in Resting State FMRI

No Conflicts Of Interest To Declare

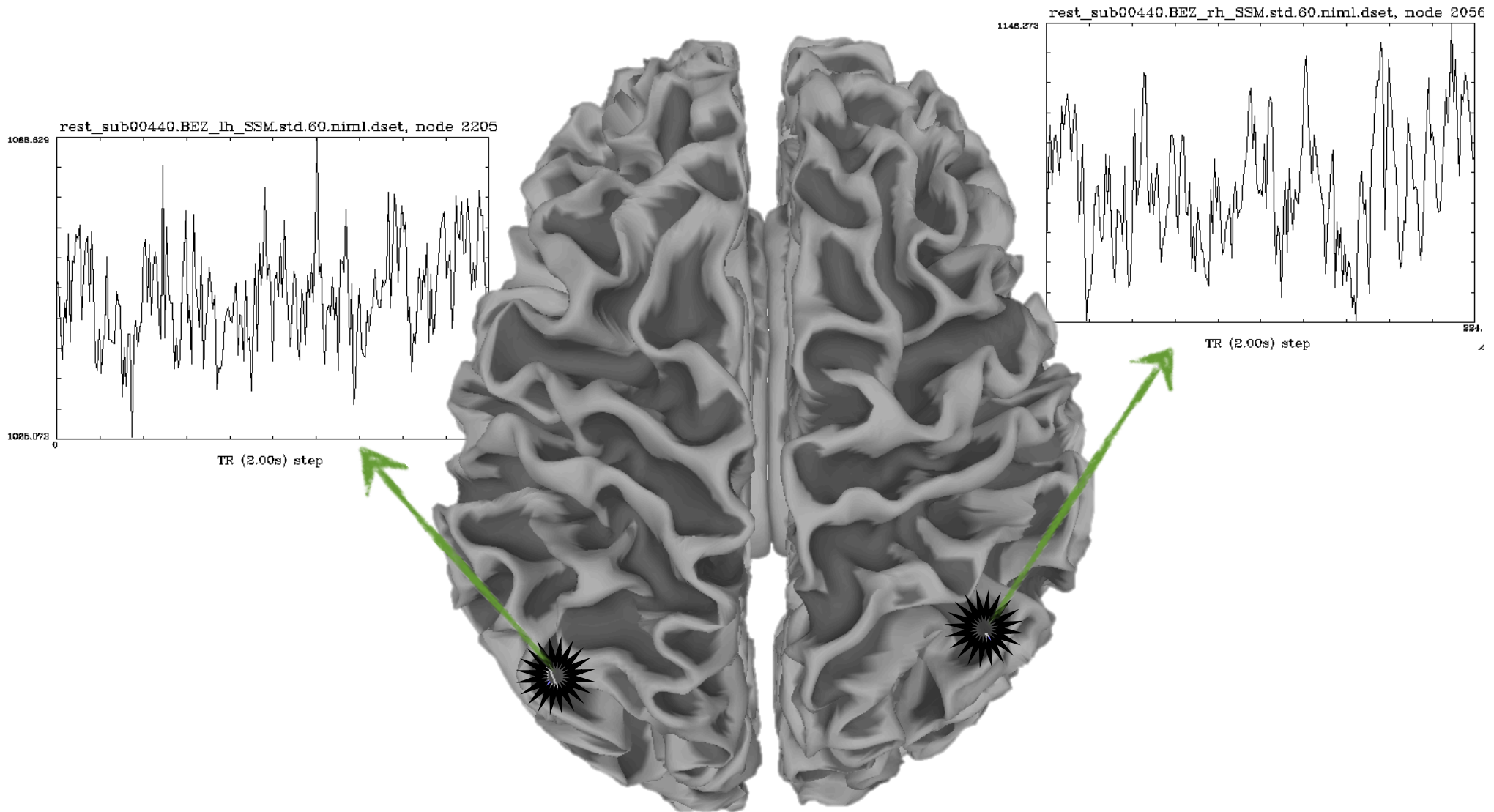
Ziad S Saad, PhD

SSCC / NIMH & NINDS / NIH / DHHS / USA /
EARTH



Resting state

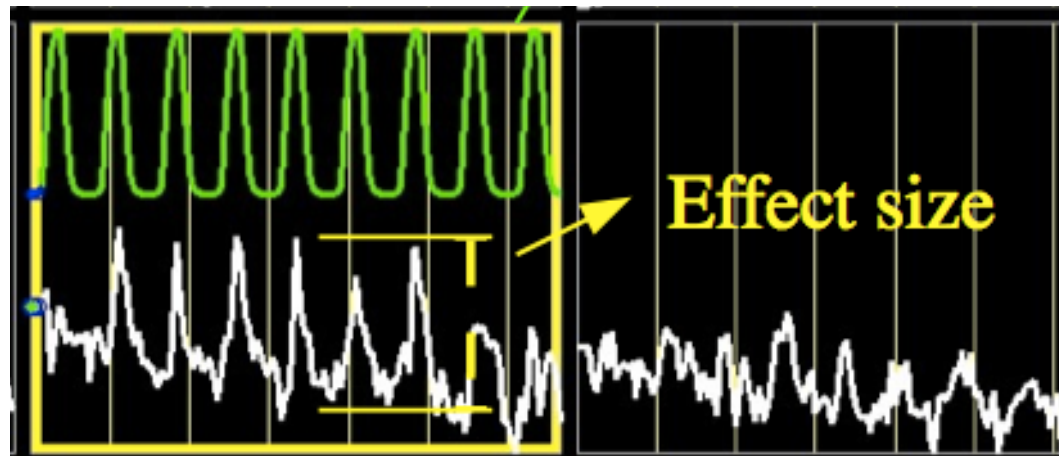
BOLD signal fluctuations **during undirected** brain activity



Resting state

BOLD signal fluctuations **during undirected** brain activity

There is **no model for signal**, such as expected response in task FMRI



Resting state

BOLD signal fluctuations **during undirected** brain activity

There is **no model for signal**, such as expected response in task fMRI

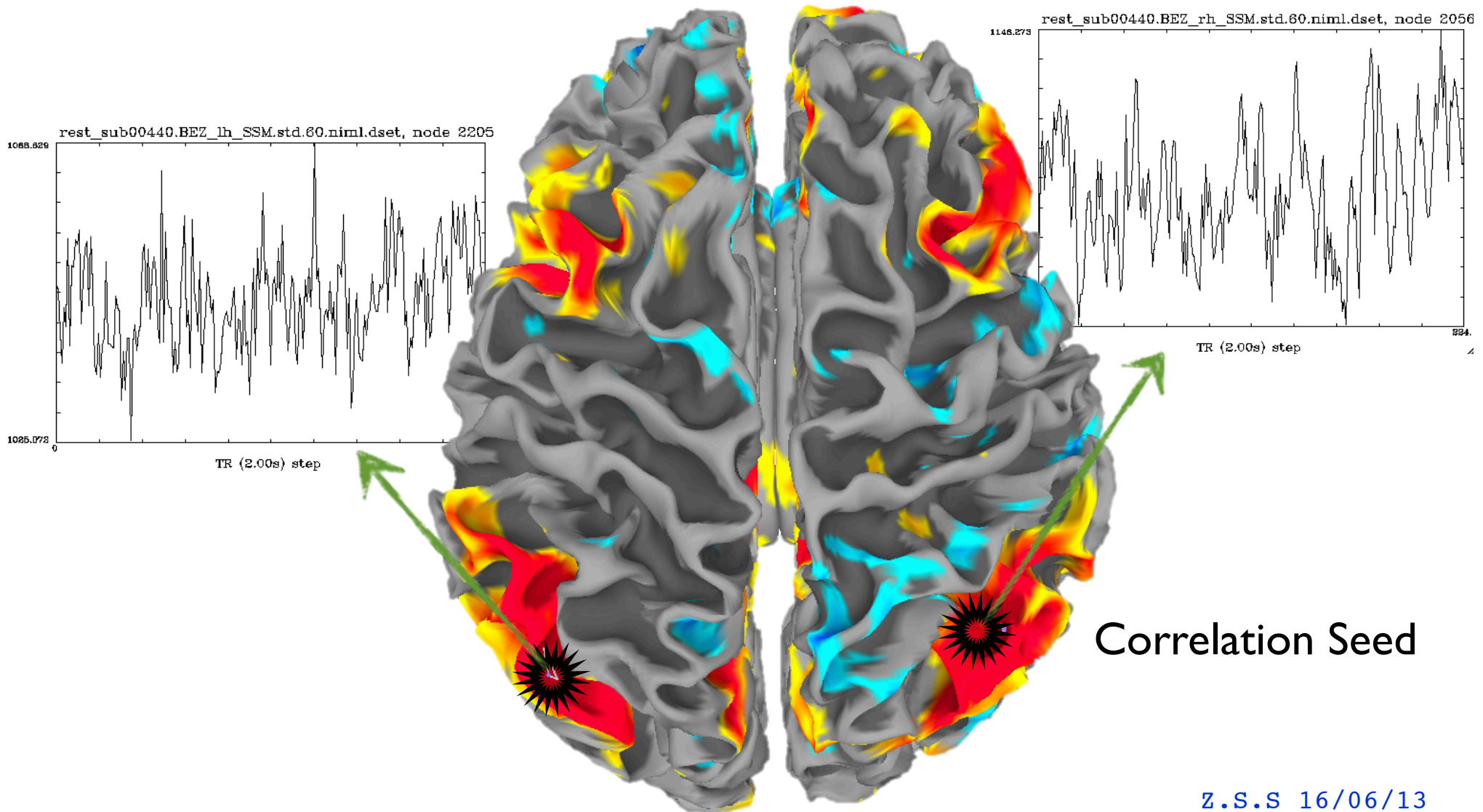
Resort to **describing relationships** between brain regions

Correlation matrices, graph theory, functional/effective/* connectivity

Factoring data into space \otimes time components in statistically interesting ways (PCA, ICA)

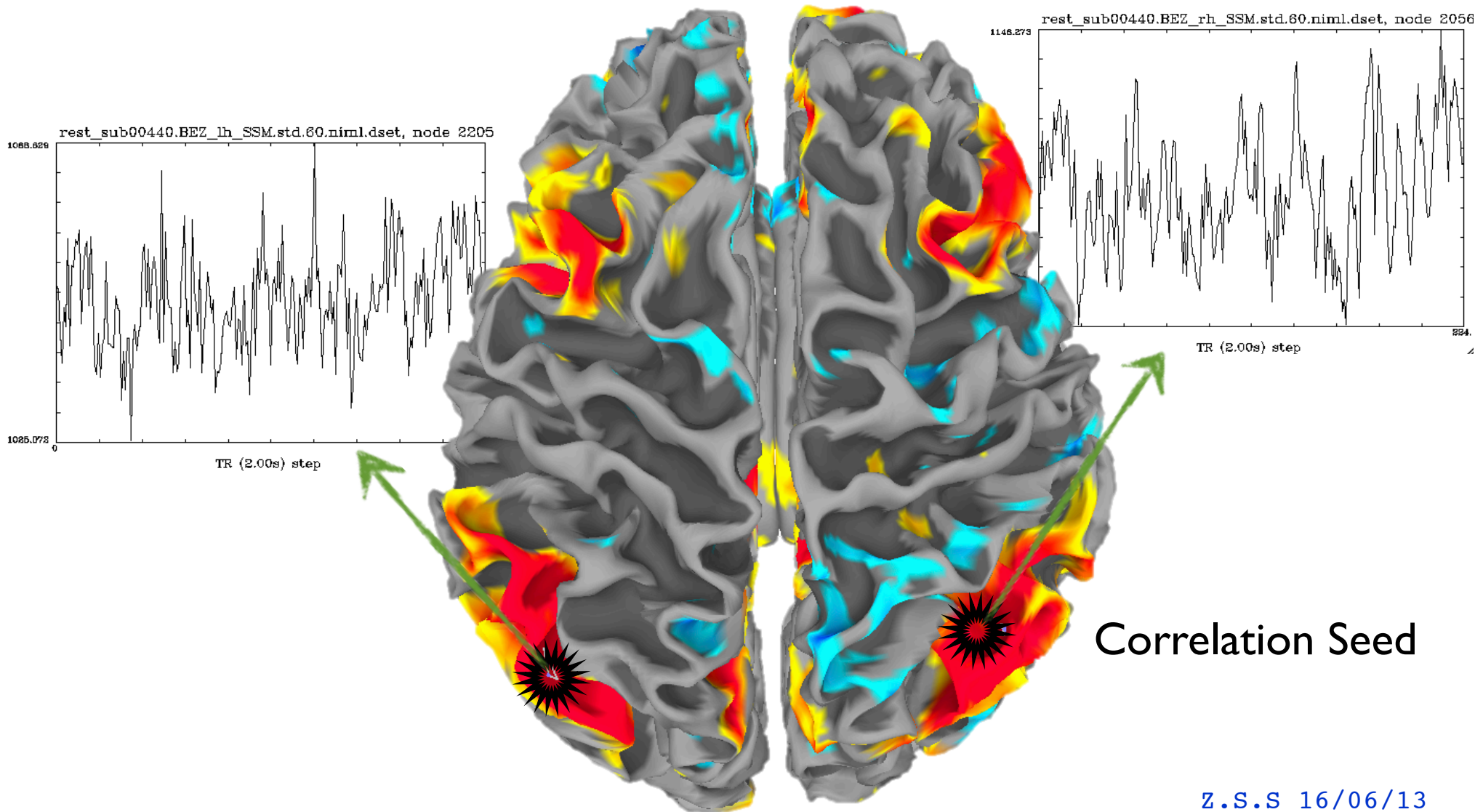
Resting state

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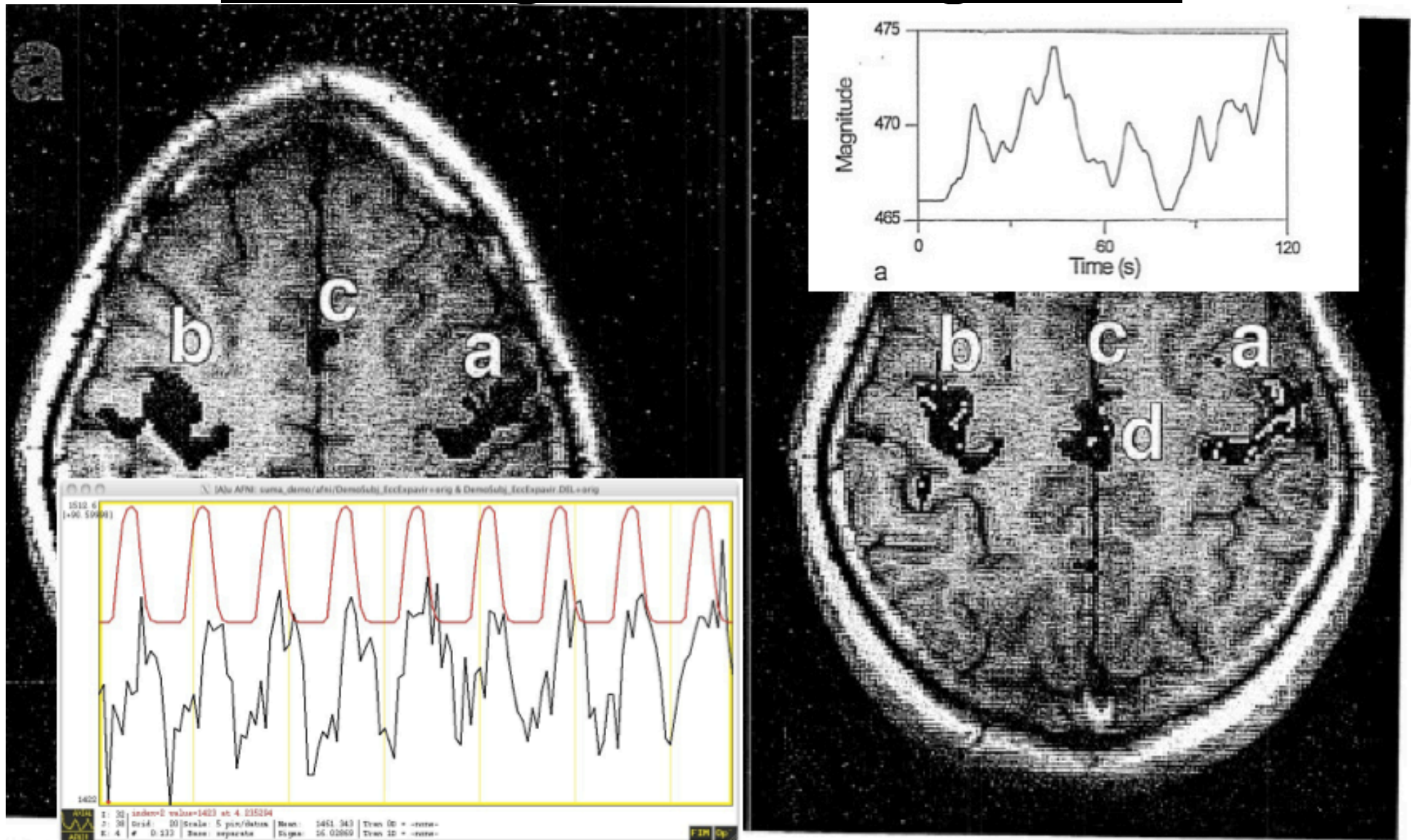


Resting state

Interpret **correlation strength as proxy** for brain function coupling between regions



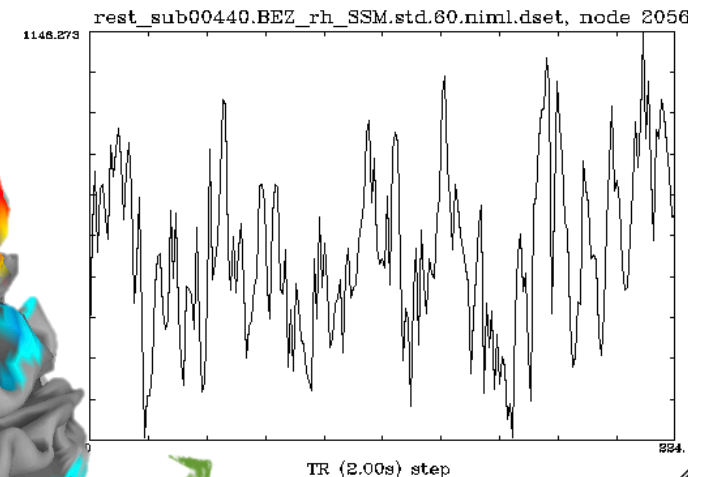
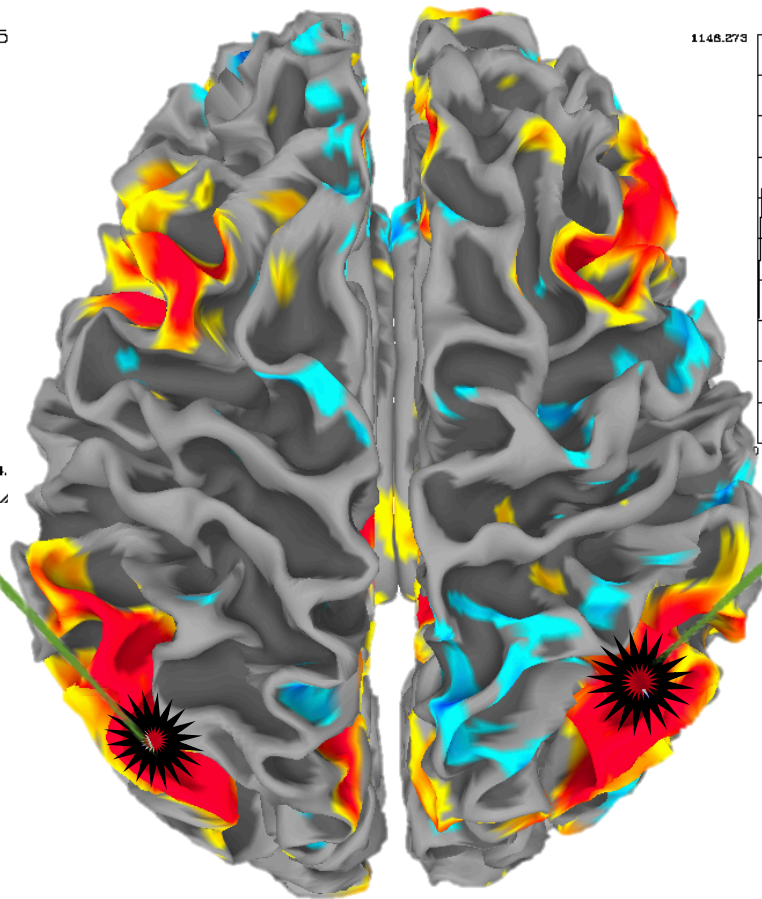
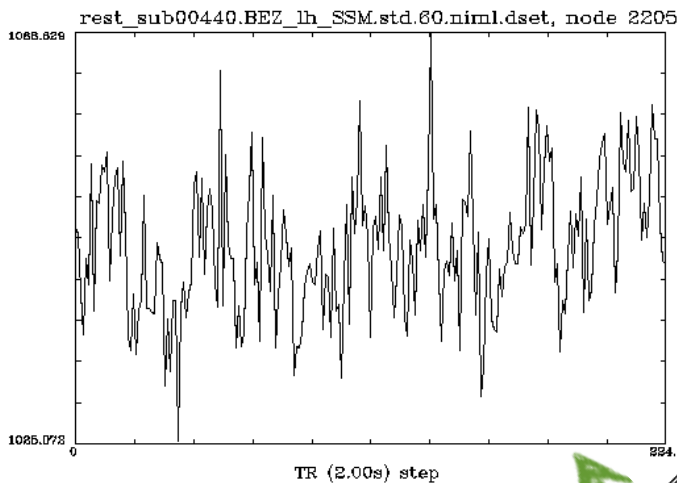
The magic of resting state (Biswal 95)



G. 3. (Left) FMRI task-activation response to bilateral left and right finger movement, superimposed on a GRASS anatomic image. (Right) Activation response using the methods of this paper. See text for assignment of labeled regions. Red is positive correlation, and yellow negative.

Resting state PROBLEM

Neuronally driven BOLD fluctuations of interest
AND
Fluctuations from respiration, heart beat, motion



The fount of our troubles

We have **no model for signal**

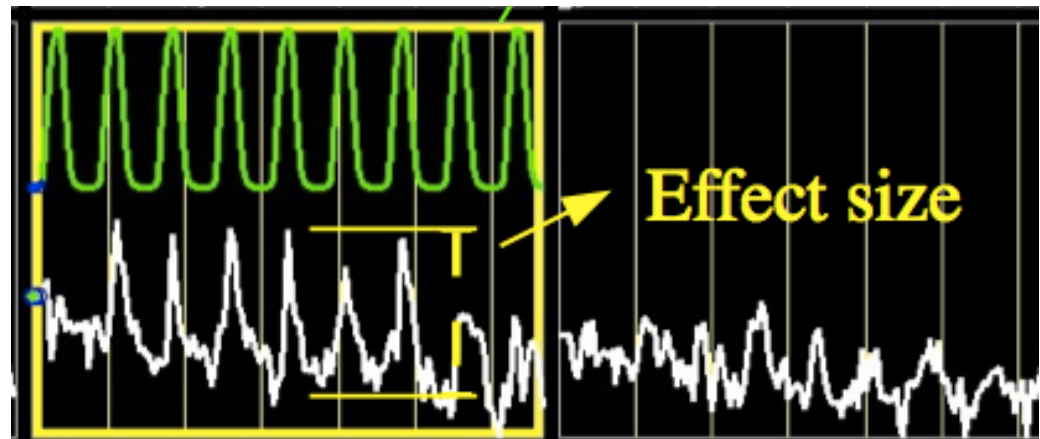
Nothing like the expected response (regressors) of task FMRI

We have **no good models for noise**

We have some, but they're far from perfect

Effect size (as correlation) is a spatially **varying function of noise** (fluctuations of no interest)

- Noise can bias correlations up, or down depending on the noise's spatial covariance
- In task FMRI by contrast, noise affects variance of effect amplitude estimate



The fount of our troubles

Difficult to attach meaning to effect size in RS-fMRI

Effect is like an SNR measure, affected by changes in both signal (numerator) and noise (denominator)

For example more motion → more noise → less
(or more!) correlation (bias) → group differences

Weak but consistent bias → significant difference

Some sources have brain-wide (global) effects on correlation distribution (e.g. ETCO₂, motion, etc.)

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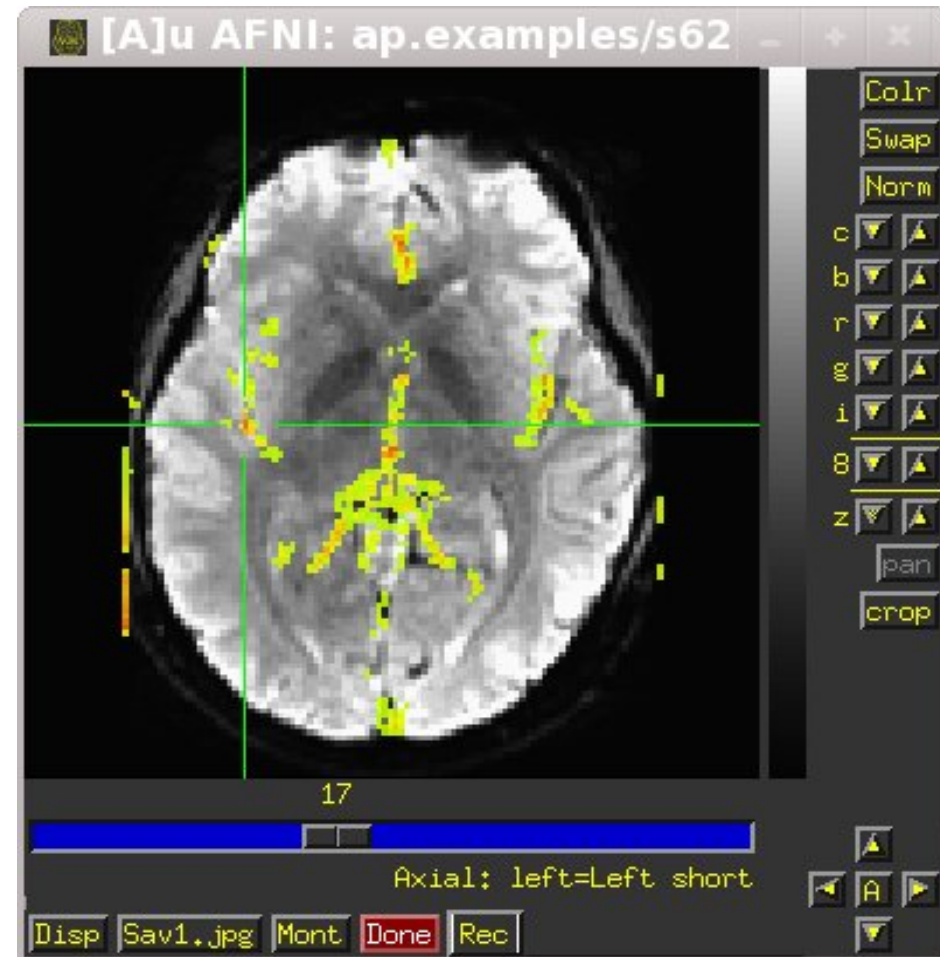
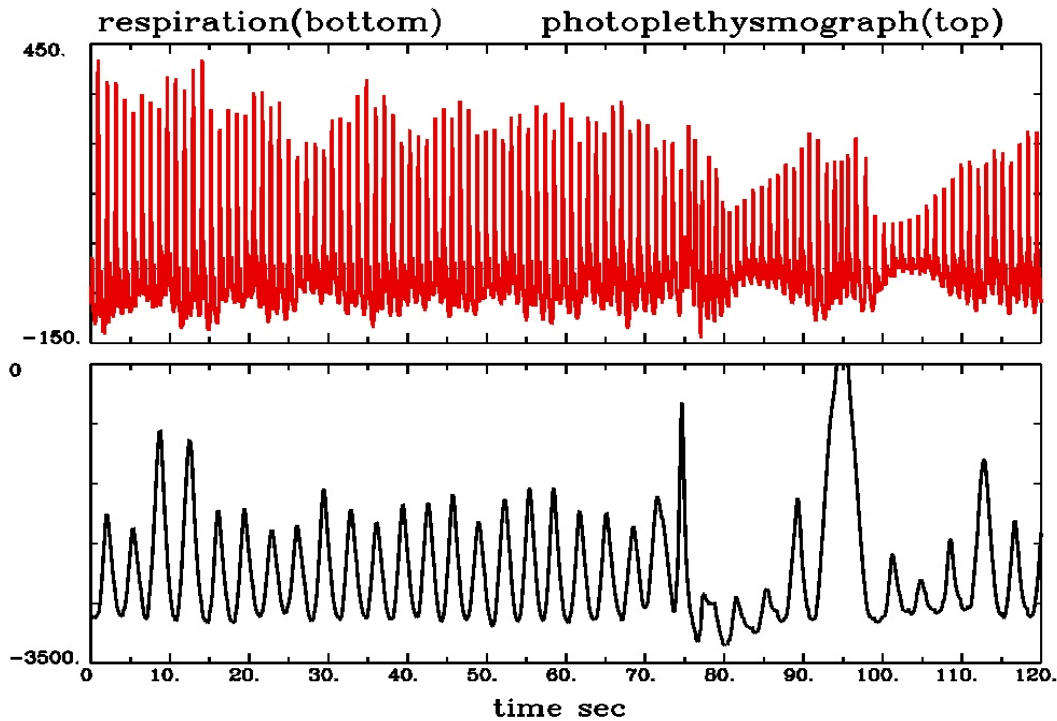
Sources of bias

- Head motion (Van Dijk, 2012) (Power, 2012)
- Physiological “Noise”
 - Respiratory or cardiac cycles (Glover, 2002)
 - Non-stationarity of breathing and cardiac rhythms (Birn, 2006) (Shmueli, 2007) (Chang, 2009)
- Hardware instability (Jo, 2010)
- Anatomical bias
- Pre-processing

Sources of bias

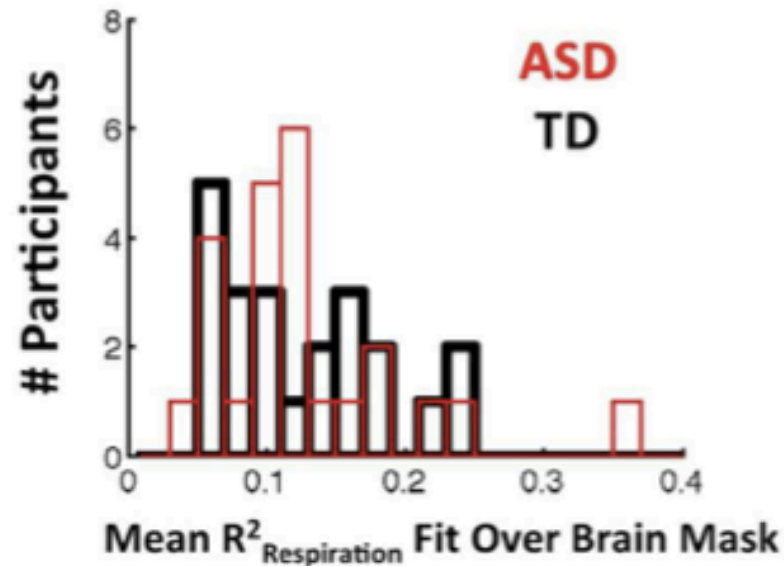
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Physiological noise



Bias from physiological noise

MR Signal Variance Accounted for by Respiration Measures



TD – ASD Connectedness, Respiration Not Removed

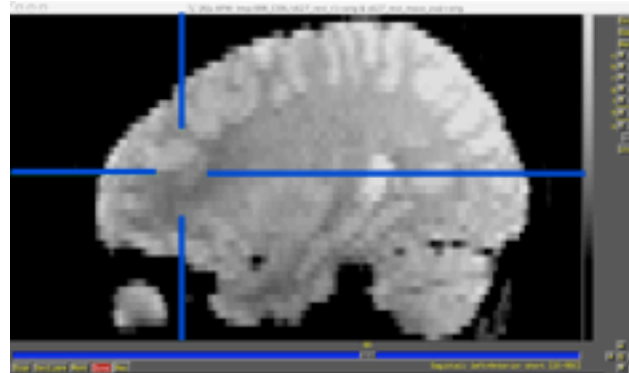
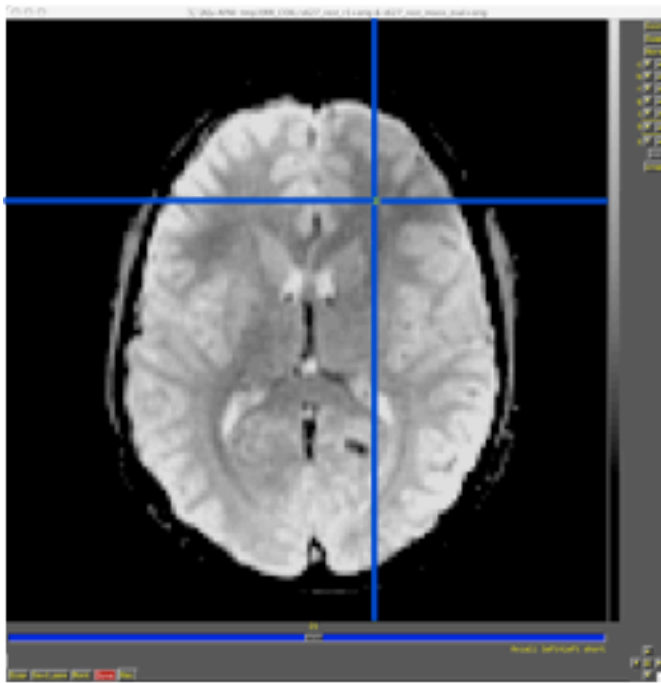
Gotts et al. 2012

- “All of these results highlight the importance of measuring and removing the effects of respiration in resting-state fMRI studies that compare two groups of participants, particularly if one of these groups involves a clinical population with anxiety symptoms that could alter normal breathing patterns.”

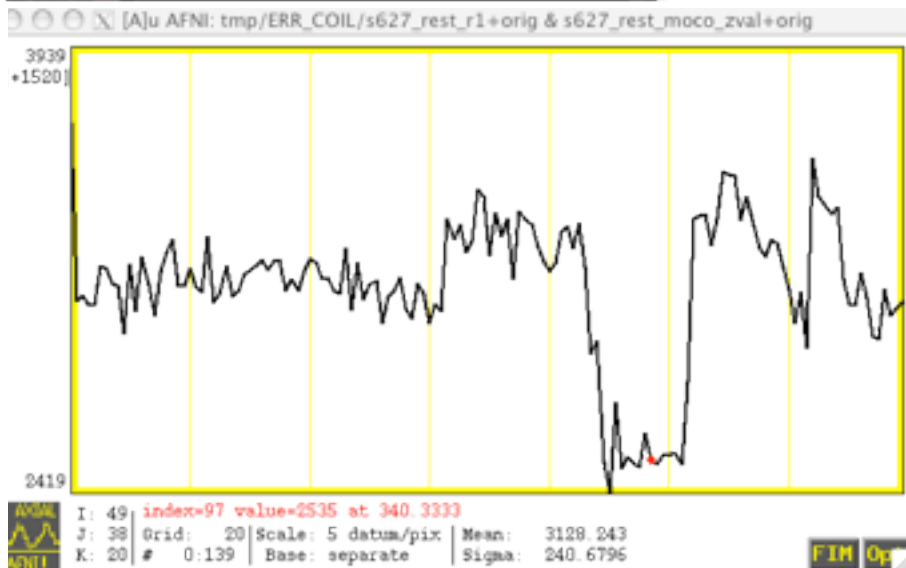
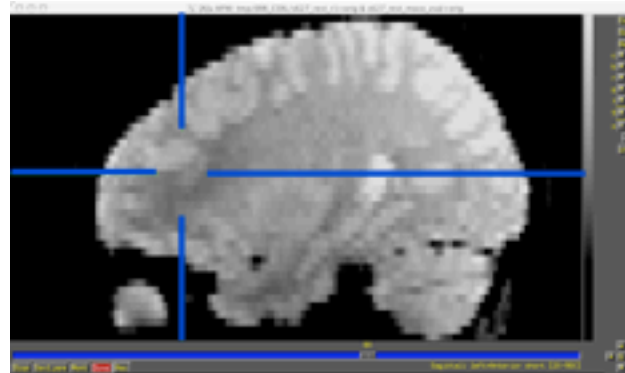
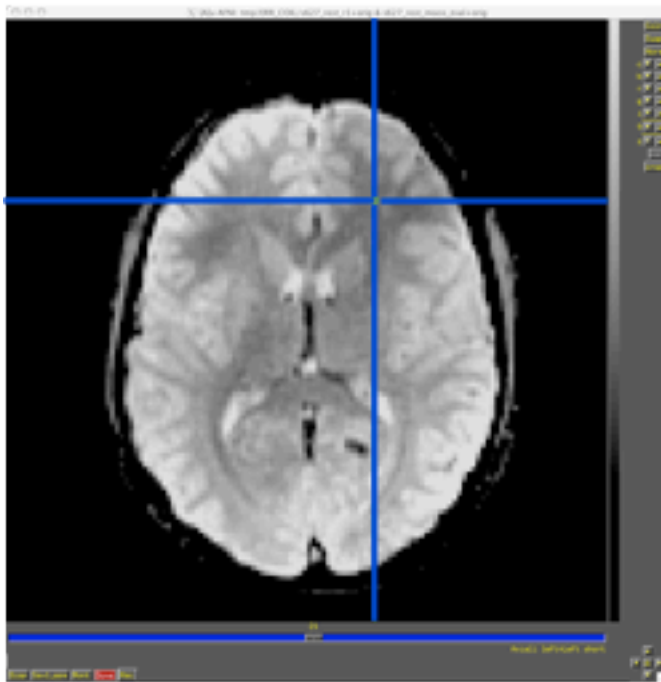
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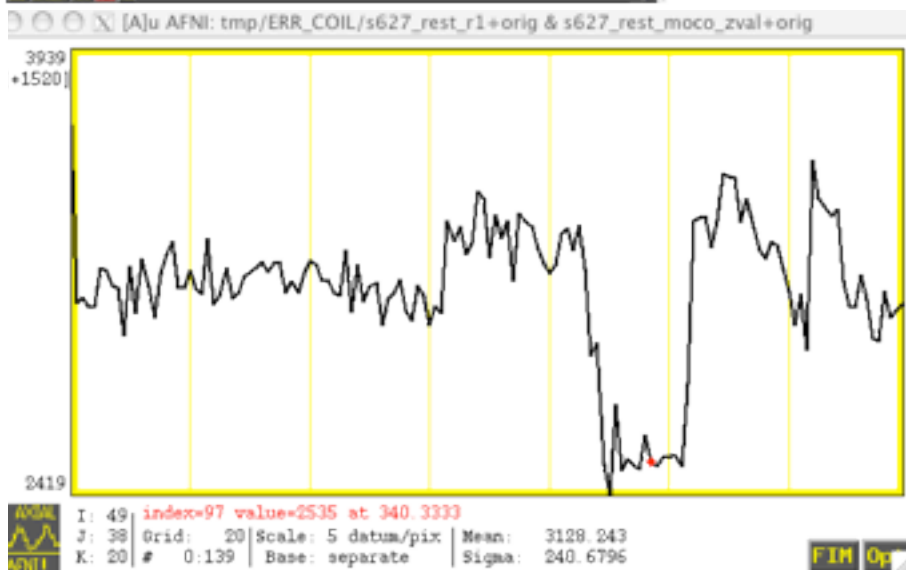
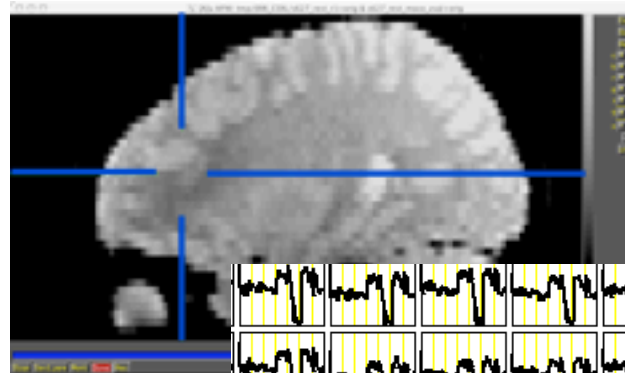
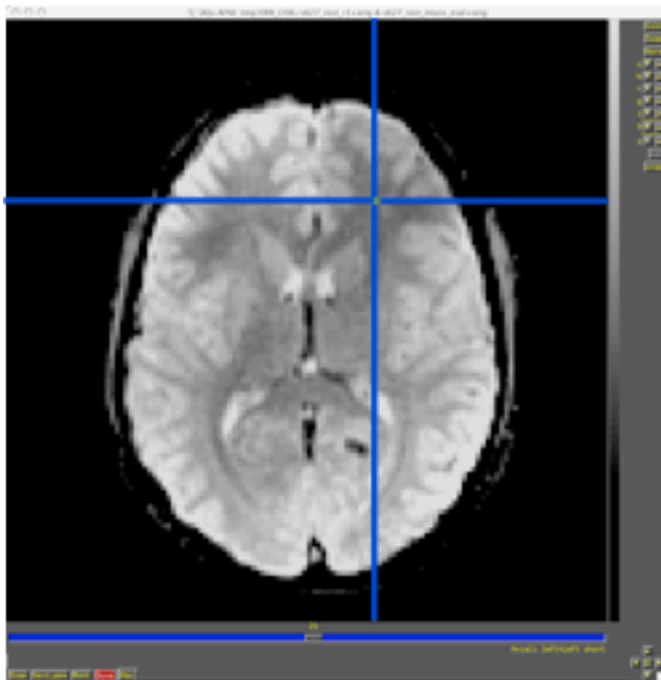
Hardware instability



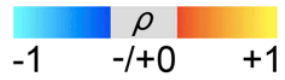
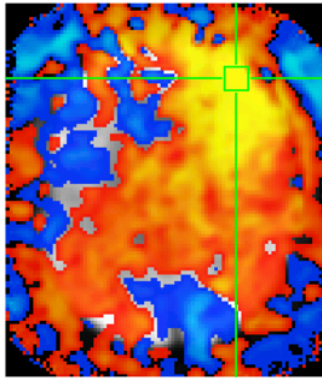
Hardware instability



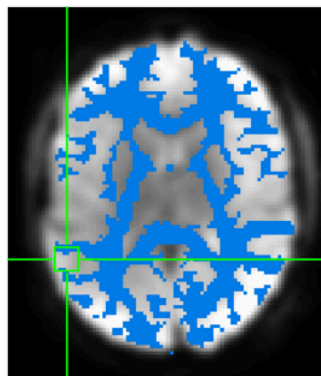
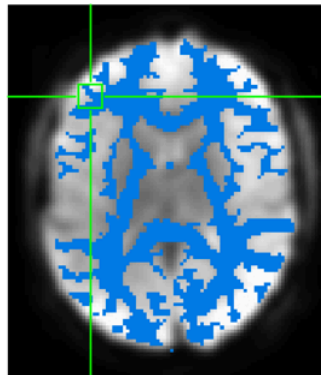
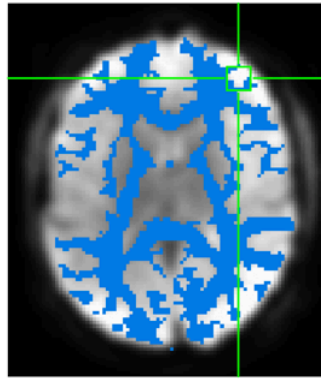
Hardware instability



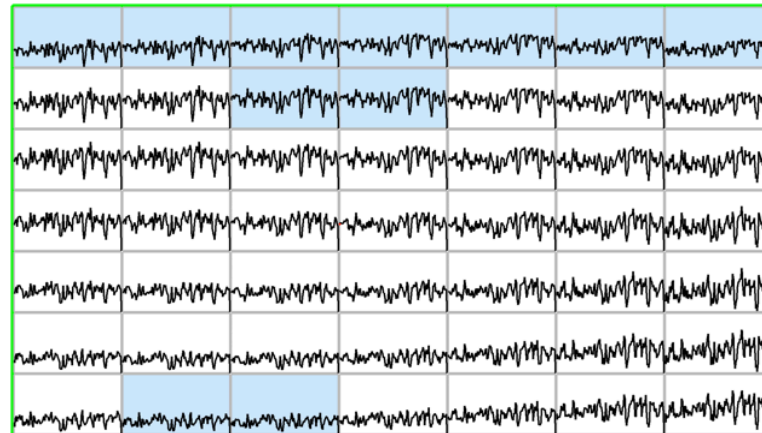
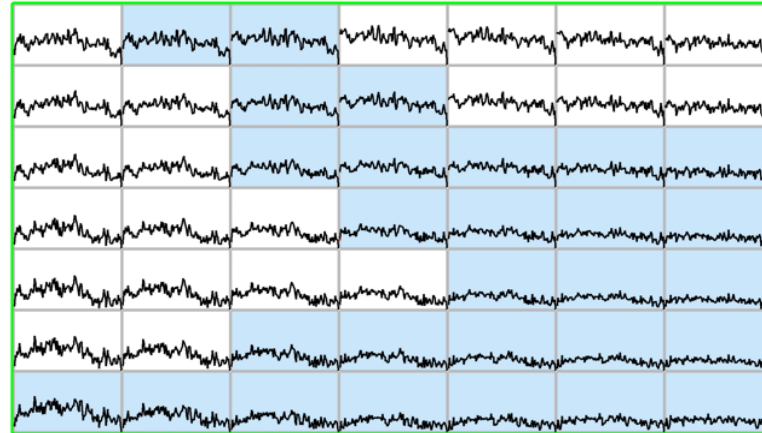
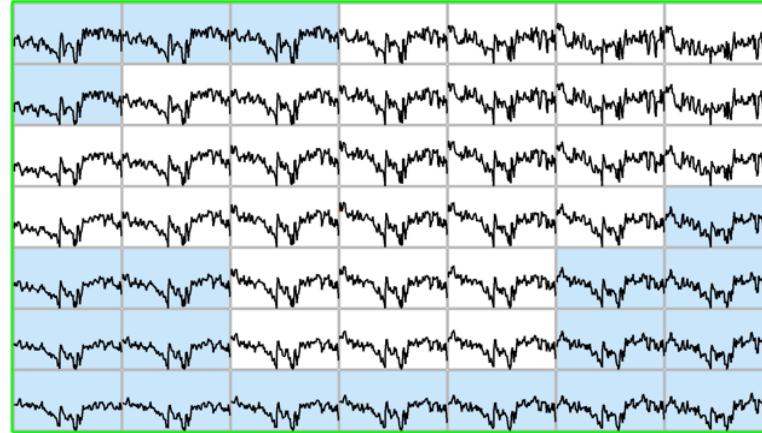
Correlation Map



Eroded WM



Time Courses

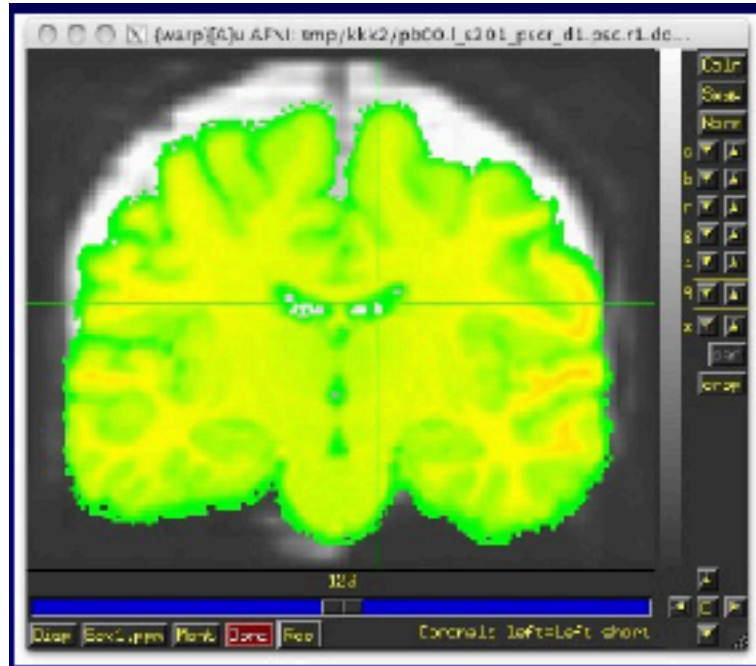


0 135 [TR]

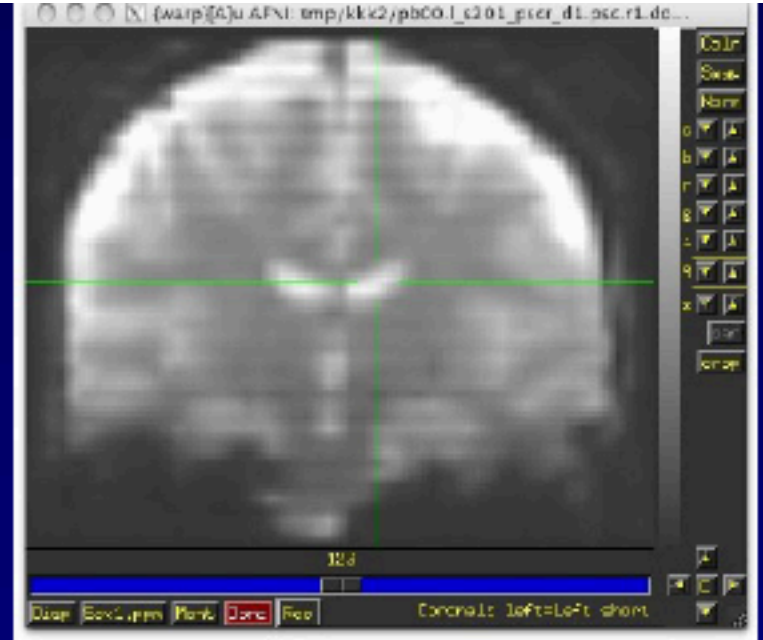
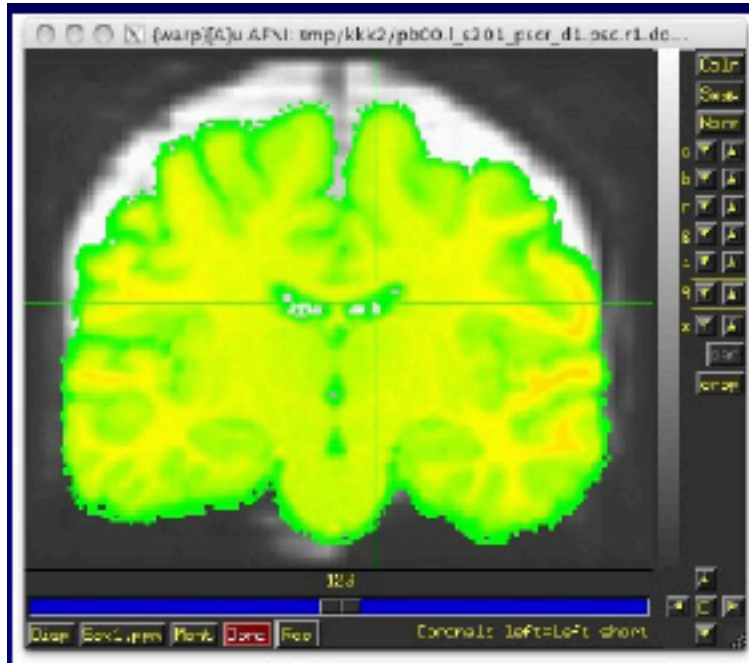
Sources of bias

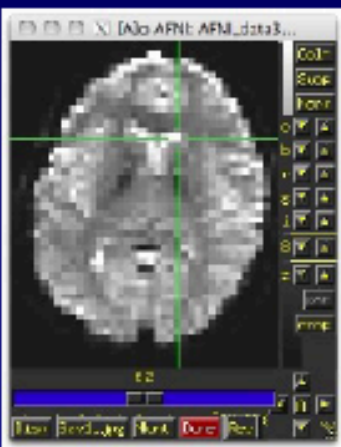
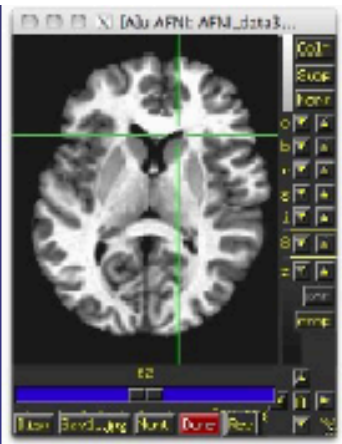
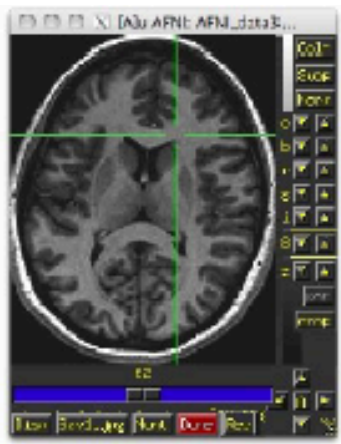
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Anatomical Bias

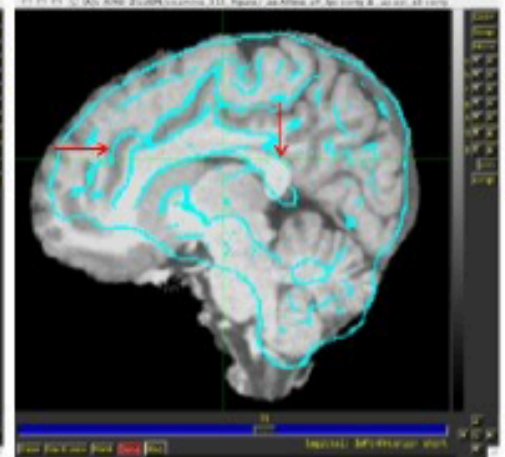
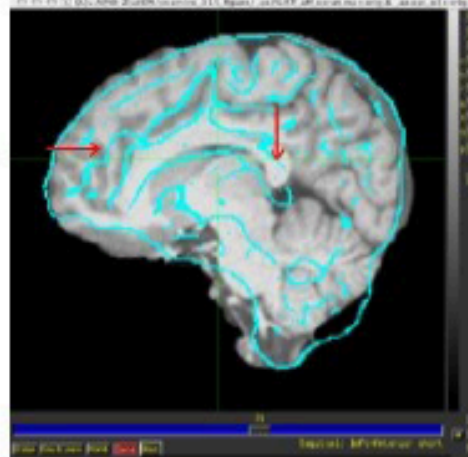
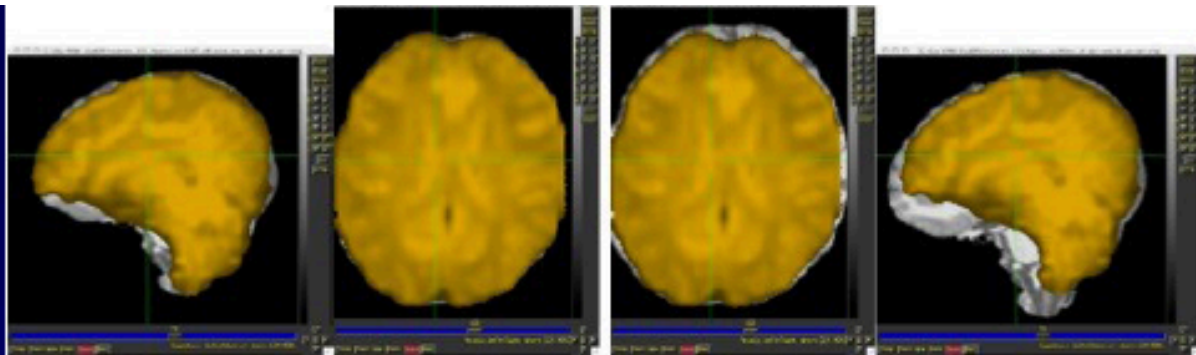


Anatomical Bias



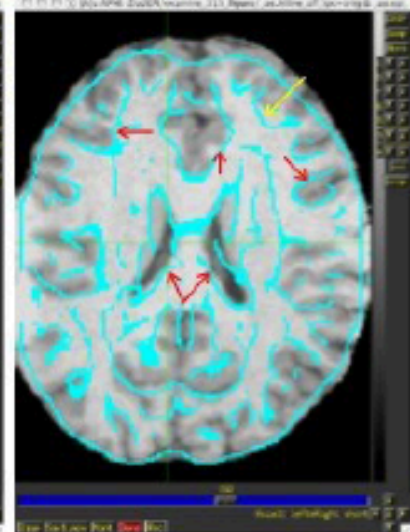
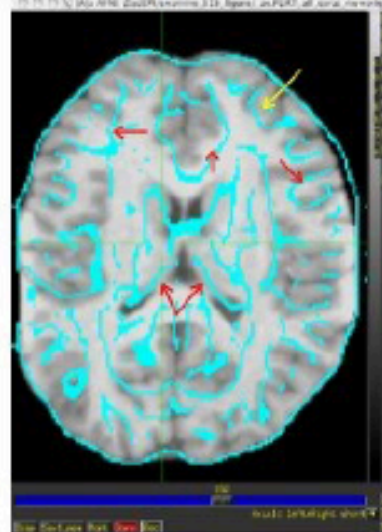


Need Spatial Contrast in EPI to judge alignment!



Cursory checks not enough

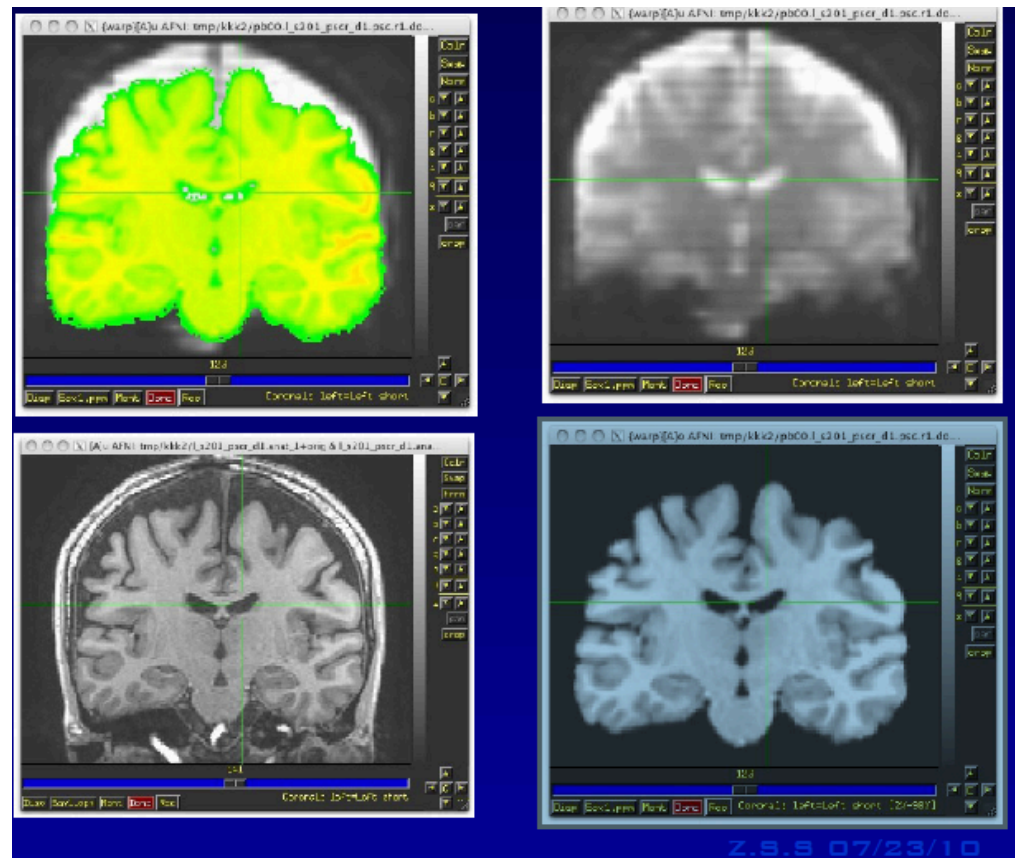
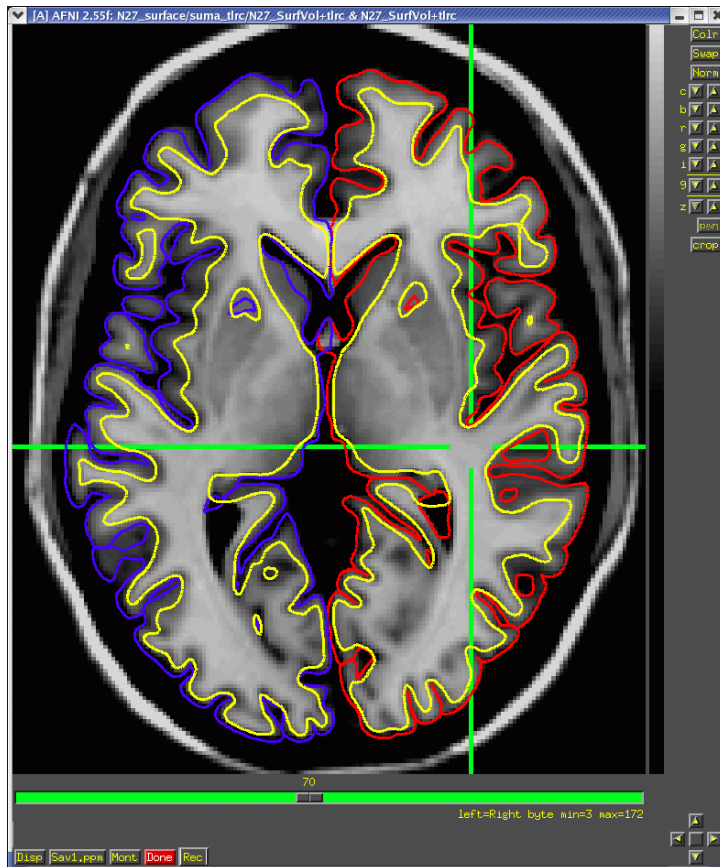
Normally, misalignment errors reduce power



With RS FMRI they can lead to effect differences

Anatomical Bias

- If concerned about systematic differences in anatomy, consider
 - Surface-based analysis with smoothing on the surface, or smooth within gray matter mask only
 - ROI-based analysis with ROIs restricted to gray-matter voxels in each subject



Adjusting for noise/bias sources

- Model noise effect on time series and project
 - Motion estimates
 - Retroicor/RVT/etc requires simultaneous recordings of cardiac and respiratory cycles
(Glover 2002; Birn 2006; Shmueli 2007; Chang 2009)
 - Nuisance signals estimates from dataset
 - Tissue-based nuisance regressors
(Beckmann 2004; Fox 2009; Behzadi 2007; Beall 2007, 2010; Jo 2010, 2013; Kundu 2012; Bright 2013; Boubela 2013)
- Group level adjustments
 - Covariates for motion, brainwide levels of correlation
(Van Dijk 2012; Satterthwaite 2012; Saad 2013; Yan 2013)

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Tissue-based nuisance regressors

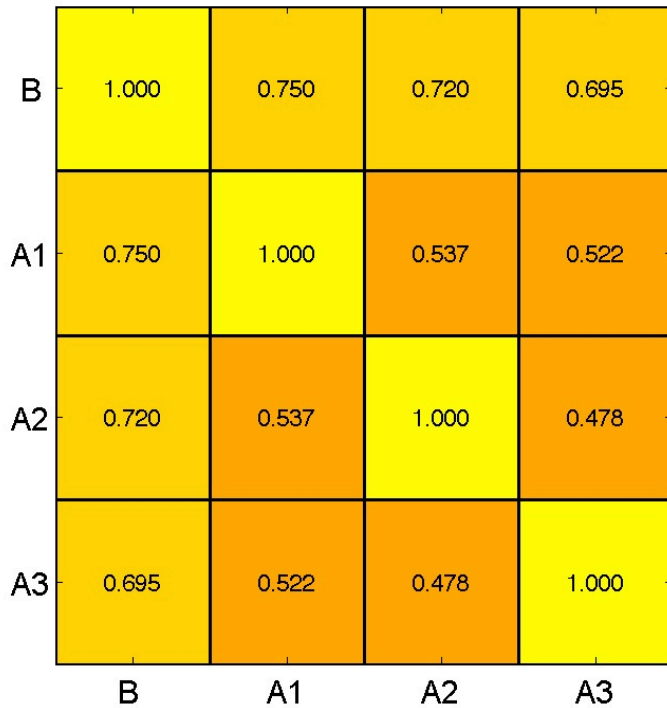
- **Avoid Projecting Fluctuations of Interest**
- OK to sample nuisance signals from regions whose fluctuations are not correlated with the *fluctuations of interest* in the regions of interest
- Should not project time series containing aggregates of fluctuations of interest, even if they contain contribution from noise
 - Sagittal sinus voxels might allow sampling of aliased heart rate, HOWEVER they also exhibit BOLD fluctuations of interest from the regions being modeled (Jo, 2010)

And why not?

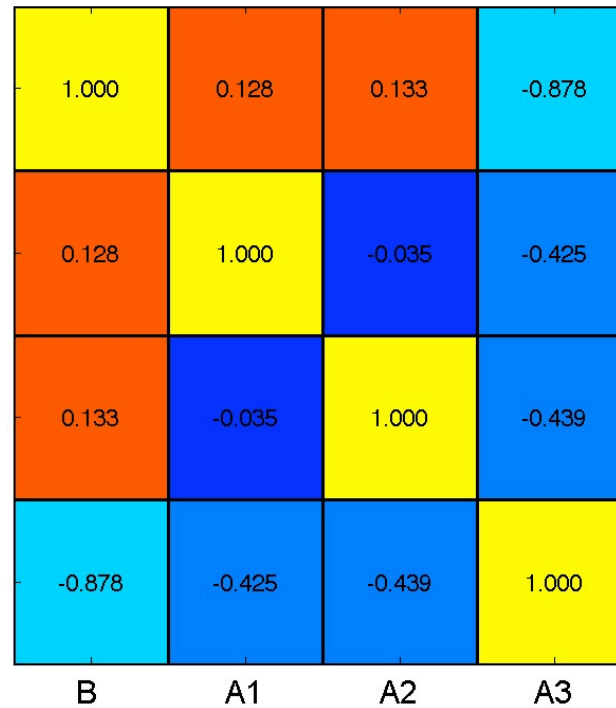
- Because you end up **differentially biasing** the correlation matrices of your groups, and considerably distorting group differences
- Best explained with GSRreg because math is straight forward.
 - What follows applies whether or not noise exists or differs between groups

Why not GSReg ?

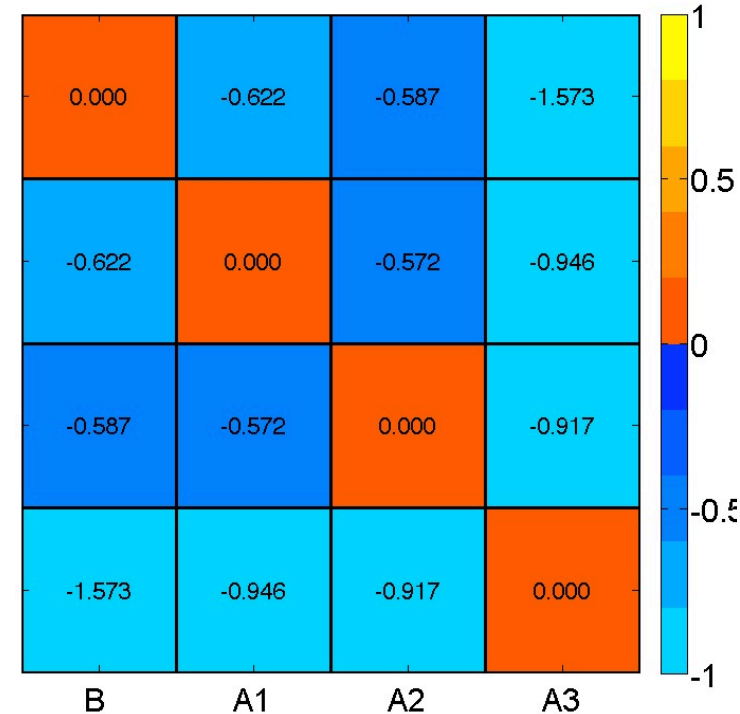
Original (R)



After GSReg (S)



$S - R$



Bias **will vary** by region pair

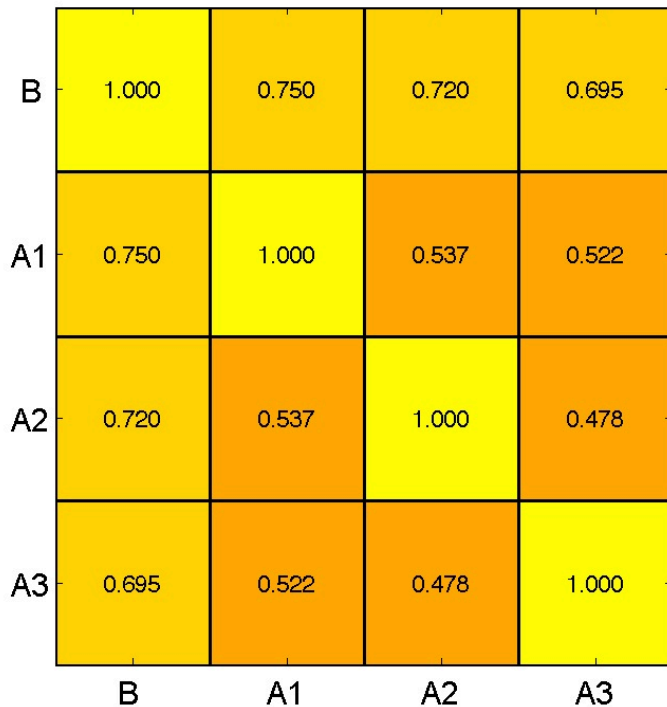
AND

Entirely dependent on initial covariance matrix P

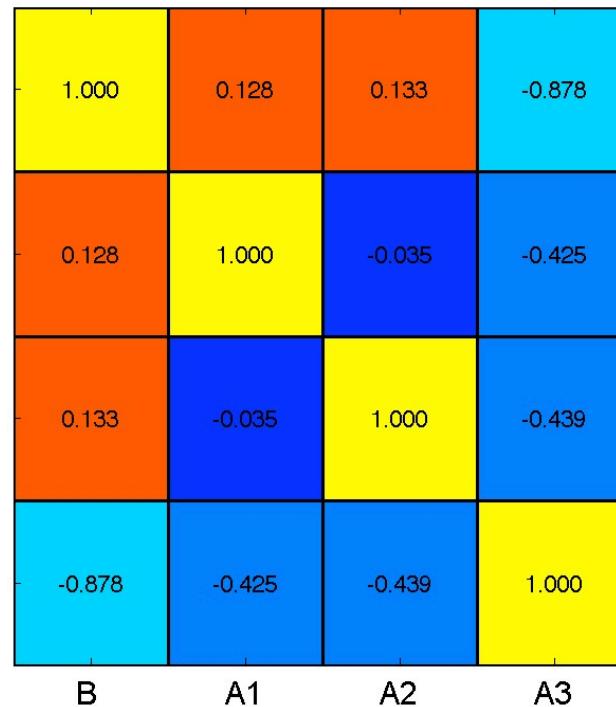
(therefore your grouping variable)

Why not GSReg ?

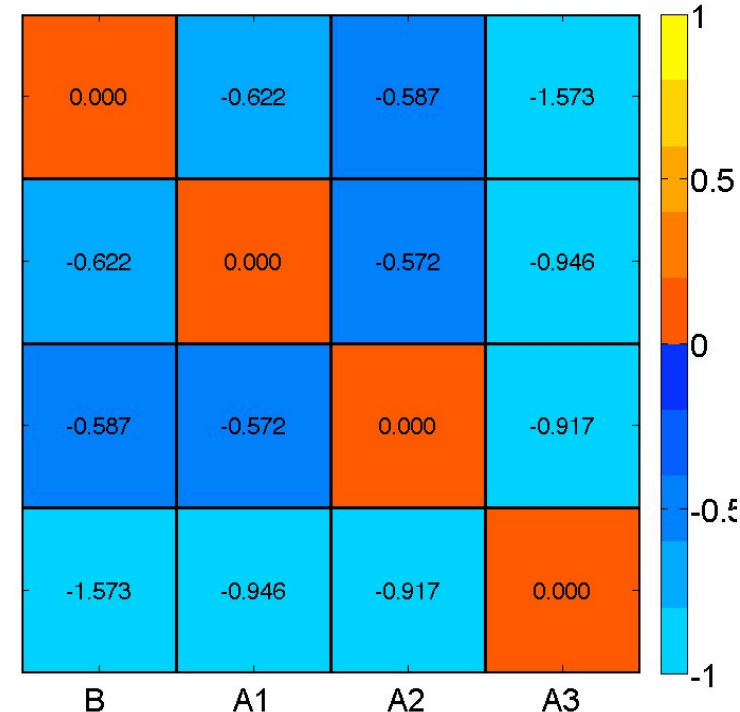
Original (R)



After GSReg (S)



$S - R$



For any FMRI time series (not simulations)

$$S - R = (P - (P11^T P)/(1^T P 1)) * \sigma_Q \sigma_Q^T - P * \sigma_P \sigma_P^T$$

$S - R$ is constant for group with same cov. matrix P

(Q is also a sole function of P) (Saad, 2013)

Are biased estimates useful?

Region pair dependent **biasing is OK** if:

Not interpreting correlations between regions as those between the sampled BOLD signals and by extension neuronal signals

Not just about interpretability of negative correlations ([Murphy, 2008](#); [Weissenbacher, 2009](#); [Cole, 2010](#))

Two strongly correlated regions after GSReg DOES NOT imply regions were strongly correlated before GSReg

Using correlations after GSReg as some feature space for parcellation, classification, etc ([Craddock, 2009](#))

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Region pair dependent **biasing can be problematic** when interpreting connectivity matrix differences:

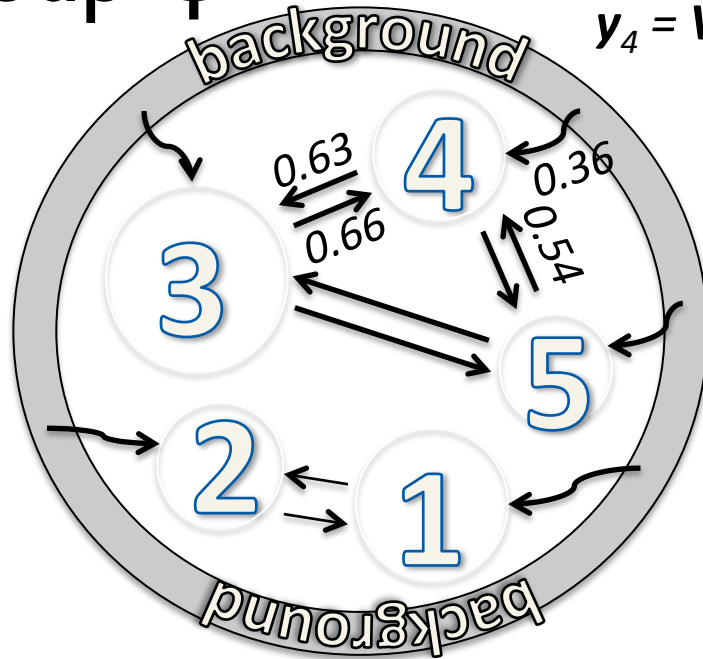
$$S - R = (P - (P11^T P)/(1^T P1)) * \sigma_Q \sigma_Q^T - P * \sigma_P \sigma_P^T$$

S-R is constant for group with same cov. matrix **P**

S-R will differ between groups with different **P**

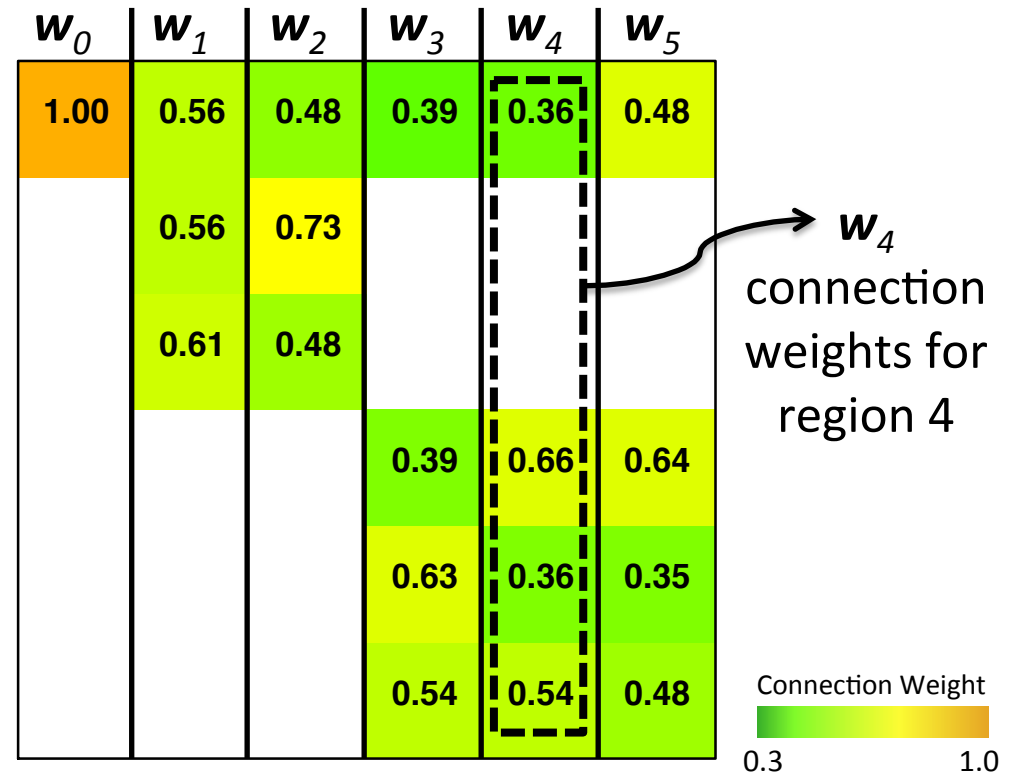
An illustrative model

Group Ψ



Observed signal from region 4:

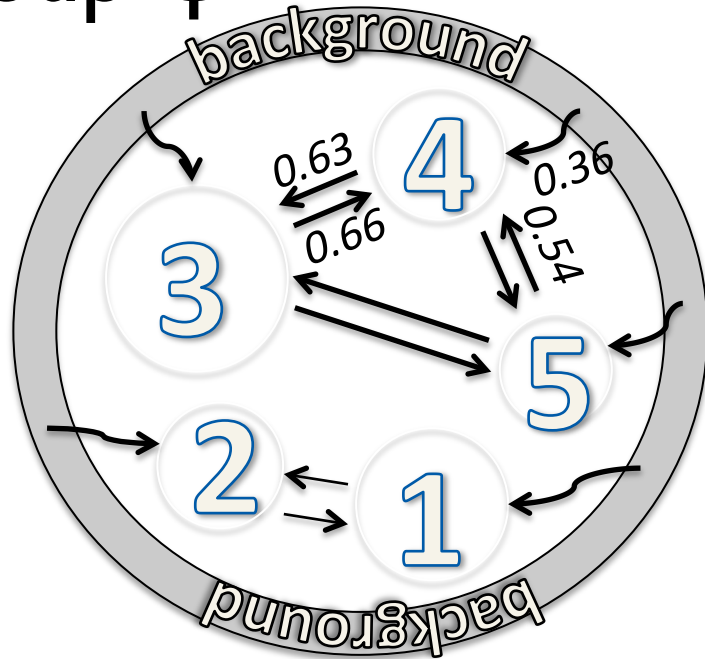
$$y_4 = V w_4 + e = 0.36 v_0 + 0.66 v_3 + 0.36 v_4 + 0.54 v_5 + e$$



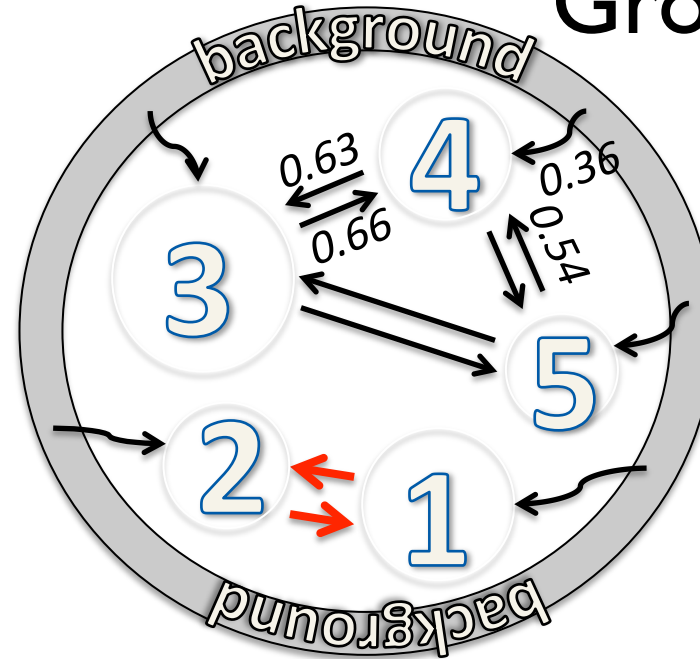
In simulations 9 regions + background were used

Comparing Groups

Group Ψ



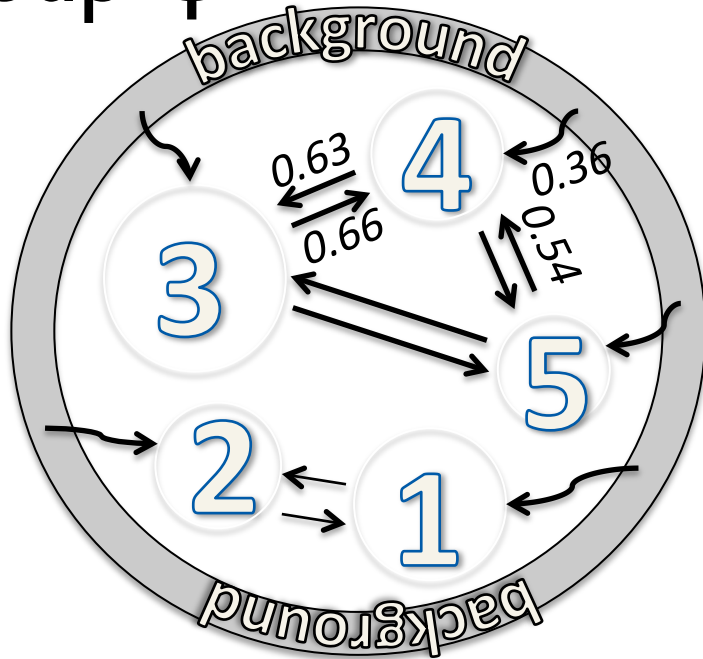
Group Ψ_L



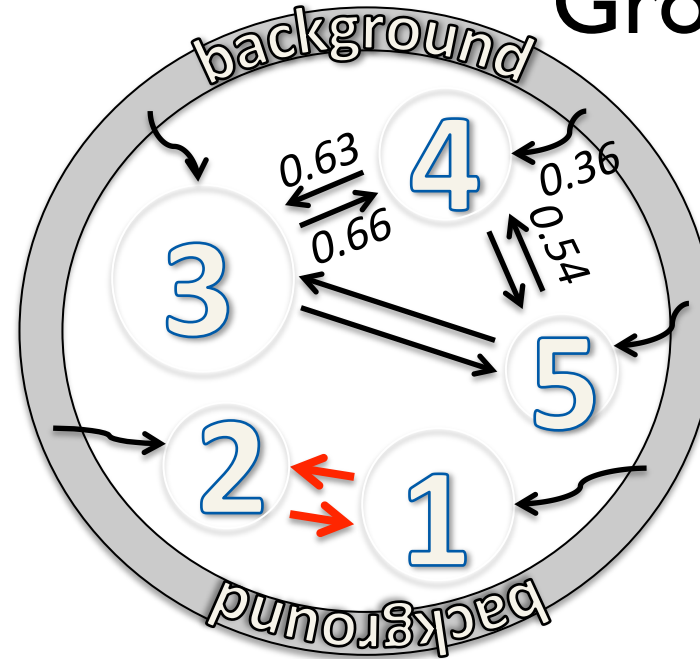
Increased connection
between regions 1 and 2 only

Comparing Groups

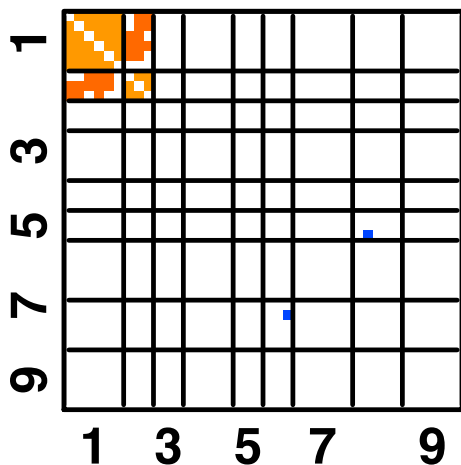
Group ψ



Group ψ_L



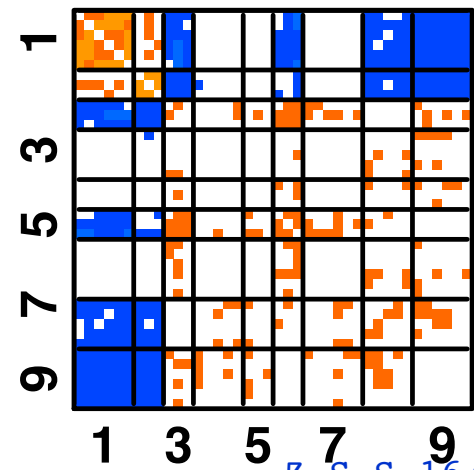
$\psi_L - \psi$ Base



Difference confined
to two regions

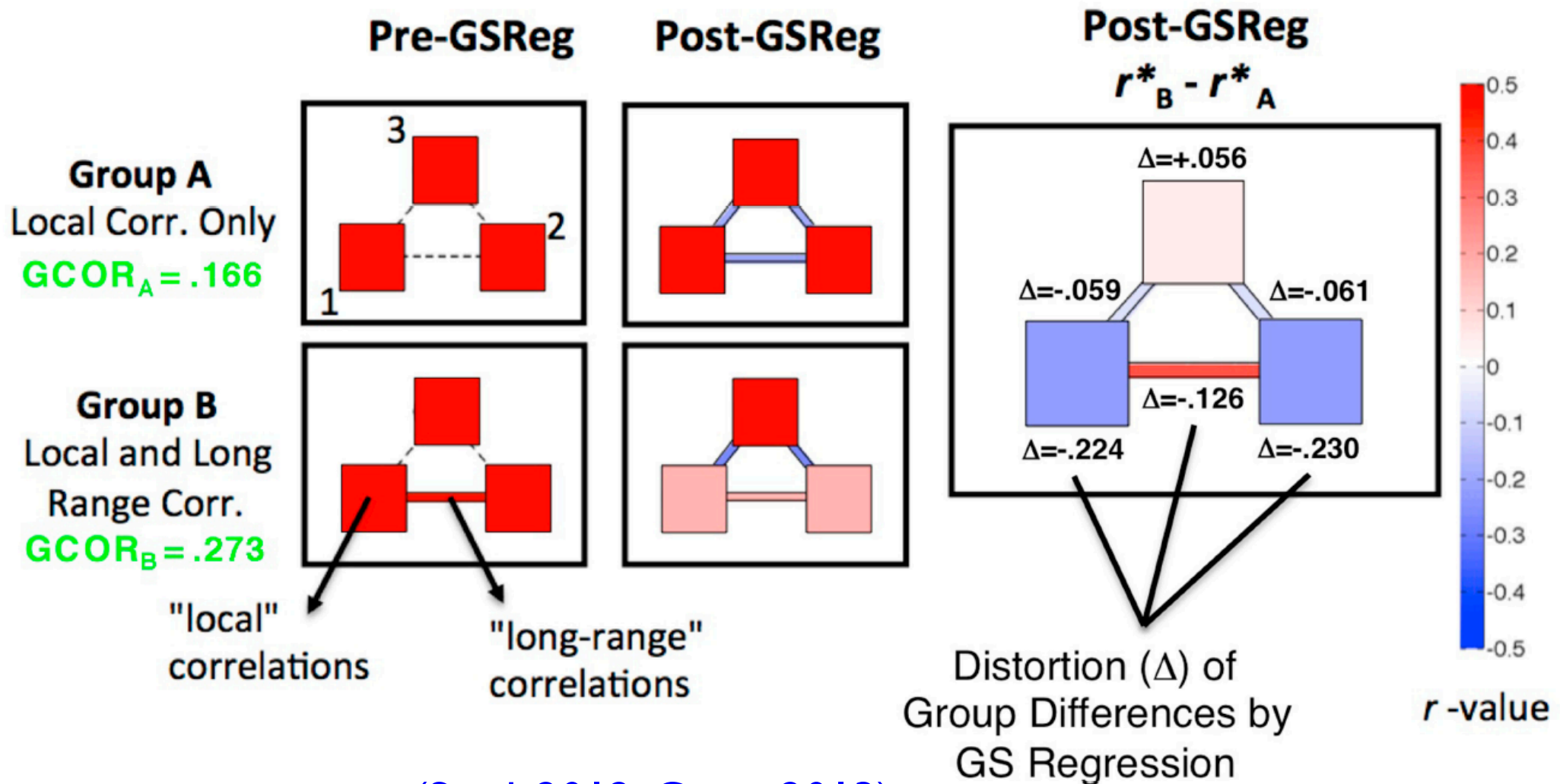
Ends up all
over the place

$\psi_L - \psi$ GSReg



Distortion of long/short range correlations

Contrast of correlations between groups A and B
 'long-range' correlations in Group B only



(Saad, 2012, Gotts 2013)

Comparing Groups with GSReg

One seeks and hopes for differences in covariance/correlation structures between groups.

Using GSReg means each group will be biased DIFFERENTLY for different region pairs.

- Even in the absence of noise difference, you could find group correlation **differences** in places where **none existed before**.
 - OK if you're teaching a classifier to differentiate between the two groups.
 - NOT OK if interpreting correlation differences to evoke correlation differences of neuronally induced BOLD signal between these regions.

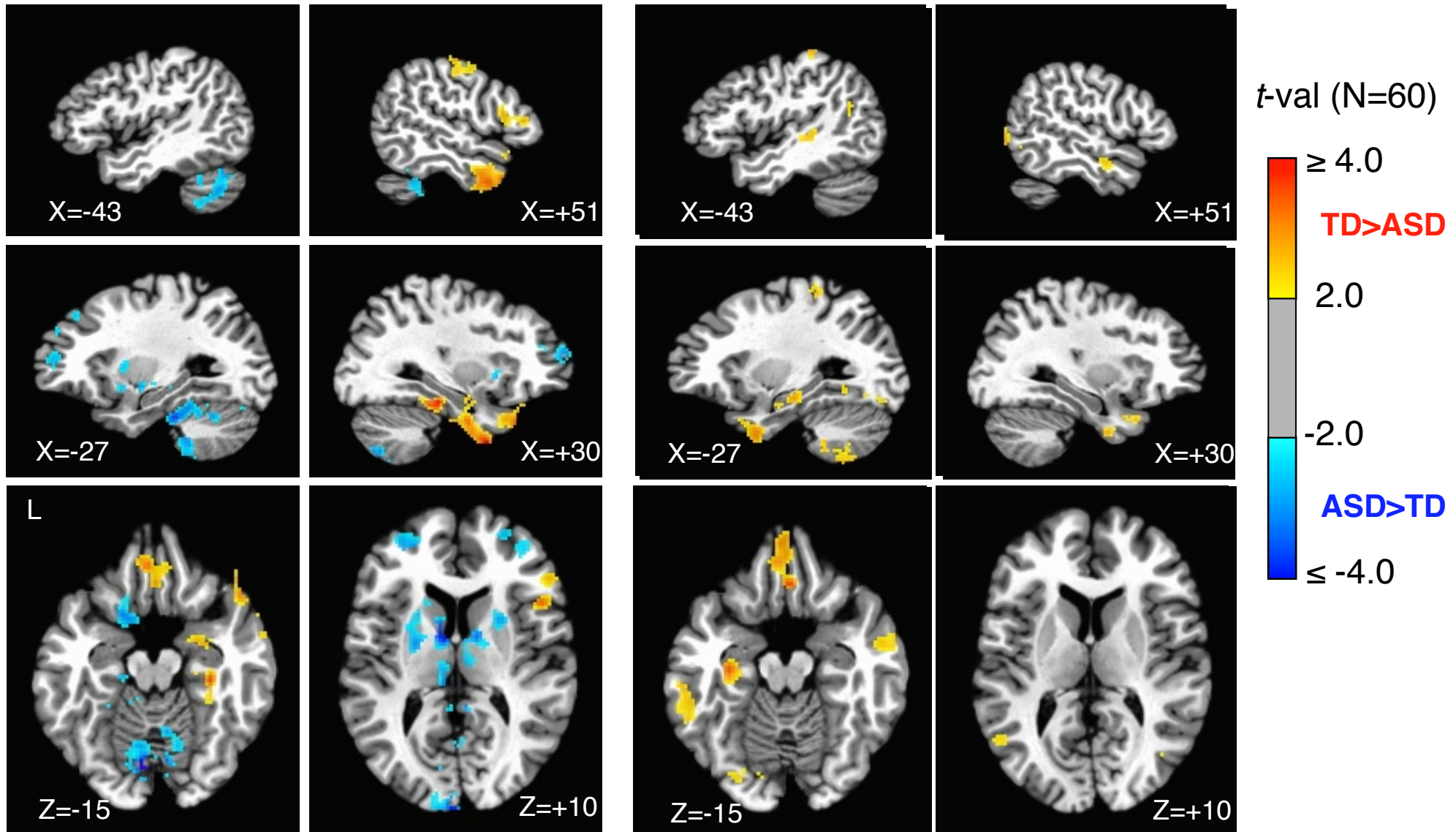
With noise previous problems remain

- However bias now depends on the covariance structures of noise and signals of interest though we can't tell them apart.
- Interaction between GSReg projection effects and grouping variable remains

SAME holds with empirical data

+ **GS Regression**

ANATICOR (Jo, 2010)



(Gotts, 2013)

Z.S.S 16/06/13

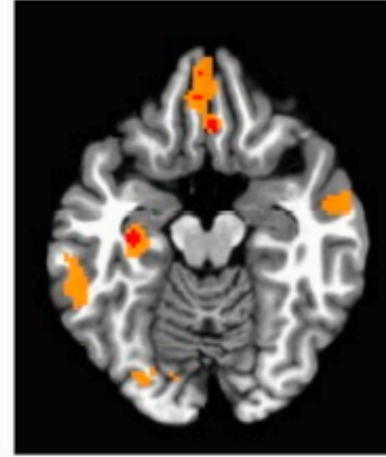
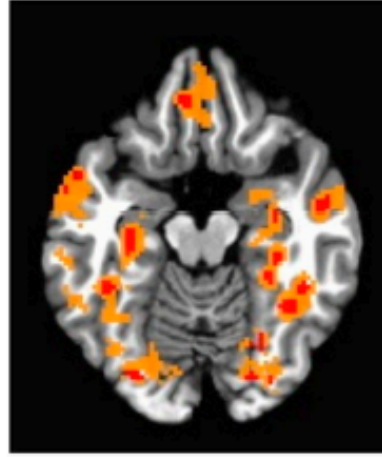
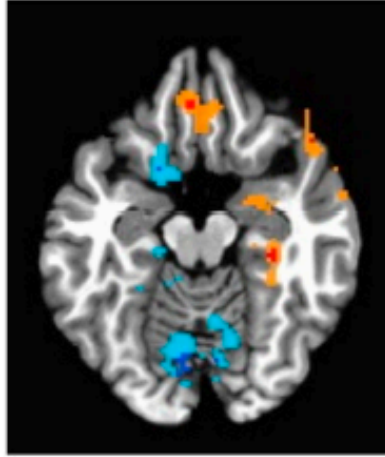
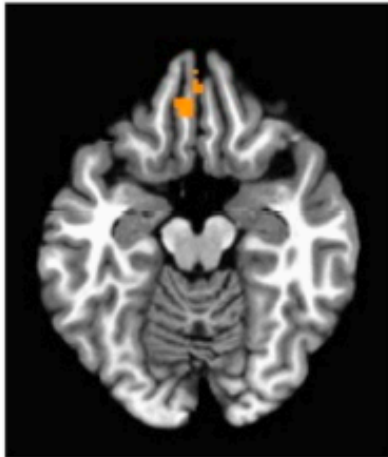
SAME holds with empirical data

Basic Model

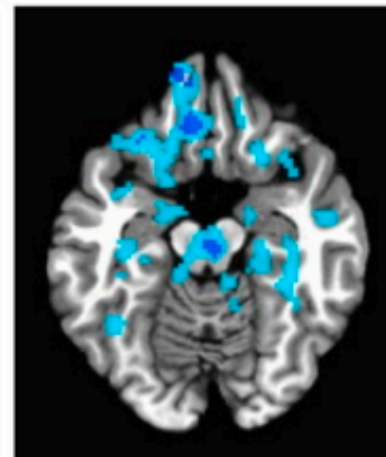
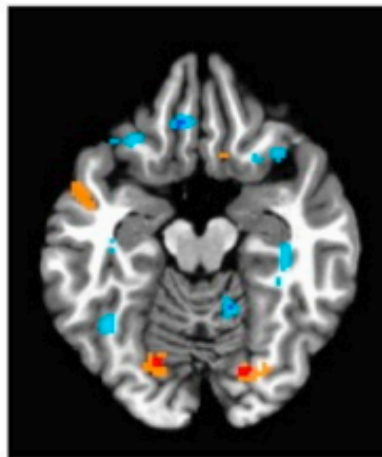
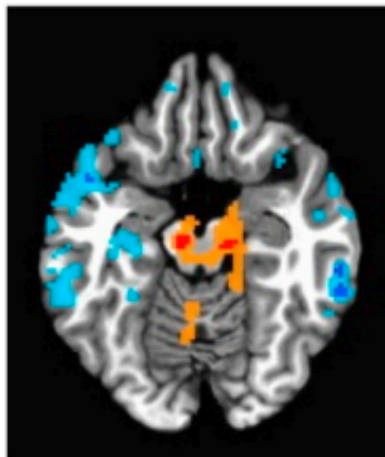
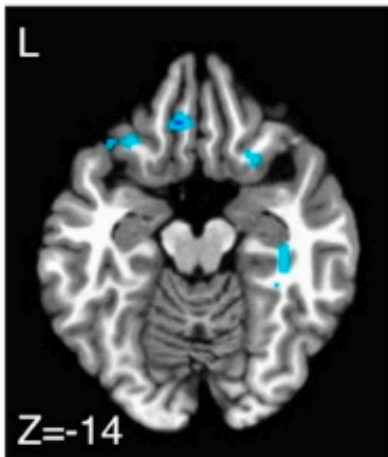
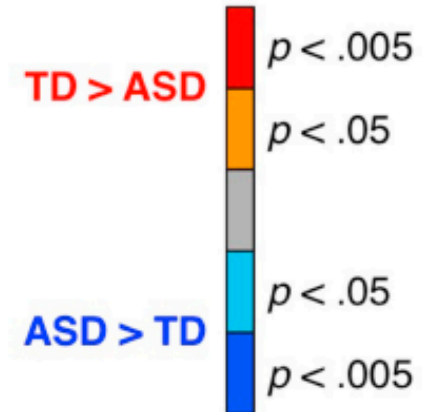
+ GS Regression

+ GCOR

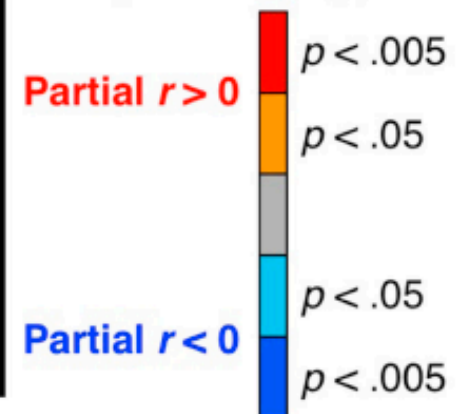
ANATICOR



Group *t*-tests



Correlation with SRS
(ASD Group)



(Gotts, 2013)

It is not just GSR

- Nuisance regressors **correlated with fluctuations of interest** in regions of interest (not the noise) can cause the same problems.
- Non-gray matter averages may be comparable to GSRreg (partial voluming with gray matter)
 - Averaging over small regions of eroded non-gray matter tissue is advantageous (Jo, 2010, 2013)
- Decomposition methods that cannot separate BOLD (fluctuations of interest) from noise also problematic.

There is some denoising with GSR

What of results being more stable after GSR?

There is a denoising component to the approach and bias is consistent for consistent covariance structure

- However, interpretation of correlations is now difficult (Cole, 2010)
- Interaction effect with grouping variable completely ignored
- Differences can get spread in unknown ways
- Tests of processing methods should always **consider group comparisons**

What of GSReg for motion compensation?

Some denoising effect → reducing residual variance and motion-based group differences

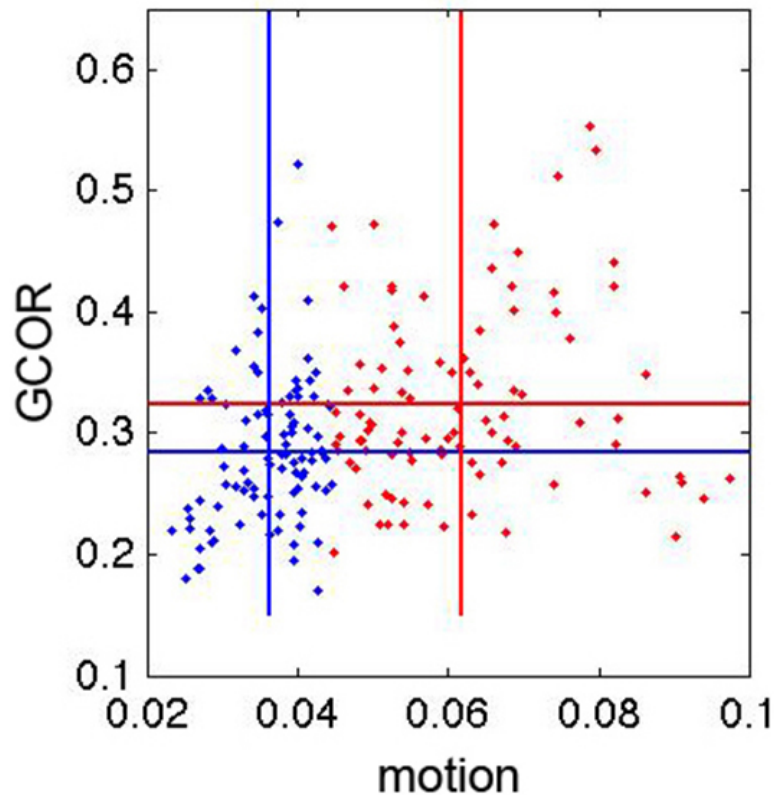
However, caveats from above remain

AND are we actually compensating for motion?

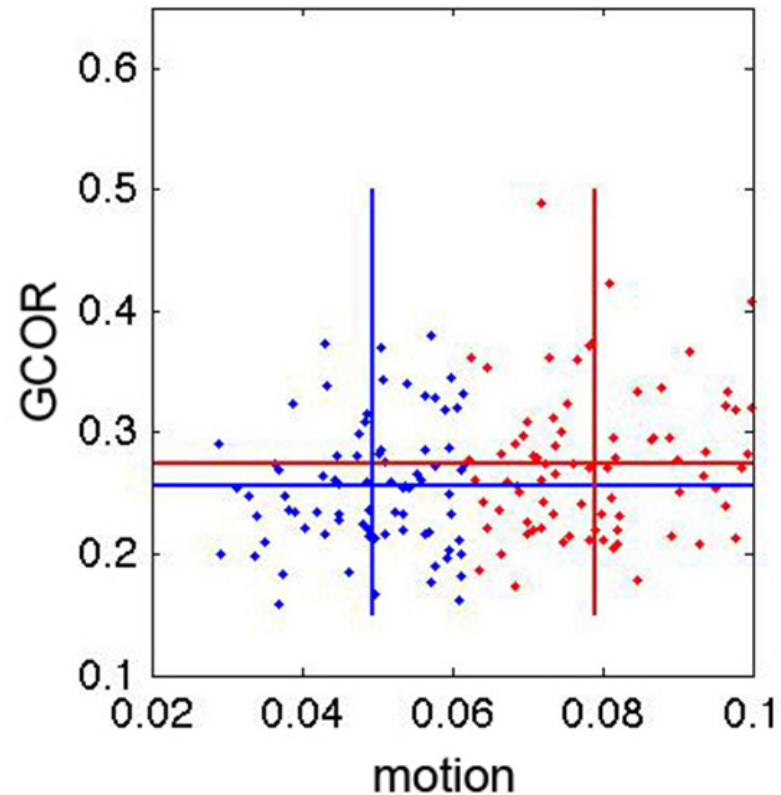
Grouping Based on Motion

Mean Motion
Small Movers
↓

Mean Motion
Big Movers
↓



FCON 1000: Cambridge_Buckner



FCON 1000: Beijing_Zang

Note weak correlation between motion and GCOR ($R^2=11\%$ Cambridge, 4.3% Beijing)

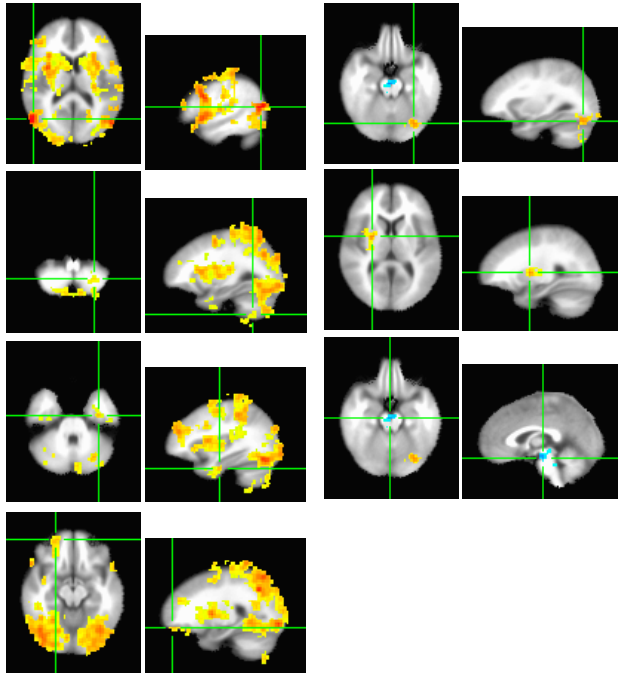
Grouping Based on Motion

FCON 1000: Cambridge_Buckner

β_1 Base

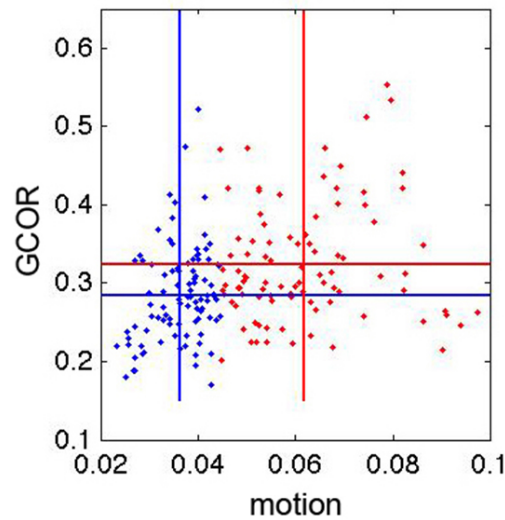
β_1 GSReg

Largest 4 Clusters



4 clusters

3 clusters

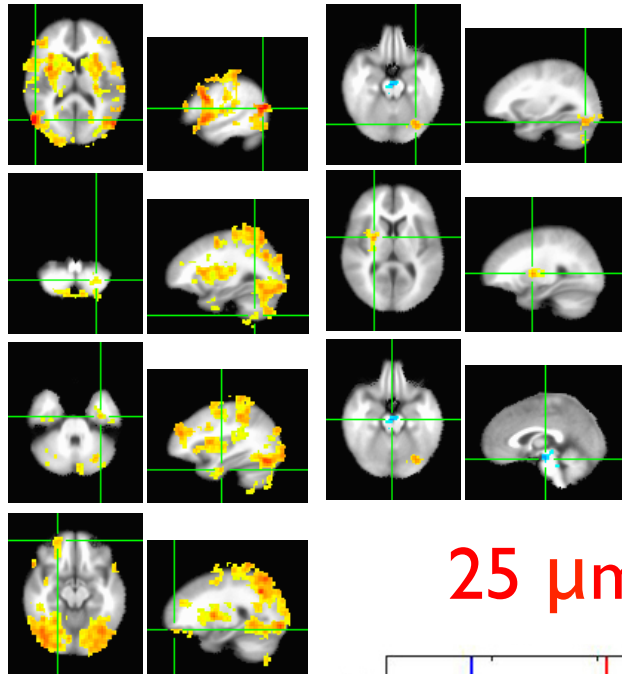


Grouping Based on Motion

FCON 1000: Cambridge_Buckner

β_1 Base

β_1 GSReg



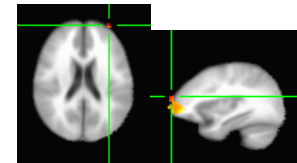
Largest 4 Clusters

4 clusters

FCON 1000: Beijing_Zang

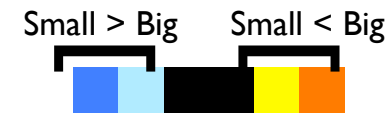
β_1 Base

β_1 GSReg



1 cluster

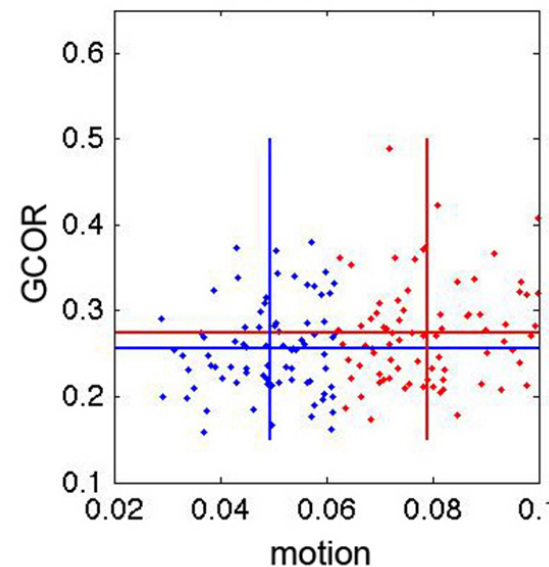
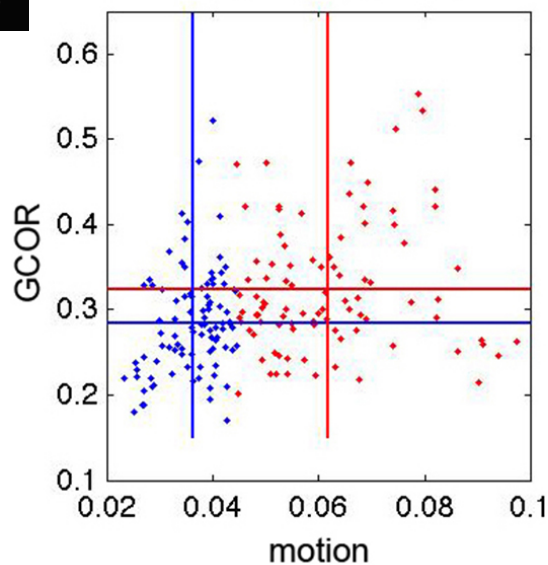
0 clusters



Group Difference, $p < 0.01$, $\alpha = 0.05$

25 $\mu\text{m}/\text{TR}$

29 $\mu\text{m}/\text{TR}$



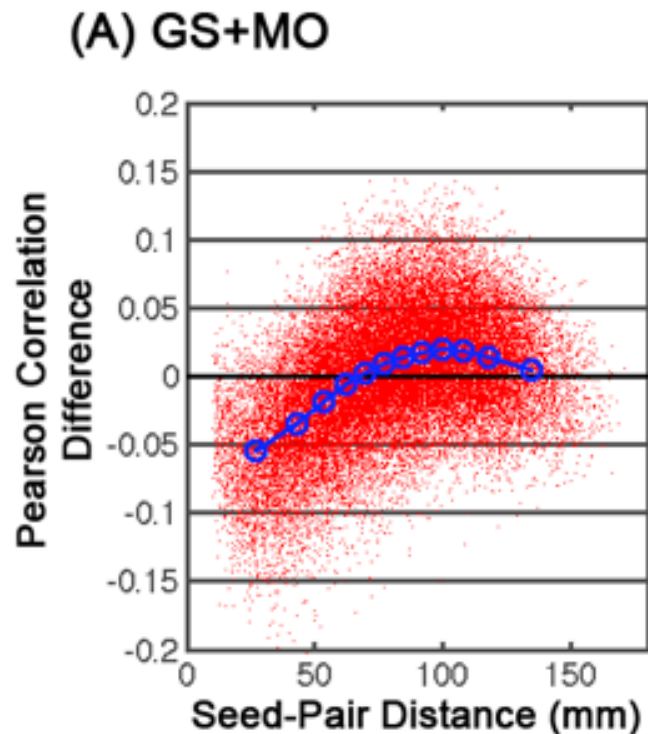
Can GSReg help with motion?

Censoring (scrubbing) high motion samples changes inter-regional correlations in distance dependent manner.

→ suggests effect of motion on correlations depends on distance between regions (Power et al. 2012)

→ importance of censoring high motion

Data generously made public by Power et al.



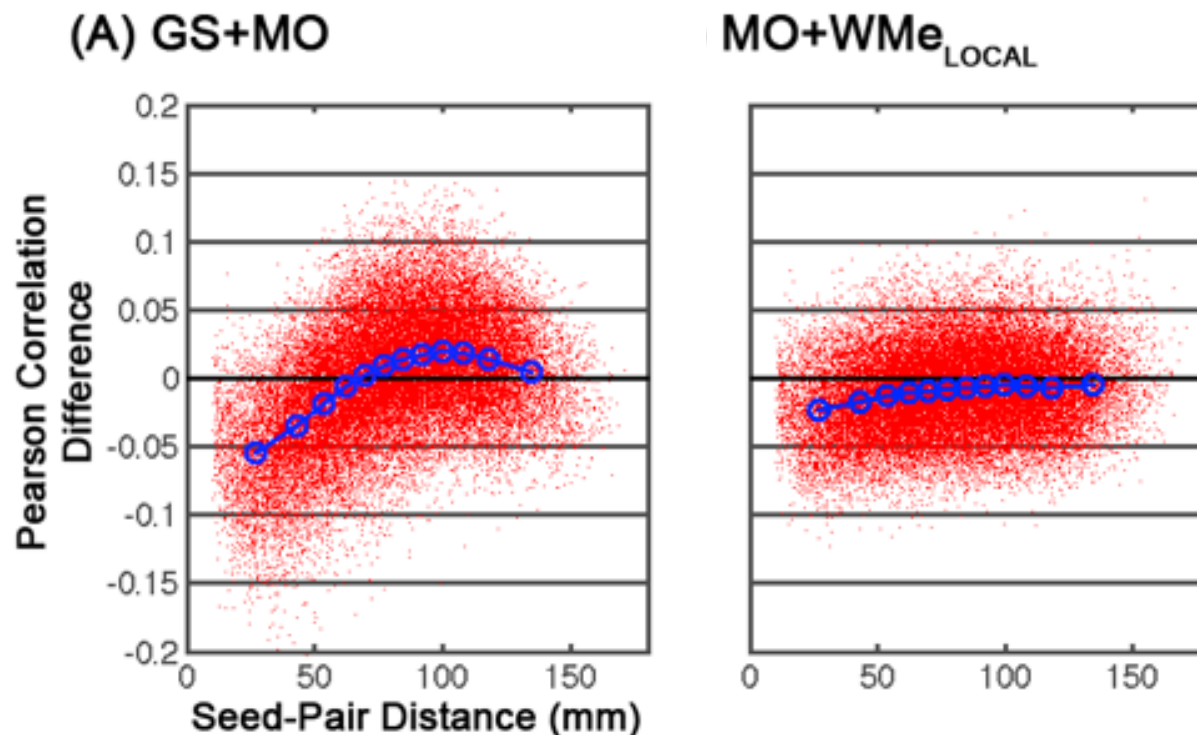
Can GSRreg help with motion?

Censoring (scrubbing) samples of high motion changes inter-regional correlations in a distance manner.

→ suggests effect of motion on correlations depends on distance between regions (Power et al. 2012)

→ importance of censoring high motion

Less dependence without GSRreg



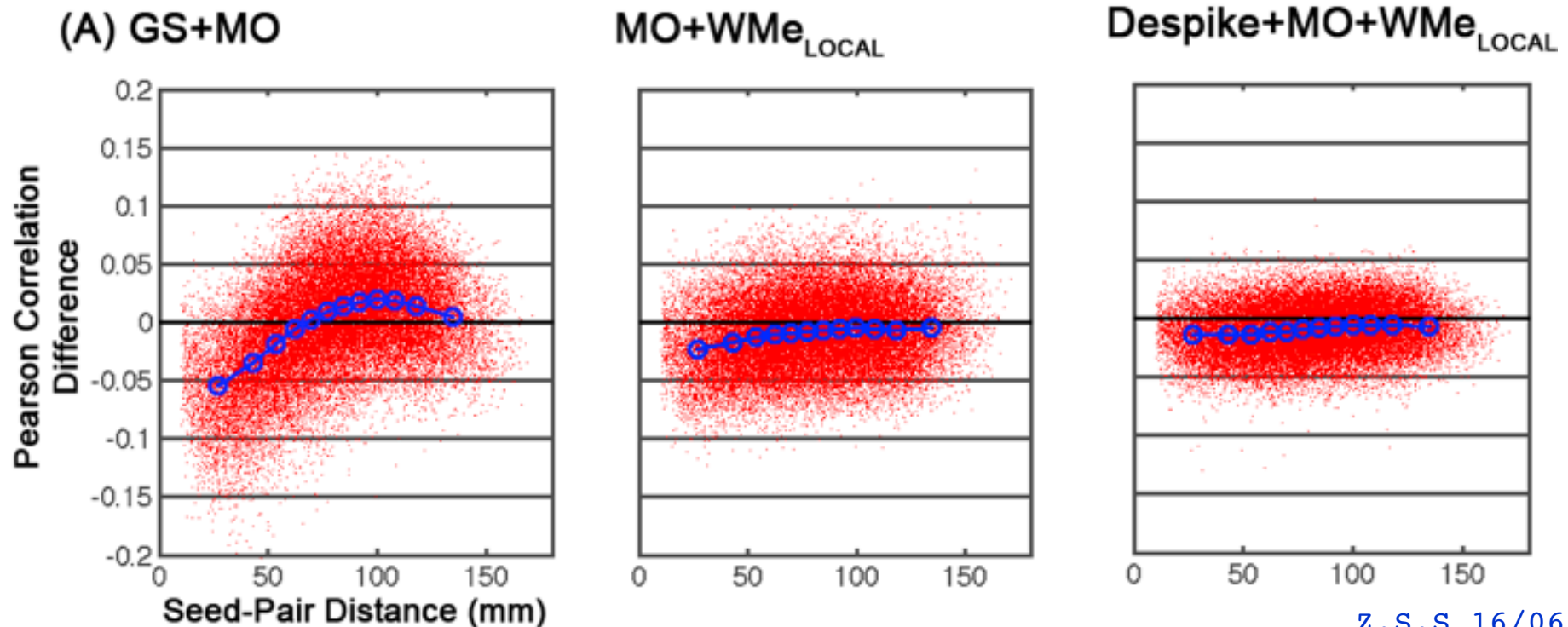
Can GSReg help with motion?

Censoring (scrubbing) samples of high motion changes inter-regional correlations in a distance manner.

→ suggests effect of motion on correlations depends on distance between regions (Power et al. 2012)

→ importance of censoring high motion

Least dependence

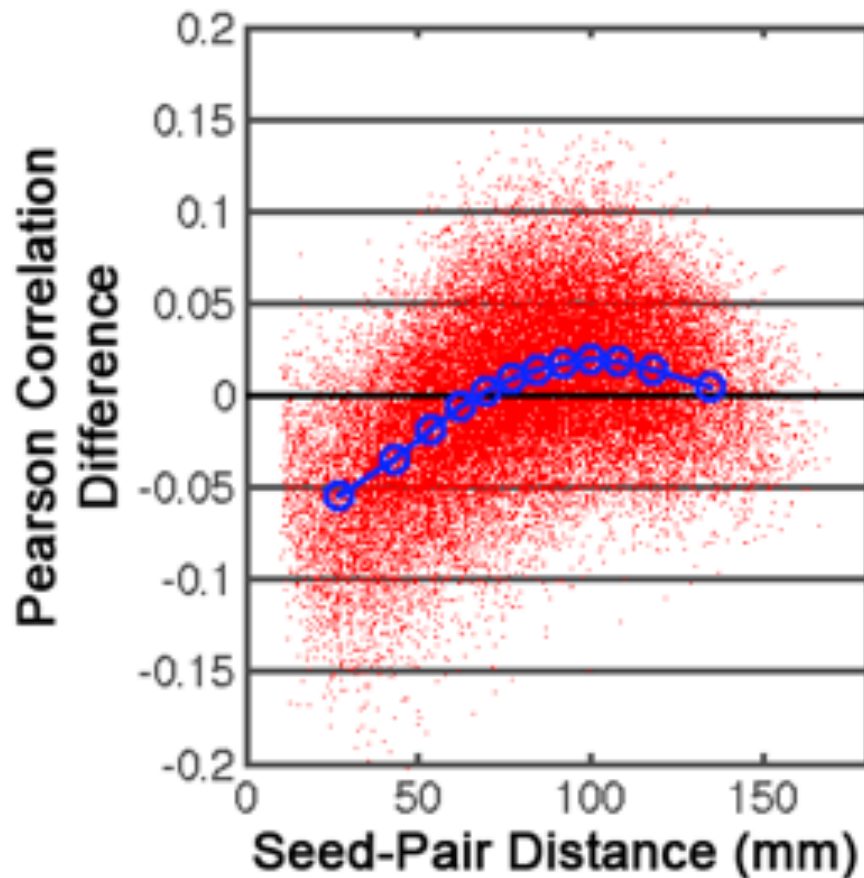


Can GSReg help with motion?

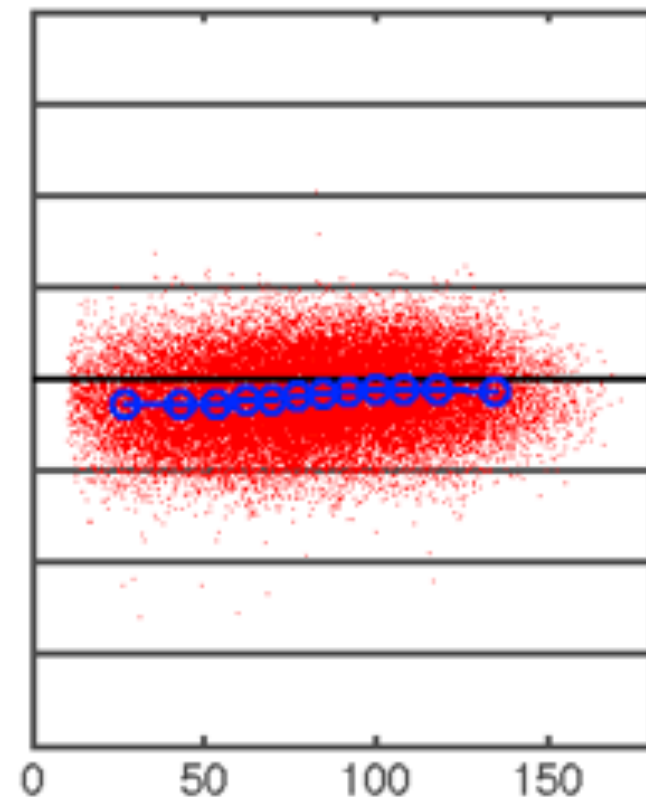
- GSReg → Correlation more sensitive to motion
- Correlation more sensitive to censoring (Jo, 2013)

Improved denoising largely eliminates distance dependent bias

(A) GS+MO



Despike+MO+WMe_{LOCAL}



Sampling nuisance TS regressors

- Sample noise without aggregating over regions with fluctuations of interest
 - Erode white matter masks to avoid partial voluming
 - Avoiding regions with fluctuations of interest (Anderson 2011)
 - Local eroded white matter masks improve denoising without increasing DOFs (Jo, 2010, 2013)
- Use decomposition methods that can separate BOLD from non BOLD fluctuations of interest (Kundu, 2012, Bright, 2013)
or attempt to identify noise components (Beckmann 2004, Beall 2010, Boubela, 2013)
- Use noise models RICOR/RVT/etc. (Glover 2000; Shmueli 2007; Birn 2008; Chang 2009)

Brain-wide correlation adjustments?

- If subject to subject variations in brain-wide correlations exist, why not correct for them?
- Consider GCOR, the average over the entire correlation matrix of every voxel with every other voxel (Saad, 2013)
 - Measure would be costly to compute if one had to estimate the entire correlation matrix first.
 - However estimating GCOR is trivial:

$$\begin{aligned}\gamma &= 1/(M^2 N) \mathbf{1}^T \mathbf{U}^T \mathbf{U} \mathbf{1} \\ &= 1/N \mathbf{g}_u^T \mathbf{g}_u,\end{aligned}$$

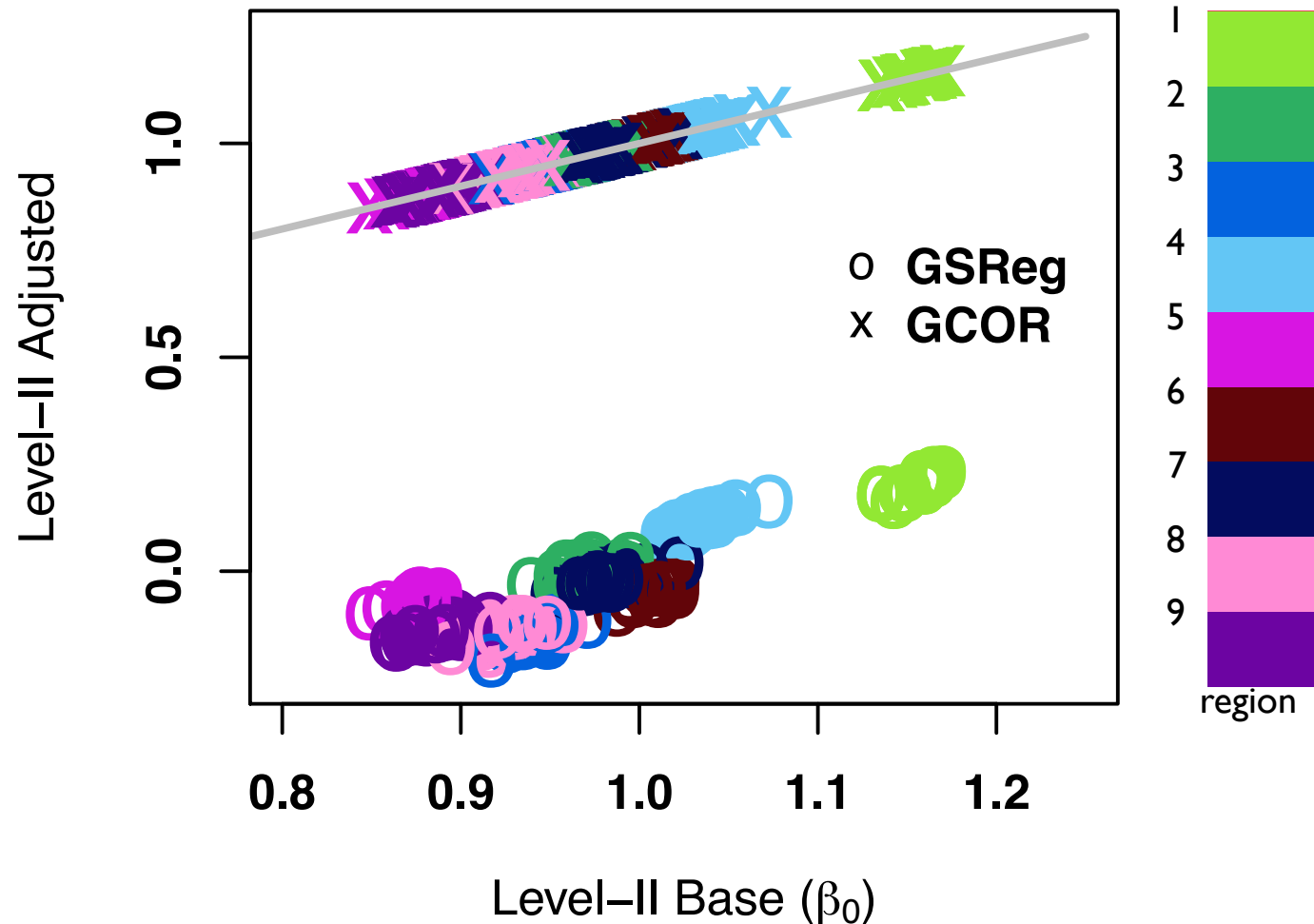
\mathbf{g}_u is the average of all (M) unit variance time series of length N in matrix \mathbf{U}

GCOR as group level covariate

- Using models described earlier, we consider group level correlation (differences) from three models:
 - No adjustment: $r_{i,j} = \beta_0 + \beta_1 x$
 - GSReg at level I: $s_{i,j} = \beta_0 + \beta_1 x$
 - GCOR as covariate: $r_{i,j} = \beta_0 + \beta_1 x + \beta_2 \gamma + \beta_3 x \gamma$

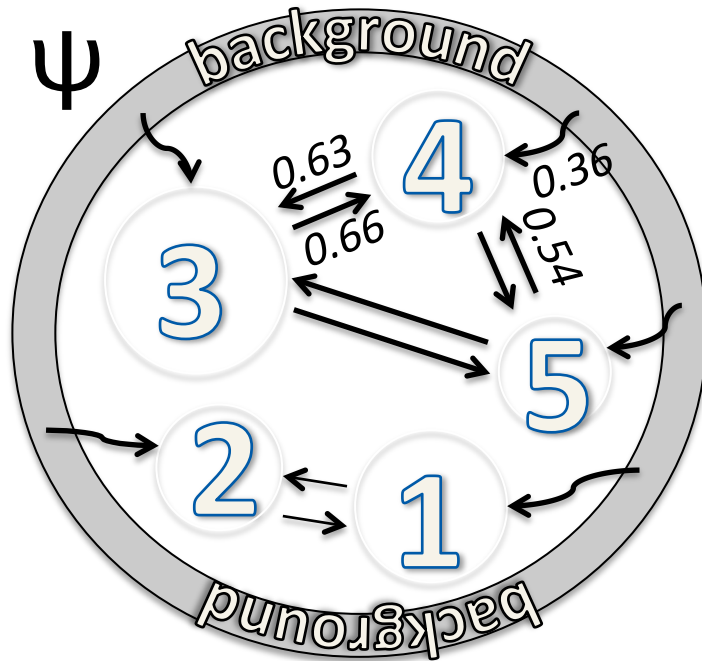
Less bias than with GSReg for 1 sample tests

Mean Correlations with Region 1

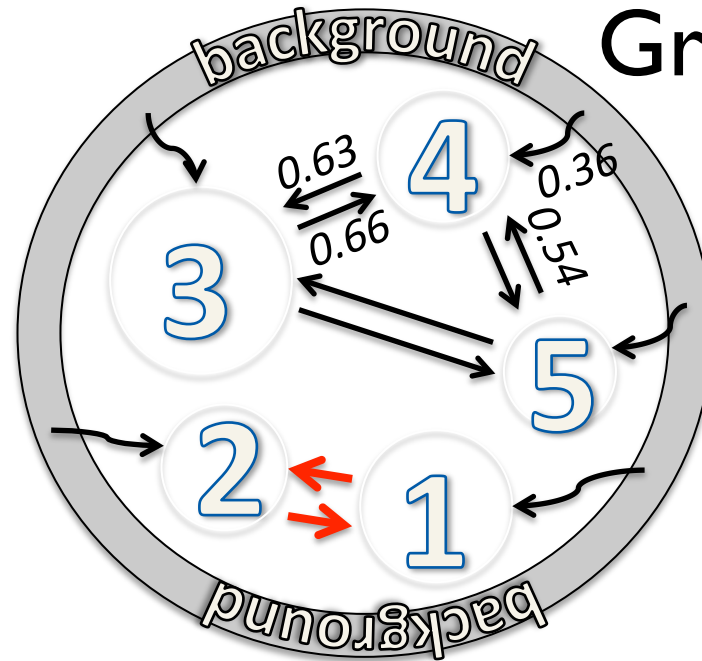


Comparing Groups

Group Ψ



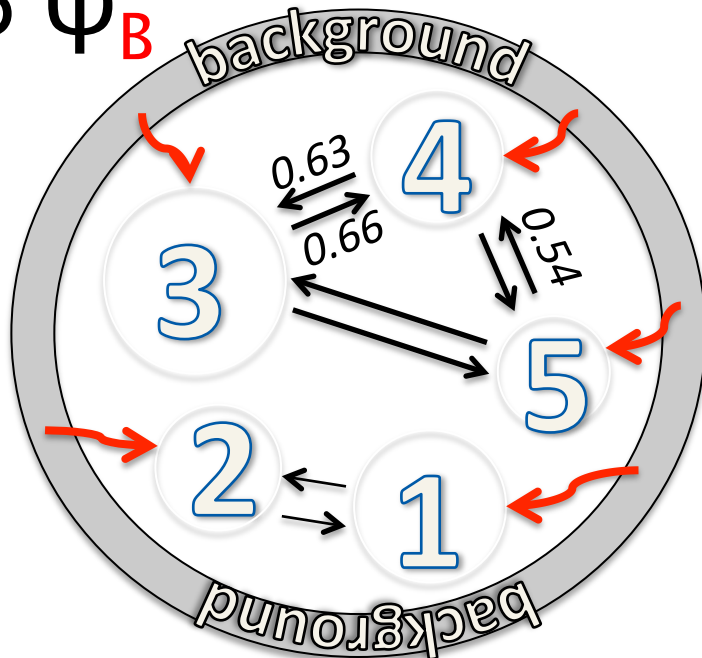
Group Ψ_L



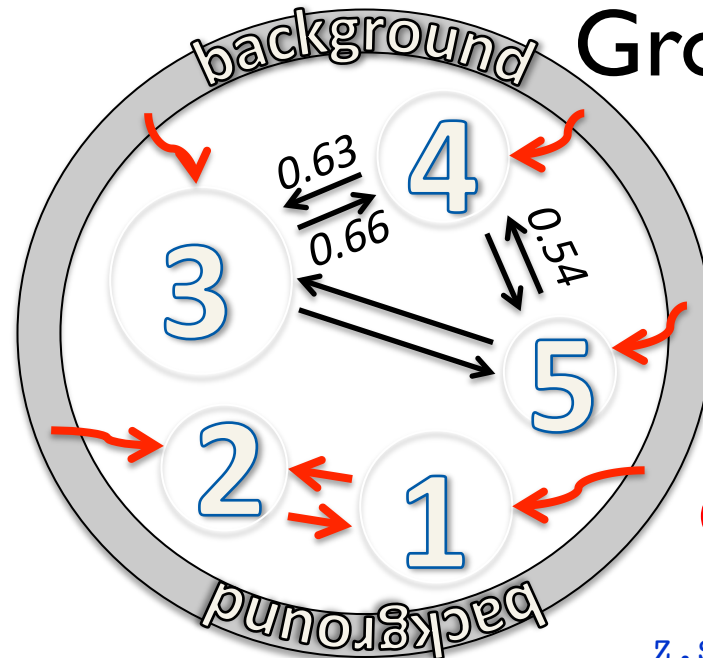
**More
Local**

Group Ψ_B

**More
Backg.**

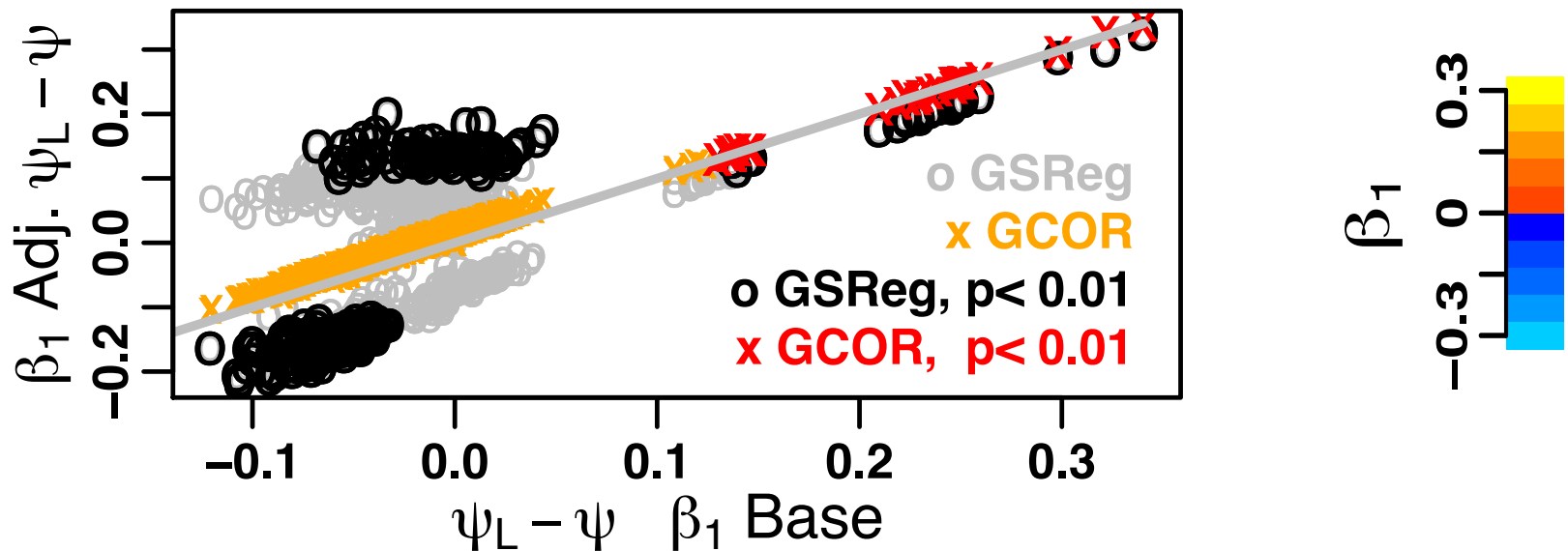
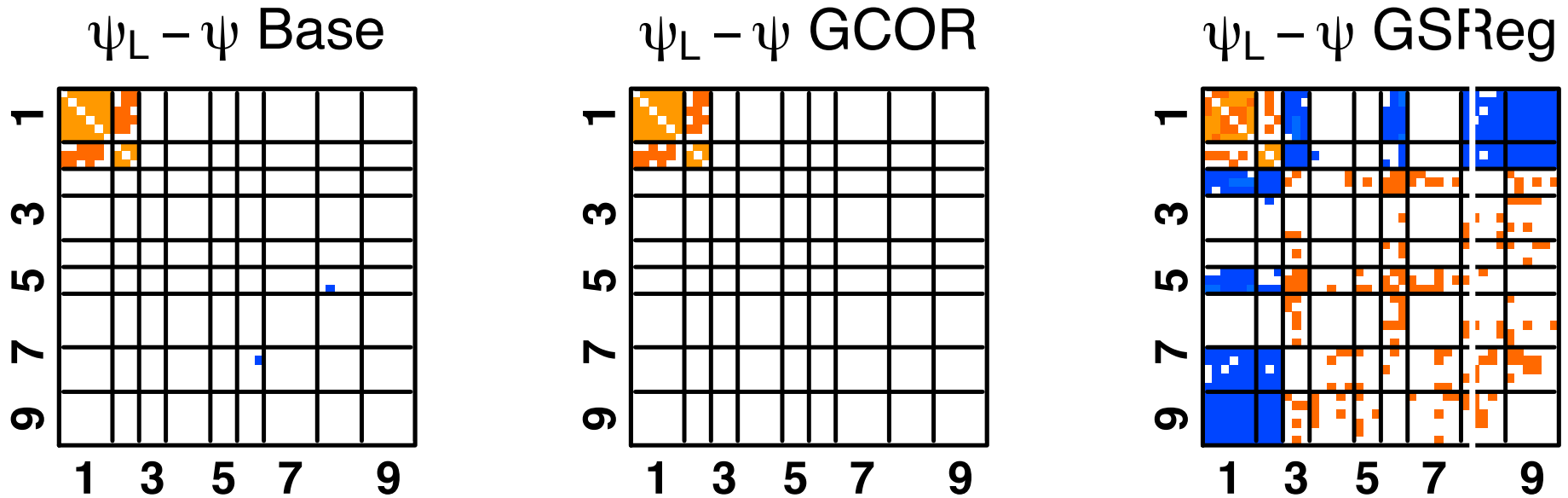


Group Ψ_{BL}

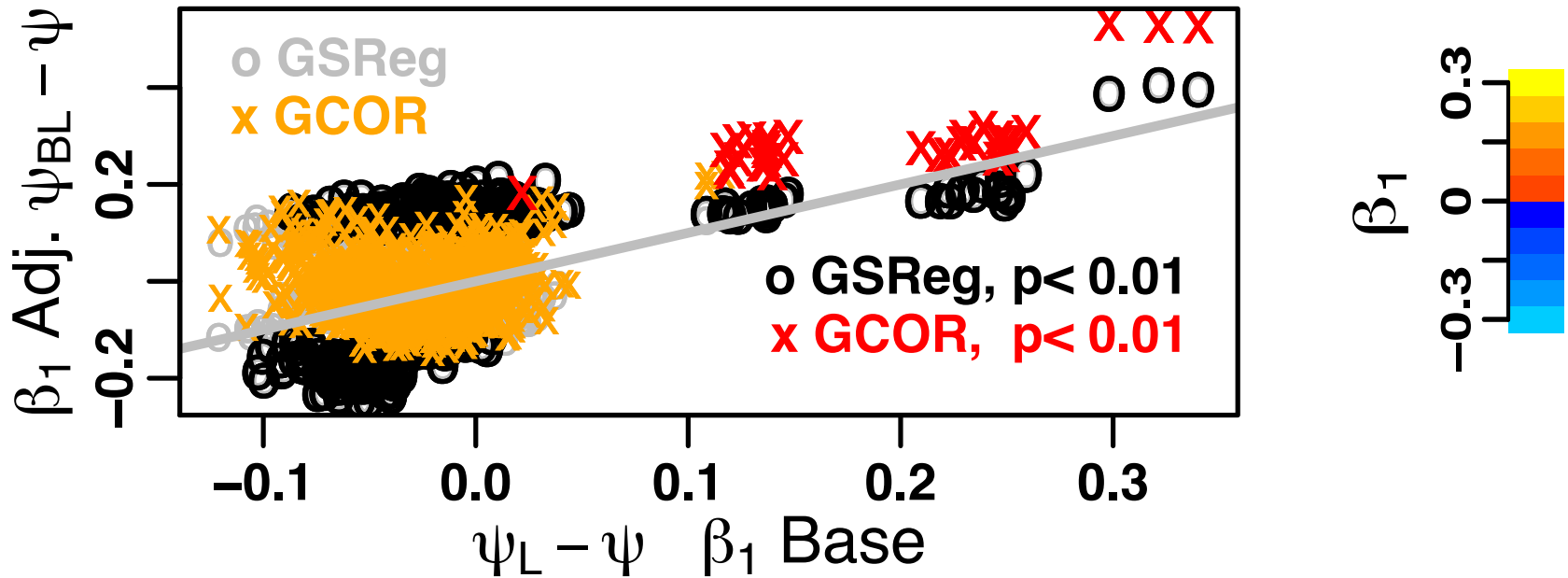
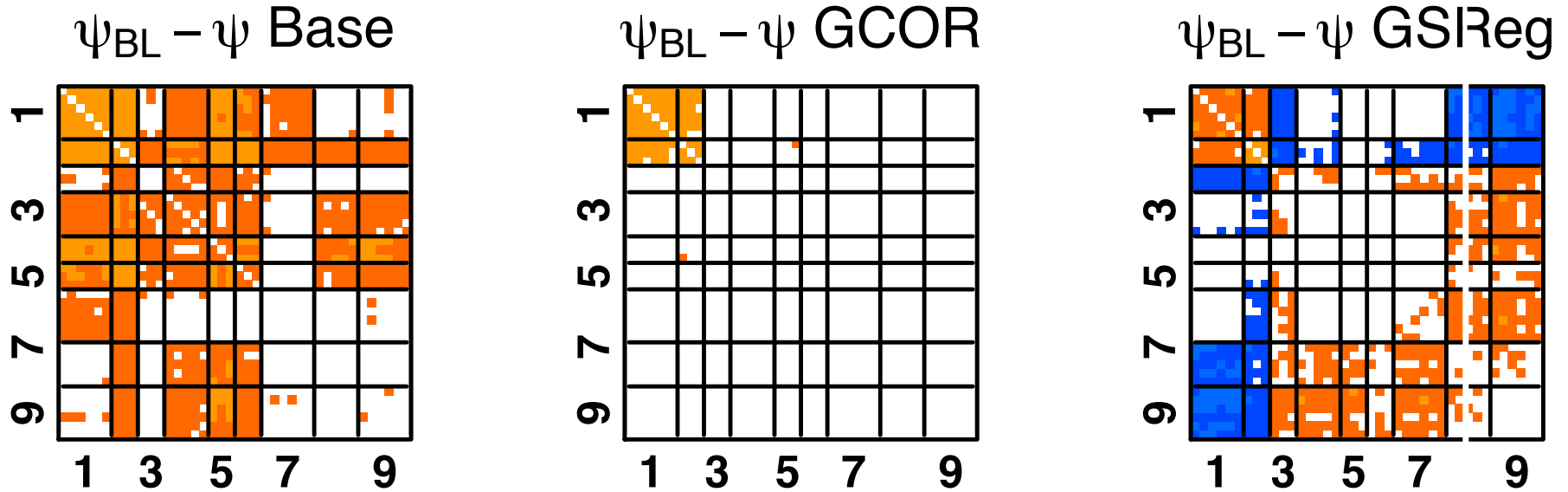


**More
Cowbell**

Group Contrast, Only Local Change



Group Contrast, Local & Backg. Change



GCOR and *Motion* Grouping

FCOR 1000: Cambridge_Buckner

β_1 Base

β_1 GSReg

β_1 GCOR

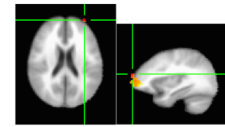
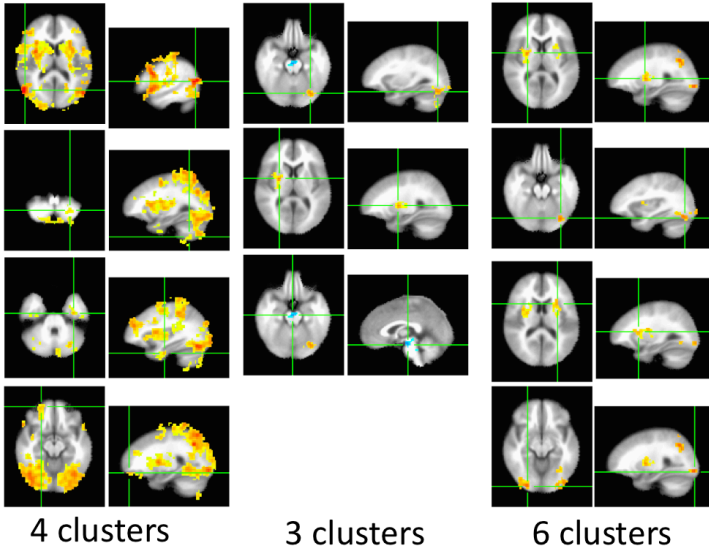
FCOR 1000: Beijing_Zang

β_1 Base

β_1 GSReg

β_1 GCOR

Largest 4 Clusters



(none)

0 cluster

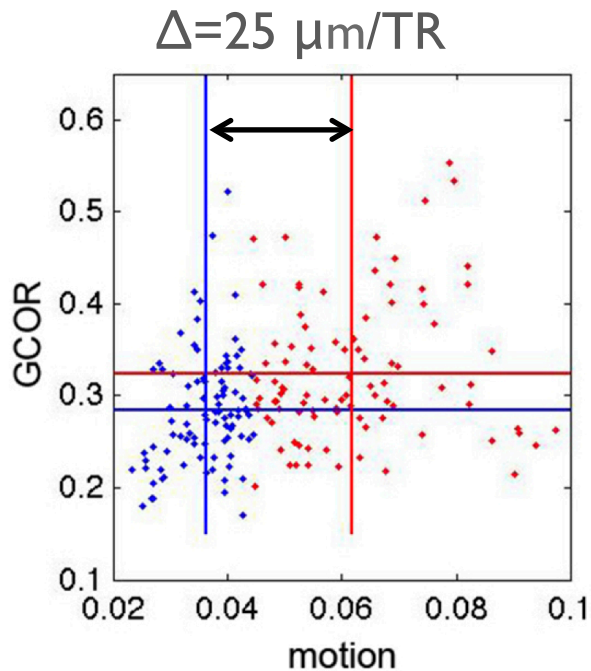
(none)

0 cluster

Small > Big Small < Big



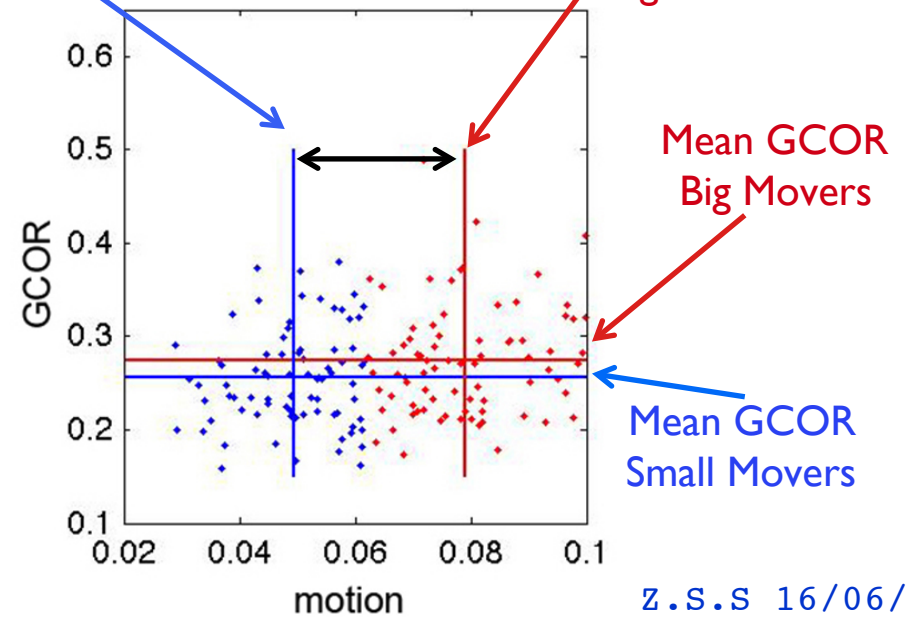
Group Difference, $p < 0.01$, $\alpha = 0.05$



Mean Motion
Small Movers

$\Delta = 29 \mu\text{m/TR}$

Mean Motion
Big Movers



GCOR as Group Level Covariate

Correlations less biased with GCOR, than GSReg.

- when GCOR has low correlation with grouping variable

Level-II tests conservative

- Less likely to detect difference as grouping variable and covariate correlation increases

Adjustment outside of level II test is NOT recommended

- There is always potential for **interaction effect with group**
- GCOR (and other params. (Yan 2013)) depend on noise AND/OR inter-regional correlations of interest
 - contrast results very likely depend on **covariate centering**
 - Centering at overall mean makes sense if GCOR is driven by noise.
 - What if it is also driven by correlations of interest?
 - contrast sign might even get reversed

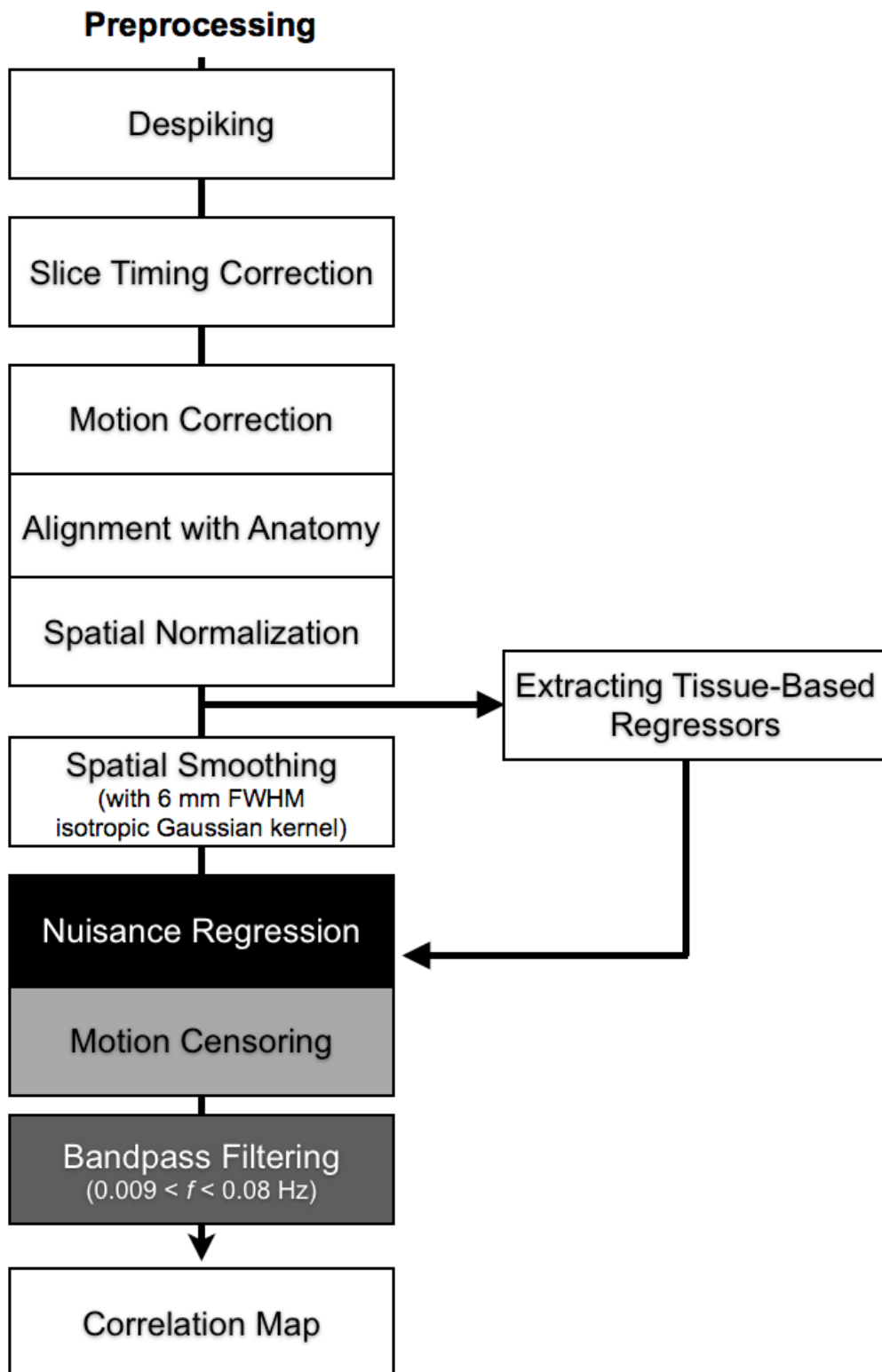
Conclusions for Global Corrections

- Stay away from regions with Fluctuations of Interest
- GSReg and its variants are problematic for group comparisons
- One MUST consider interactions of method with grouping variable
 - Generative models clarify matters since there is no base truth
- GCOR is very simple to compute and is useful to assess global correlation levels
- Use of GCOR and comparable measures is safer than GSReg
 - However, their interaction with grouping variable can confound interpretation

Use should be as last resort

- Use them as covariates and consider interaction terms
- Separate covariate modeling prior to level-II not recommended
- Risks of false negatives
- Centering issues

RS FMRI processing pipeline



Jo et al. 2013

Single-Subject RS-fMRI Processing

Generate Analysis Pipeline with *afni_proc.py*

```
afni_proc.py -subj_id subj123  
-dsets epi_run1+orig.HEAD  
-copy_anat anat+orig  
-blocks despike ricor tshift align  
          volreg blur regress  
-regress_anaticor  
-regress_censor_motion 0.2  
-regress_bandpass 0.01 0.1  
-ricor_regs RICOR/r*.slibase.1D
```

See *afni_proc.py -h_view* for more detailed examples,

Single-Subject RS-fMRI Processing

Generate Analysis Pipeline with *afni_proc.py*

```
afni_proc.py -subj_id subj123 ← Subject ID \
  -dsets epi_run1+orig.HEAD ← EPI timeseries \
  -copy_anat anat+orig ← Anatomical \
  -blocks despike ricor tshift align \
  volreg blur regress \
  -regress_anaticor \
  -regress_censor_motion 0.2 \
  -regress_bandpass 0.01 0.1 \
  -ricor_regs RICOR/r*.slibase.1D \
```

See *afni_proc.py -h_view* for more detailed examples,

Single-Subject RS-FMRI Processing

Generate Analysis Pipeline with *afni_proc.py*

```
afni_proc.py -subj_id subj123  
-dsets epi_run1+orig.HEAD  
-copy_anat anat+orig  
-blocks despike ricor tshift align  
          volreg blur regress ← Processing blocks  
-regress_anaticor      Use defaults or specify sequence  
-regress_censor_motion 0.2  
-regress_bandpass 0.01 0.1  
-ricor_regs RICOR/r*.slibase.1D
```

See *afni_proc.py -h_view* for more detailed examples,

Single-Subject RS-fMRI Processing

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-dsets epi_run1+orig.HEAD  
-copy_anat anat+orig  
-blocks despike ricor tshift align  
          volreg blur regress  
-regress_anaticor ← Use Local Eroded White Matter  
-regress_censor_motion for2denoising. (Jo et al. 2010)  
-regress_bandpass 0.01 0.1  
-ricor_regs RICOR/r*.slibase.1D
```

See *afni_proc.py -h_view* for more detailed examples,

Single-Subject RS-fMRI Processing

Generate Analysis Pipeline with *afni_proc.py*

```
afni_proc.py -subj_id subj123  
-dsets epi_run1+orig.HEAD  
-copy_anat anat+orig  
-blocks despike ricor tshift align  
          volreg blur regress  
-regress_anaticor  
-regress_censor_motion 0.2 ← Motion censoring  
-regress_bandpass 0.01 0.1 and bandpass filter  
-ricor_regs RICOR/r*.slibase.1D
```

See *afni_proc.py -h_view* for more detailed examples,

Single-Subject RS-fMRI Processing

Generate Analysis Pipeline with *afni_proc.py*

```
afni_proc.py -subj_id subj123
-dsets epi_run1+orig.HEAD
-copy_anat anat+orig
-blocks despike ricor tshift align
        volreg blur regress
-regress_anaticor
-regress_censor_motion 0.2
-regress_bandpass 0.01 0.1
-ricor_regs RICOR/r*.slibase.1D ← RICOR+RVT for
    respiration & cardiac denoising (Glover 2002, Birn 2006)
```

See *afni_proc.py -h_view* for more detailed examples,

Conclusions

The best approach remains with careful denoising

- motion parameter estimates
- physiological measurements
- local estimates of nuisance signals from eroded white matter
- denoising decompositions in as far as they can dissociate nuisance estimates from signal fluctuations of interest

Look at your data, one subject at a time!

Acknowledgments

Robert Cox
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Rick Reynolds

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Catie Chang
Carlton Chu

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for releasing data

