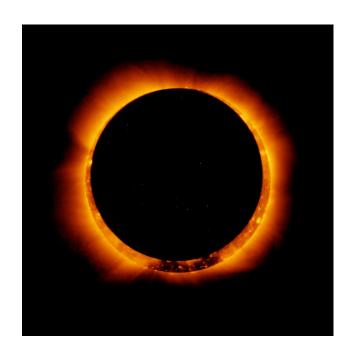
Alignment and Atlases





What does aligning mean and why do we want to do it?

- Alignment means to bring two objects into the same space so that each location within one object corresponds to the same location in the other
- Why?
 - motion correction across time
 - align EPI to anatomical data or vice versa to assign a location with a functional result
 - compare data from longitudinal studies
 - compare data from different scanners, sites
 - compare results with a standard template or atlas for standardized locations and structures

Alignment goals and tools in AFNI

- EPI data across time in a single run or across runs to a base image
 - 3dvolreg motion correction (rigid)
- Align data to template
 - 3dWarpDrive, @auto_tlrc align similar volumes (affine) even across subjects
 - 3dQwarp, auto_warp.py align similar volumes <u>nonlinearly</u> to template
- Align images across modalities EPI to anat
 - 3dAllineate align different or similar volumes
 - align_epi_anat.py general alignment script to align EPI with anatomical data
- Include motion correction, alignment of EPI to anatomical in fMRI processing pipeline script
 - afni_proc.py
- Correct for motion between two volumes by aligning in two dimensions using corresponding slices
 - ♦ @2dwarper.Allin non-linear alignment of slices
 - @2dwarper, 2dimreg limit alignment to specific plane

Alignment tools in AFNI (continued)

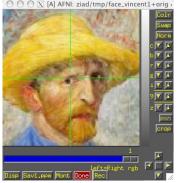
- Align partial data to roughly the right part of the brain
- Nudge plug-in visually align two volumes
- rotate by known amount between volumes
- 3drotate moves (shifts and rotates) volumes
- ♦ 3dWarp make oblique, deoblique to match another dataset
- Put centers of data from outside sources in roughly the same space
- @Align_Centers, 3dCM put centers or centers of mass of dataset in same place
- align specific regions across subjects
- 3dTagalign, tagset plugin place and align volumes using corresponding fiducial marker points
- align one jpeg image to another
- imreg align two 2D images

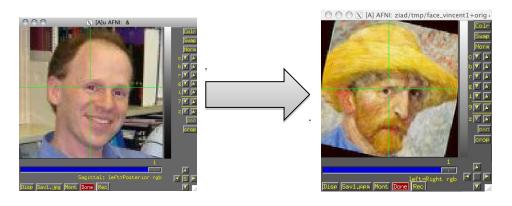
Image and Volume Registration with AFNI

- Goal: bring images collected with different methods and at different times into spatial alignment
- Facilitates comparison of data on a voxel-by-voxel basis
 - Functional time series data will be less contaminated by artifacts due to subject movement
 - Can compare results across scanning sessions once images are properly registered
 - Can put volumes in standard space such as the stereotaxic Talairach-Tournoux coordinates
- Most (all?) image registration methods now in use do pair-wise alignment:
 - Given a base image J(x) and target (or source) image I(x), find a geometrical transformation T[x] so that I(T[x]) ≈ J(x)
 - T[x] will depend on some parameters
 - Goal is to find the parameters that make the transformed I a 'best fit' to J
 - ♦ To register an entire time series, each volume $I_n(x)$ is aligned to J(x) with its own transformation $T_n[x]$, for n=0, 1, ...
 - \rightarrow Result is time series $I_n(T_n[x])$ for n=0, 1, ...
 - User must choose base image J(x)

- Most image registration methods make 3 algorithmic choices:
 - ♦ How to measure mismatch E (for error) between I(T[x]) and J(x)?
 - → Or ... How to measure goodness of fit between I(T[x]) and J(x)?
 - ♦ How to adjust parameters of T[x] to minimize E?
 - How to interpolate I(T[x]) to the J(x) grid?
 - So we can compare voxel intensities directly
- The input volume is transformed by the optimal **T[x]** and a record of the transform is kept in the header of the output.
- Finding the transform to minimize E is the bulk of the registration work. Applying the transform is easy and is done on the fly in many cases.
- If data starts off far from each other, may add a coarse pass (twopass) step
 - guess a lot among all the parameters (rotations, shifts, ...), measure cost
 - best guesses, tweak the parameters (optimize) and measure again

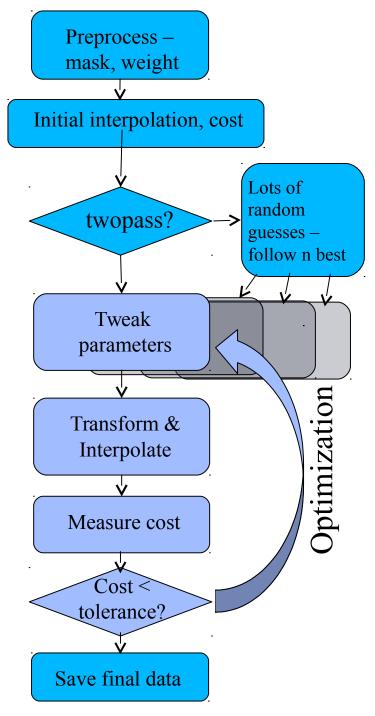
Now, applications of alignment...



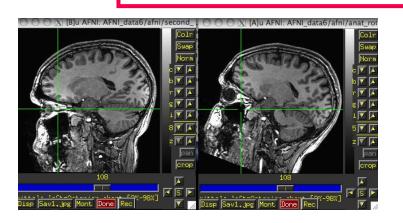


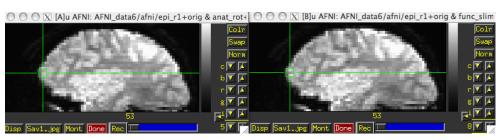
Alignment process - overview

- Preprocess mask data, weight data
- If far off, take some random guesses (-twopass)
- Optimize parameters on initial or best sets (6,12,39,1000's)
 - Use new parameters to transform input
 - Interpolate onto base data's grid
 - Measure alignment error with cost functional
 - Less than minimum error finished
 - Better keep adjusting with same direction
 - Worse try other parameters
- Create final output by interpolating onto output grid
 - save datasets, transform parameters



Within Modality Registration





- AFNI <u>3dvolreg</u> and <u>3dWarpDrive</u> programs match images by grayscale (intensity) values
 - ♦ E = (weighted) sum of squares differences = $\sum_{x} w(x) \cdot \{I(T[x]) J(x)\}^2$
 - Only useful for registering 'like images':
 - □ Good for SPGR↔SPGR, EPI↔EPI, but not good for SPGR↔EPI
 - Several interpolation methods :
 - → Fourier, linear, cubic, quintic, and heptic polynomials
 - ♦ <u>3dvolreg</u> is designed to run VERY fast for EPI↔EPI registration with small movements good for FMRI purposes but restricted to 6-parameter rigid-body transformations.
 - <u>3dWarpDrive</u> is slower, but it allows for up to 12 parameters affine transformation. This corrects for scaling and shearing differences in addition to the rigid body transformations.

Looking for Motion

afni GUI – graph-image video/ricochet, arrow keys. Graph spikes.

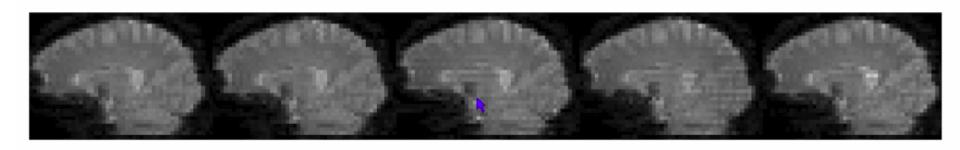


Image courtesy of Jonathan Power, NIMH

In statistical results, "activation" / "deactivation" occurs at high contrast boundaries like edge of brain or ventricles.

- AFNI program 3dvolreg is for aligning 3D volumes by rigid movements
 - T[x] has 6 parameters:
 - ➤ Shifts along x-, y-, and z-axes; Rotations about x-, y-, and z-axes
 - Generically useful for intra- and inter-session alignment
 - Motions that occur within a single TR (2-3 s) cannot be corrected this way, since method assumes rigid movement of the entire volume
- AFNI program <u>3dWarpDrive</u> is for aligning 3D volumes by affine transformations
 - T[x] has up to 12 parameters:
 - \rightarrow Same as <u>3dvolreg</u> plus 3 Scales and 3 Shears along x-, y-, and z-axes
 - Generically useful for intra- and inter-session alignment
 - Generically useful for intra- and inter-subject alignment
 - AFNI program 2dImReg is for aligning 2D slices
 - ♦ T[x] has 3 parameters for each slice in volume:
 - Shift along x-, y-axes; Rotation about z-axis
 - ➤ No out of slice plane shifts or rotations!
 - Useful for sagittal EPI scans where dominant subject movement is 'nodding' motion that may be faster than TR
 - It is possible and sometimes even useful to run 2dImReg to clean up sagittal nodding motion, followed by 3dvolreg to deal with out-of-slice motion

• Intra-session registration example:

```
3dvolreg -base 4 -heptic -zpad 4 \
-prefix fred1_epi_vr \
-1Dfile fred1_vr_dfile.1D \
fred1_epi+orig 
Input dataset name
```

- → base 4 ⇒ Selects sub-brick #4 of dataset fred1_epi+orig as base image J(x)
- → heptic ⇒ Use 7th order polynomial interpolation
- → zpad 4 ⇒ Pad each target image, I(x), with layers of zero voxels 4 deep on each face prior to shift/rotation, then strip them off afterwards (before output)
 - → Zero padding is particularly desirable for -Fourier interpolation
 - → also good for large rotations, some data may get 'lost' if no zero padding
- → -1Dfile fred1_vr_dfile.1D ⇒ Save estimated movement parameters into a 1D (i.e., text) file with the given name
 - → Movement parameters can be plotted with the 1dplot command and used later....

```
Try this (in AFNI_data6/afni):

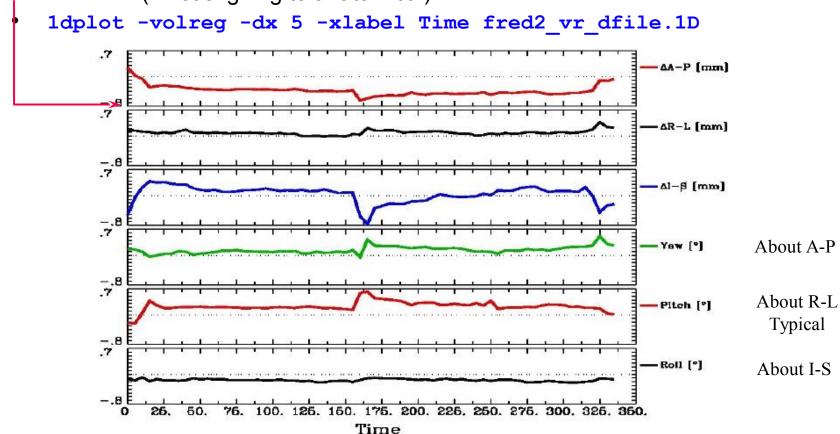
3dvolreg -base 3 -cubic -prefix epi_r1_vrt -1Dfile vr_dfile.1D epi_r1+orig

1dplot -volreg vr_dfile.1D &
```

-12- ♦ Can now register second dataset from same session:

```
3dvolreg -base 'fred1_epi+orig[4]' -heptic -zpad 4 \
    -prefix fred2_epi_vr -1Dfile fred2_vr_dfile.1D \
    fred2_epi+orig
```

- Note base is from different dataset (fred1_epi+orig) than input (fred2_epi+orig)
 - Aligning all EPI volumes from session to EPI closest in time to SPGR (if not aligning to anatomical)



Note motion peaks at time ≈ 160s: subject jerked head up at that time

"Fixing Motion"

- Motion occurs over slices and not volumes and moves data off original grid
- "Regressing out" motion parameters, derivatives, displacement, euclidean norm of derivatives (summary parameters)
- Censoring ("scrubbing", "sweeping under the mat",...)
- Experimental design kids, monkeys, juice, talking, waving hands wildly....
- Interpreting results differences in motion between groups or something physiological
- Notice activation following high contrast borders, "blinds" effects

```
Try this (in AFNI_data6/afni):

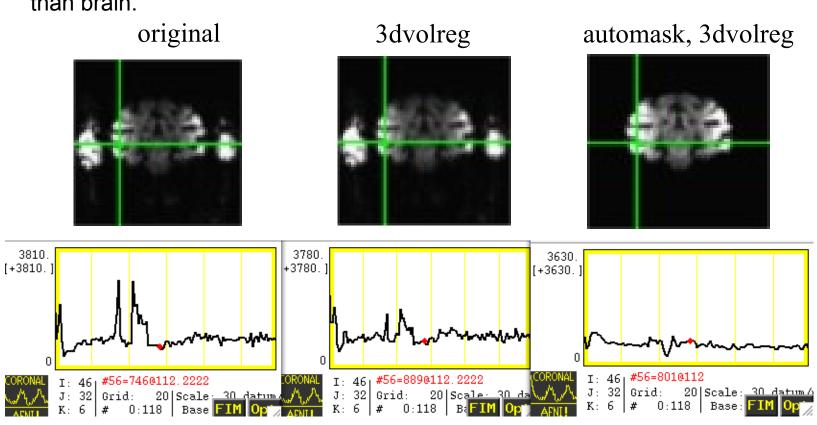
1d_tool.py -infile vr_dfile.1D -set_nruns 1 -censor_motion 1 ett

1dplot ett_enorm.1D &

cat ett CENSORTR.txt
```

Motion correction – caveats

- Motion is usually not completely correctable, so set motion parameters as regressors of no interest. Interpolation generally blurs data and depends on method and grid/resolution of EPI.
- Check in the AFNI GUI to be sure the data is not bouncing around after correction
- Example Monkey sips juice at stimulus time, and large jaw muscles move. If the muscles are not masked, then motion correction may track muscles rather than brain.



Cross Modality Registration

- 3dAllineate can be used to align images from different methods
 - For example, to align EPI data to SPGR / MPRAGE:
 - ► Run 3dSkullStrip on the SPGR dataset so that it will be more like the EPI dataset (which will have the skull fat suppressed)
 - Use 3dAllineate to align the EPI volume(s) to the skull-stripped SPGR volume
 - → Program works well if the EPI volume covers most of the brain
 - Allows more general spatial transformations affine, bilinear, non-linear (polynomial warping)
- 3dAllineate has several different "cost" functions (E) available

```
$ leastsq = Least Squares (3dvolreg, 3dWarpDrive)
```

- mutualinfo = Mutual Information
- orm_mutualinfo = Normalized Mutual Information
- hellinger = Hellinger Metric [the default cost function]
- corrratio mul = Correlation ratio (symmetrized by multiplication)
- corratio add = Correlation ratio (symmetrized by addition)
- corratio_uns = Correlation ratio (unsymmetric)
 - lpc = Local Pearson Correlation (negative)
 - 1pa = Local Pearson Correlation (absolute value)

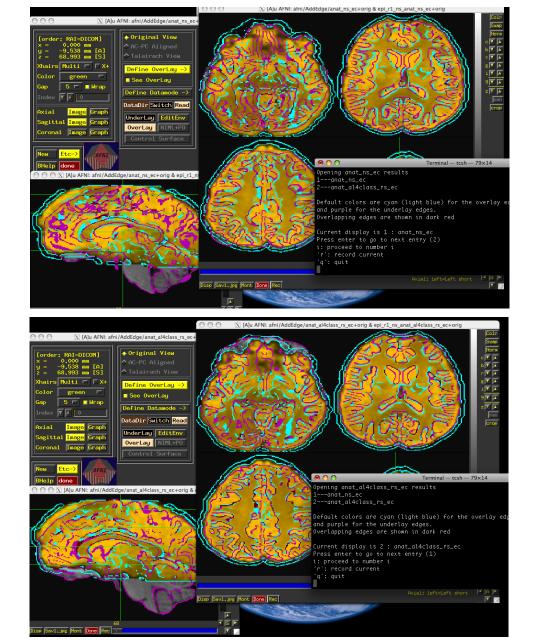
align_epi_anat.py

- Goal: Want to align anat and EPI (anat to EPI or EPI to anat or dset1to2 or dset2to1)
- LPC method Local Pearson Correlation to match dark CSF in anatomical data with bright CSF in EPI data.
- align_epi_anat.py script preprocessing and calls 3dAllineate for alignment
- @AddEdge for visualization
- Simple Example:

```
align_epi_anat.py -anat anat+orig \
-epi epi_r1+orig \
-AddEdge -epi_base 0 -suffix _al4class
cd AddEdge
afni -niml -yesplugouts &

@AddEdge
```

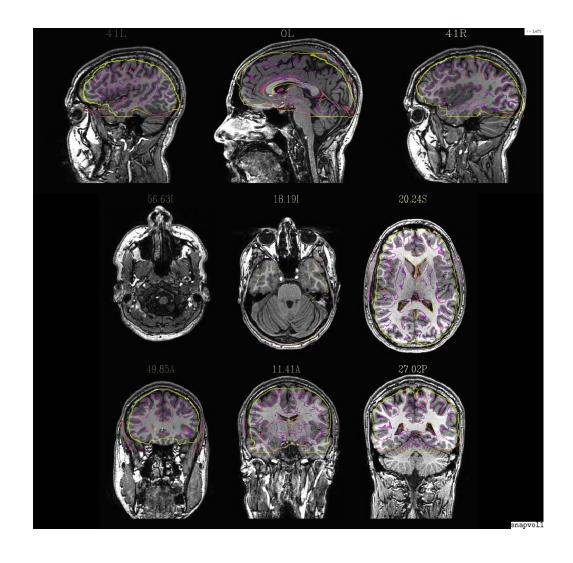
Combines deoblique, motion correction, alignment and talairach transformations into a single transformation. Also performs slice timing correction and applies transformations to "child" datasets.



@AddEdge display

Before

After



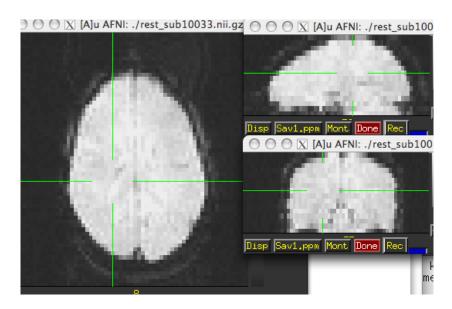
@snapshot_volreg anat+orig. epi_r1+orig edges.jpg
aiv edges.jpg

Alignment Visualization in AFNI

- Graph and image travel through time for motion correction or for a thousand datasets in a row.
- Multiple controllers and crosshairs up to ten datasets at a time, quick and rough.
- Overlay display opacity control, thresholding. A single pair good for different or similar datasets.
- Overlay toggle, Underlay toggle wiggle, good but a little tricky ('o' and 'u' keys in image viewer)
- Sliding Overlay ('4'/'5' keys), Fade-in overlay ('6' key), Checkerboard Underlay ('#' key) two similar datasets in underlay but must be virtually identical. Good for comparing two processing methods
- Edge display for underlay effective pairwise comparison for quick fine structure display and comparison with overlay dataset with opacity. One dataset should have reliable structure and contrast. Now with 'e' toggle.
- @AddEdge single or dual edges with good contrast for pairwise comparison.

Alignment strategies with align_epi_anat.py

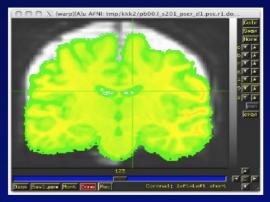
- Defaults work usually (>90% FCON1000)
 - Problems:
- Far off start "-big_move", "-giant_move", "-ginormous_move"
- Poor contrast "-cost lpa", "-cost nmi", "-cost lpc+ZZ"
- ◆ Poor non-uniformity "-edge", "-cost lpa"
- stroke/MS lesions, tumors, monkeys, rats, multi-modality (CT/PET/DTI/...), something else? – see us, post message

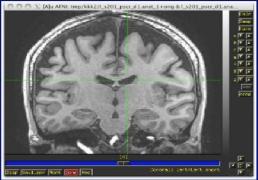


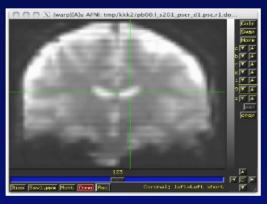
Real and Imaginary Problems

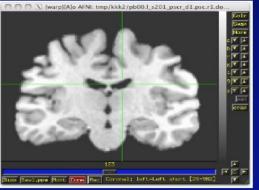
Saved by the contrast

 However, bias may result in erroneous group differences





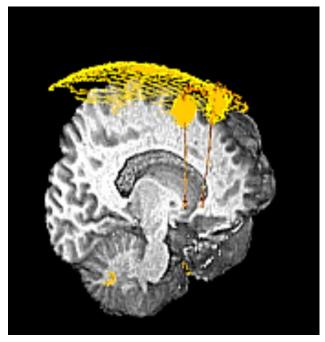




Z.S.S 10/04/10

Alignment -special cases

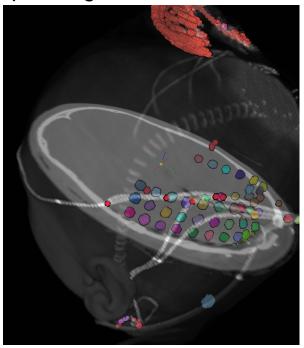
DBS – align CT with electrodes to pre-surgical MRI, PET



Dataset courtesy of Justin Rajendra, (Formerly at Emory, Now in our group. Woohoo!)

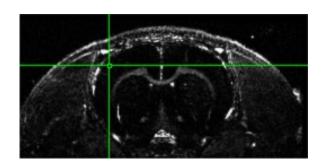
Also see @Install_DBSproc for DBS with CT and DTI processing (S. Horovitz)

ECOG – align CT with electrodes to pre-surgical MRI

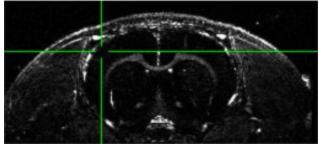


Dataset courtesy of Anna Gaglianese (University of Utrecht, Netherlands)

Rat Brains



Alignment of 12 hour Manganese enhanced MRI scan (MEMRI) to start

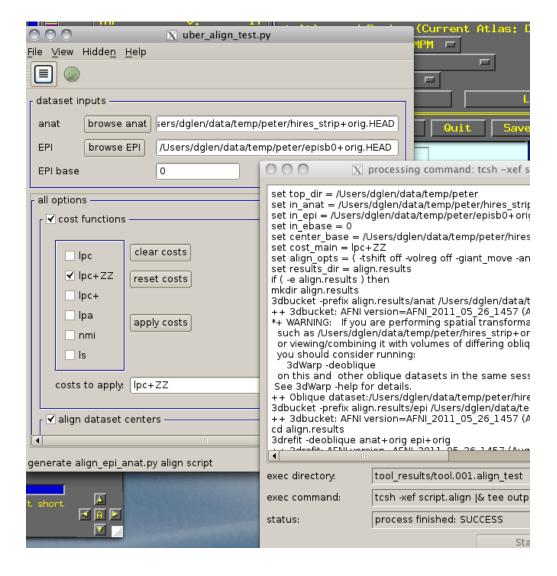


```
#!/bin/tcsh
# align_times.csh
set basedset = 14_pre+orig
foreach timedset ( 14_*hr+orig.HEAD)
    align_epi_anat.py -prep_off -anat $timedset -epi $basedset \
    -epi_base 0 -anat_has_skull no -epi_strip None -suffix _edge2prep \
    -cost lpa -overwrite -edge -rat_align
end
3dTcat -prefix 14_timealigned_edge 14_pre+orig. 14*edge2prep+orig.HEAD
```

Data from Der-Yow Chen (NINDS)

uber_align_test.py

select input
data
set options
create script
run script



afni_proc.py – alignment handling

- Single script to do all the processing of a typical fMRI pipeline including motion correction (3dvolreg), alignment (align_epi_anat.py)
- combines transformations when possible
- from example 6 in afni_proc.py's prodigious help:

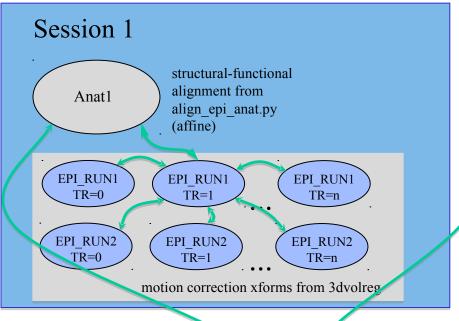
```
afni_proc.py -subj_id sb23.e6.align
    -dsets sb23/epi_r??+orig.HEAD \
    -do_block align tlrc \
    -copy_anat sb23/sb23_mpra+orig \
    -tcat_remove_first_trs 3 \
    -volreg_align_to last \
    -volreg_align_e2a \
    -volreg_tlrc_warp \
```

To process in orig space, remove -volreg_tlrc_warp.

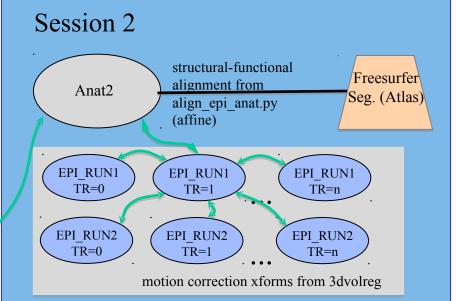
To apply manual tlrc transformation, use -volreg_tlrc_adwarp.

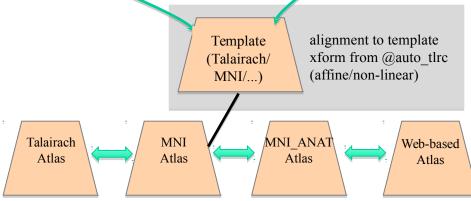
To process as anat aligned to EPI, remove -volreg_align_e2a.

Transformation Chains Example

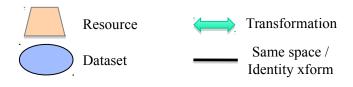


Known or User-defined transformations

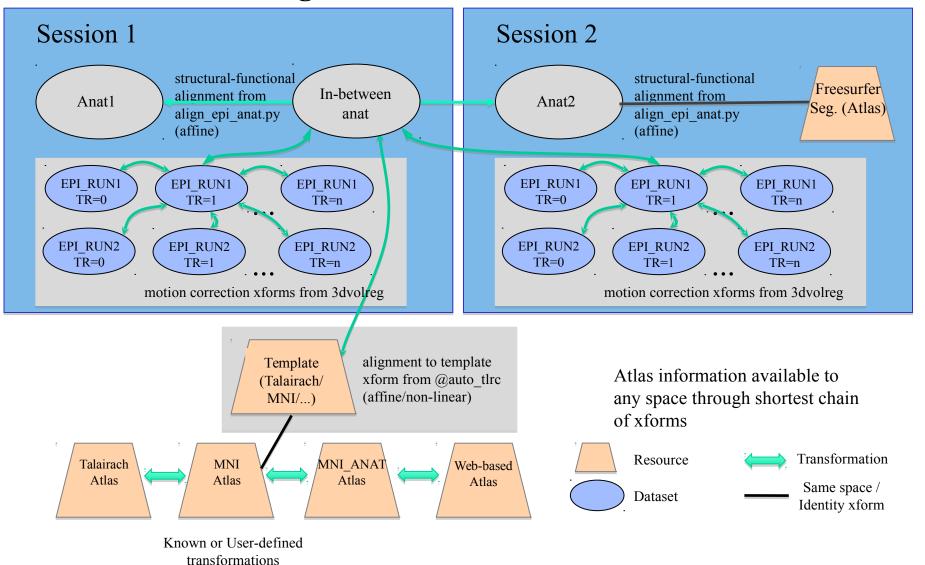




Atlas information available to any space through shortest chain of xforms



Alignment across two sessions



http://afni.nimh.nih.gov/sscc/dglen/alignmentacross2sessions

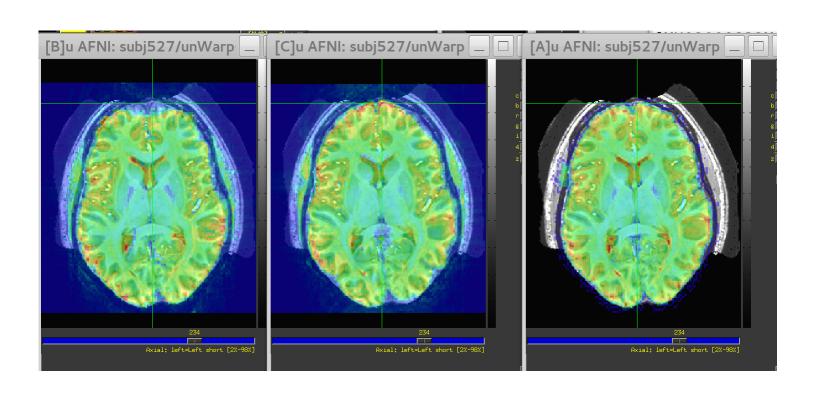
Nonlinear Warping

3dQwarp

- $I_{\text{new}}(\mathbf{x}) = I_{\text{old}}(\mathbf{W}(\mathbf{x}))$
 - \diamond where **W**(**x**) depends on a *lot* of parameters (1000-50000+)
 - Method: Incremental transformation with Hermite cubic polynomials over finer and finer 3D patches. Output is both aligned dataset and the warp and the inverse warp deformations in Dx,Dy,Dz
 - **★** Better alignment of anatomical volumes to template space
 - → Then carry the functional results to template space for better group analyses?
 - → As an aid to brain segmentation and atlas-ing accuracy?
- ★ Pre- and post-surgical alignment, EPI distortion correction
- Related programs and scripts:
 - ♦ 3dNwarpApply, 3dNwarpCat, 3dNwarpCalc, 3dNwarpAdjust, 3dNwarpFuncs
 - auto_warp.py, afni_proc.py

UnwarpEPI.py - blipup-blipdown script (Vinai Roopchansingh)

Blip-up/down distortion correction

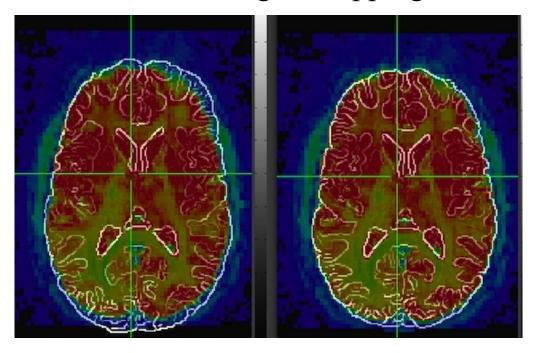


Data courtesy of Sam Torrisi, NIMH Blip-up (uncorrected)

Blip-down

Corrected

Left and Right - flipping



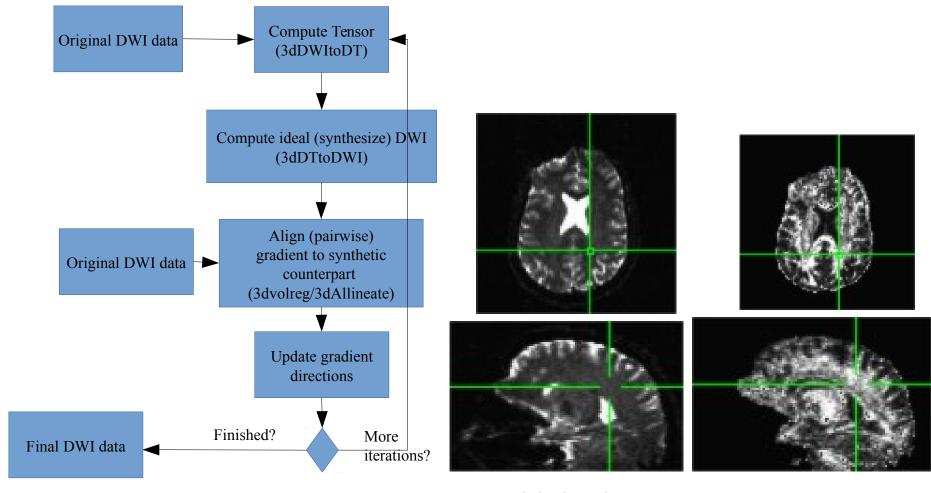
align_epi_anat.py -anat anat+orig -epi epi_r1+orig -epi_base 0 \
-giant_move -check_flip

The output will include this warning if the data is flipped:

If everything is okay, this message appears instead:

Data does not need flipping

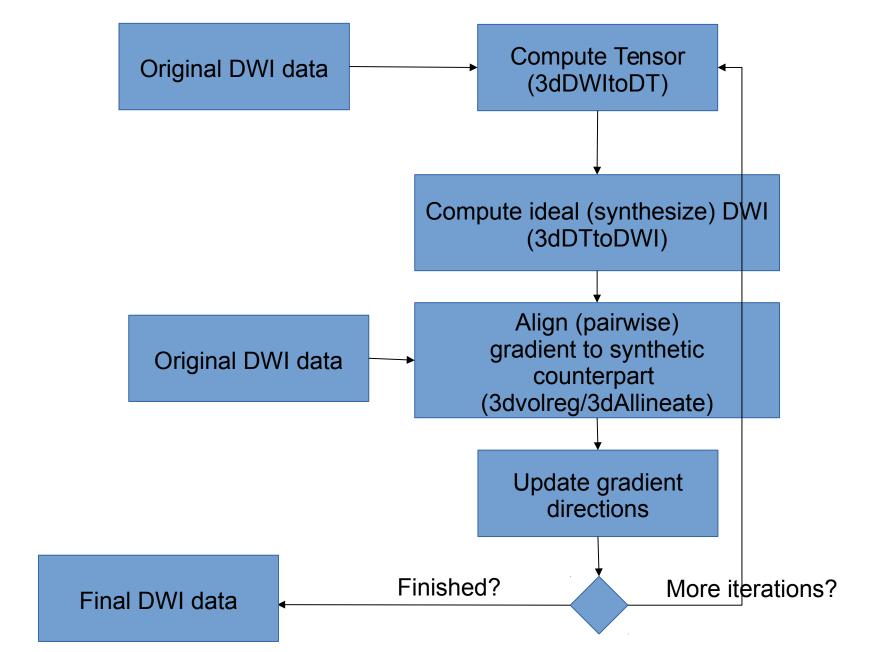
DWI Motion Correction



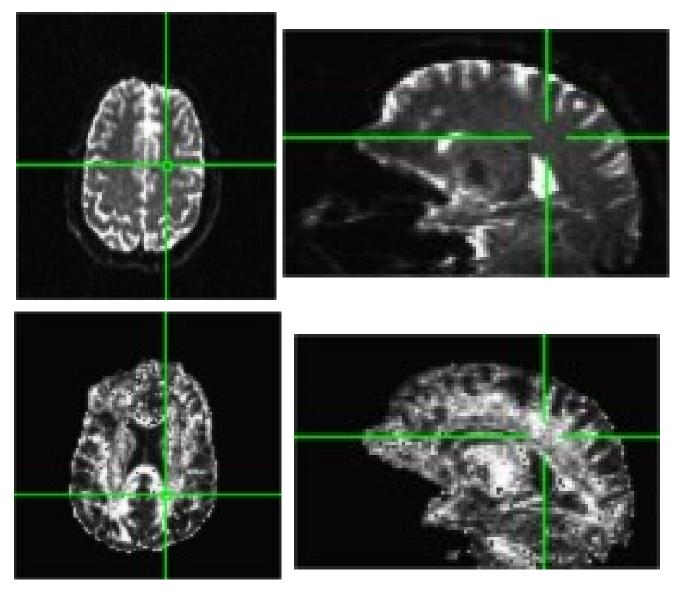
Original motion

FA maps with iteration

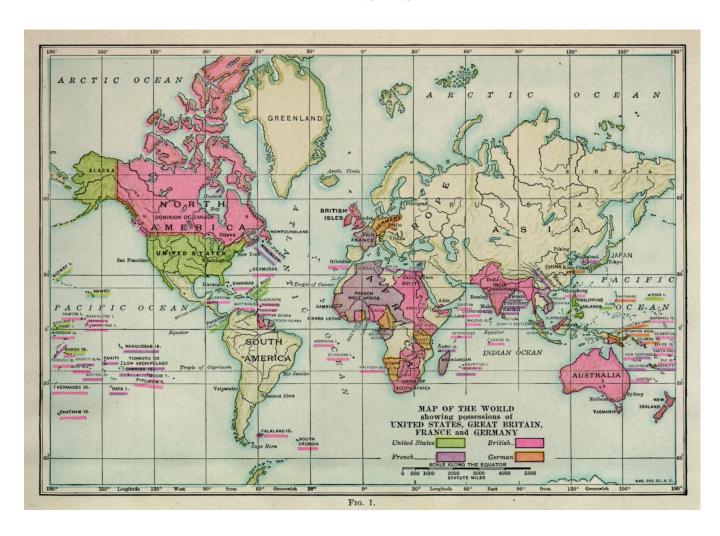
Method overview



DWI Motion Correction

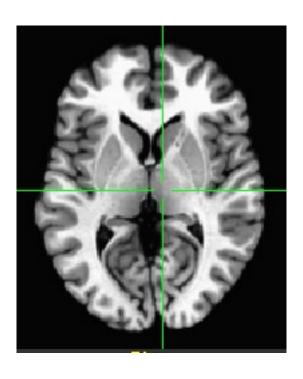


ATLASES



ATLAS DEFINITIONS

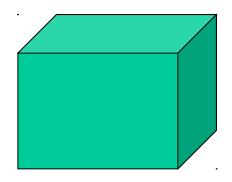
Template - a reference dataset used for matching shapes. Examples: TT_N27+tlrc, MNI_EPI+tlrc, TT_ICBM452+tlrc.



TT N27+tlrc

ATLAS DEFINITIONS

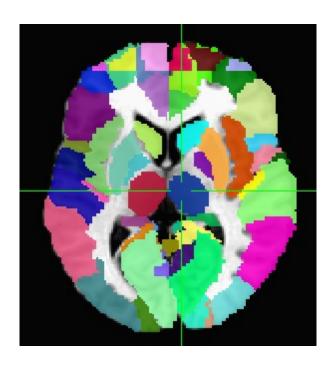
Template Space - x,y,z coordinate system shared by many datasets (the basic shoebox) Examples: TLRC (Talairach-Tourneaux), MNI, MNI_ANAT, ORIG.



ATLAS DEFINITIONS

Atlas - segmentation info.

Examples: TTatlas+tlrc, TT_N27_EZ_ML+tlrc, roidset+orig.



TT N27 EZ ML+tlrc

Registration To Standard Spaces

Transforming Datasets to Talairach-Tournoux Coordinates

The original purpose of AFNI (circa 1994 A.D.) was to perform the transformation of

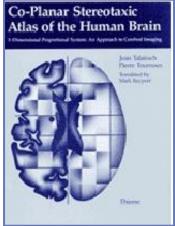
datasets to Talairach-Tournoux (stereotaxic) coordinates

- The transformation can be manual, or automatic
- In manual mode, you must mark various anatomical locations, defined in

Jean Talairach and Pierre Tournoux

"Co-Planar Stereotaxic Atlas of the Human Brain"

Thieme Medical Publishers, New York, 1988



- Marking is best done on a high-resolution T1-weighted structural MRI volume
- In automatic mode, you need to choose a template to which your data are aligned. Different templates are made available with AFNI's distribution. You can also use your own templates.
- Transformation carries over to all other (follower) datasets in the same directory
 - This is where the importance of getting the relative spatial placement of datasets done correctly in to3d really matters
 - You can then write follower datasets, typically functional or EPI timeseries, to disk in Talairach coordinates
 - → Purpose: voxel-wise comparison with other subjects
 - → May want to blur volumes a little before comparisons, to allow for residual anatomic variability: AFNI programs 3dmerge or 3dBlurToFWHM

- Hidden in GUI right click on "DataDir" or set AFNI_ENABLE_MARKERS to YES in .AFNIRC
- Manual Transformation proceeds in two stages:
 - 1. Alignment of AC-PC and I-S axes (to +acpc coordinates)
 - 2. Scaling to Talairach-Tournoux Atlas brain size (to +tlrc coordinates)
- Stage 1: Alignment to +acpc coordinates:
 - Anterior commissure (AC) and posterior commissure (PC) are aligned to be the y-axis
 - The longitudinal (inter-hemispheric or mid-sagittal) fissure is aligned to be the yzplane, thus defining the z-axis
 - The axis perpendicular to these is the x-axis (right-left)
 - Five markers that you must place using the [<u>Define Markers</u>] control panel:

```
AC superior edge = top middle of anterior commissure

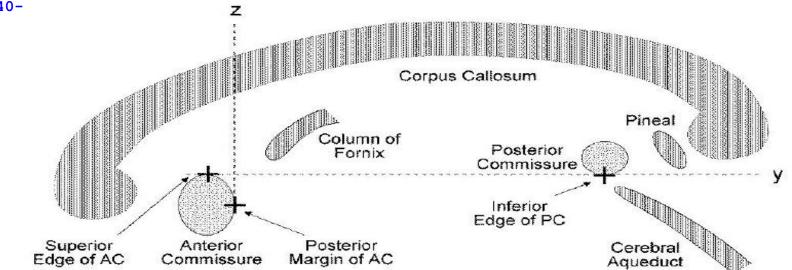
AC posterior margin = rear middle of anterior commissure

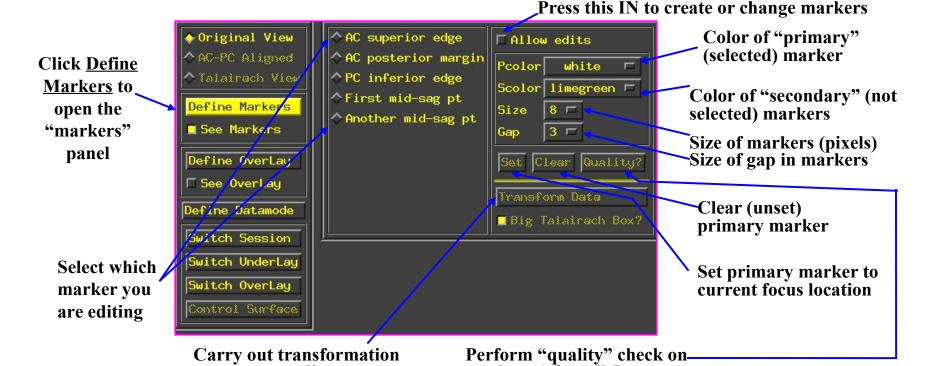
PC inferior edge = bottom middle of posterior commissure

First mid-sag point = some point in the mid-sagittal plane

Another mid-sag point = some other point in the mid-sagittal plane
```

- This procedure tries to follow the Atlas as precisely as possible
 - ➤ Even at the cost of confusion to the user (e.g., you)



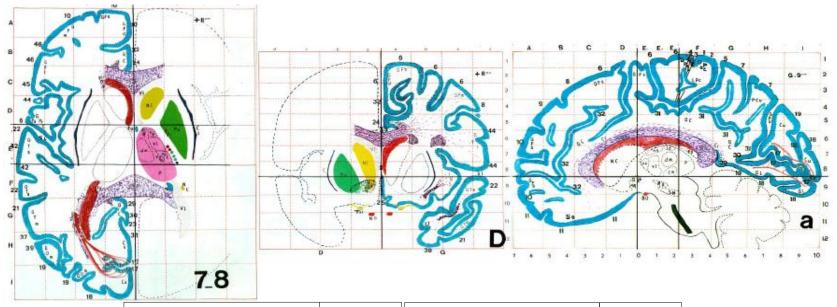


to +acpc coordinates

markers (after all 5 are set)

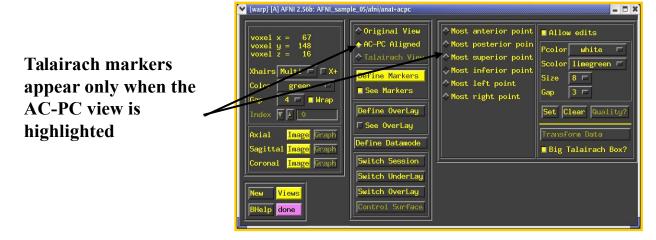
• Stage 2: Scaling to Talairach-Tournoux (+tlrc) coordinates:

 Once the AC-PC landmarks are set and we are in ACPC view, we now stretch/shrink the brain to fit the Talairach-Tournoux Atlas brain size (sample TT Atlas pages shown below, just for fun)



Most anterior to AC	70 mm		
AC to PC	23 mm		
PC to most posterior	79 mm		
AC to most superior	74 mm	Length of cerebrum	172mm
AC to left (or right)	68 mm	Weith toffoer petrium	136mm

- Selecting the Talairach-Tournoux markers for the bounding box:
 - ♦ There are 12 sub-regions to be scaled (3 A-P x 2 I-S x 2 L-R)
 - ♦ To enable this, the transformed +acpc dataset gets its own set of markers
 - → Click on the [AC-PC Aligned] button to view our volume in ac-pc coordinates
 - ► Select the [Define Markers] control panel
 - ◆ A new set of six Talairach markers will appear and the user now sets the bounding box markers (see Appendix C for details):

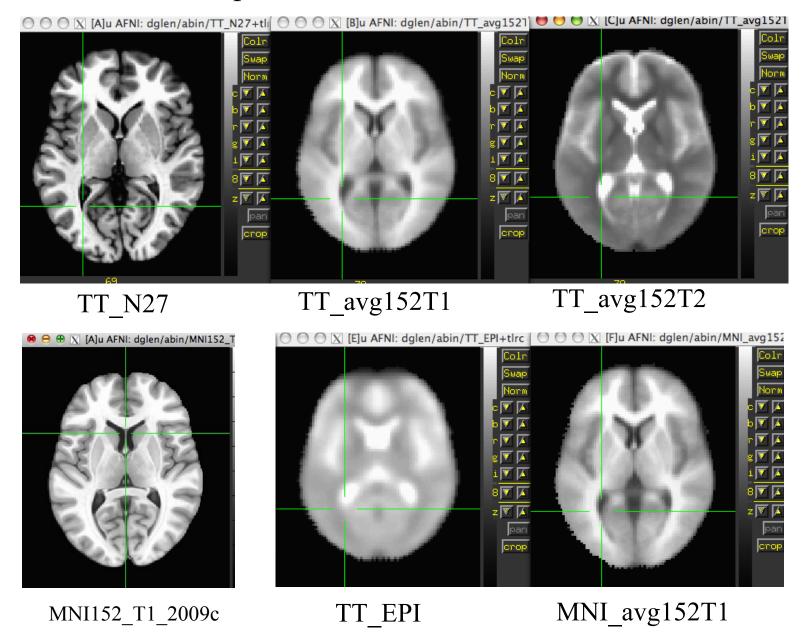


- Once all the markers are set, and the quality tests passed. Pressing [<u>Transform Data</u>] will write new *header* containing the Talairach transformations (see Appendix C for details)
 - ➤ Recall: With AFNI, spatial transformations are stored in the header of the output

- Is manual selection of AC-PC and Talairach markers bringing you down? You can now perform a TLRC transform *automatically* using an AFNI script called <code>@auto_tlrc</code>.
 - Differences from Manual Transformation:
 - ➡ Instead of setting ac-pc landmarks and volume boundaries by hand, the anatomical volume is warped (using 12-parameter affine transform) to a template volume in TLRC space.
 - → Anterior Commisure (AC) center no longer at 0,0,0 and size of brain box is that of the template you use.
 - For various reasons, some good and some bad, templates adopted by the neuroimaging community are not all of the same size. Be mindful when using various atlases or comparing standard-space coordinates.
 - ➤ You, the user, can choose from various templates for reference but be consistent in your group analysis.
 - ➤ Easy, automatic. Just check final results to make sure nothing went seriously awry. AFNI is perfect but your data is not.

- Templates in @auto tlrc that the user can choose from:
 - TT N27+tlrc
 - AKA "Colin brain". One subject (Colin) scanned 27 times and averaged. (www.loni.ucla.edu, www.bic.mni.mcgill.ca)
 - Has a full set of FreeSurfer (surfer.nmr.mgh.harvard.edu) surface models that can be used in SUMA (link).
 - Is the template for cytoarchitectonic atlases (www.fz-juelich.de/ime/spm_anatomy_toolbox)
 - For improved alignment with cytoarchitectonic atlases, I recommend using the TT_N27 template because the atlases were created for it. In the future, we might provide atlases registered to other templates.
 - TT icbm452+tlrc:
 - International Consortium for Brain Mapping template, average volume of 452 normal brains. (www.loni.ucla.edu, www.bic.mni.mcgill.ca)
 - * TT avg152T1+tlrc:
 - Montreal Neurological Institute (www.bic.mni.mcgill.ca) template, average volume of 152 normal brains.
 - " TT_EPI+tlrc:
 - EPI template from spm2, masked as TT_avg152T1. TT_avg152 and TT_EPI volumes are based on those in SPM's distribution. (www.fil.ion.ucl.ac.uk/spm/)
 - MNI152 T1 2009c+tlrc:
 - MNI's 152 nonlinear asymmetric template

Templates included with AFNI



Steps performed by @auto_tlrc

- For warping a volume to a template (Usage mode 1):
 - Pad the input data set to avoid clipping errors from shifts and rotations
 - 2. Strip skull (if needed)
 - 3. Resample to resolution and size of TLRC template
 - 4. Perform 12-parameter affine registration using **3dWarpDrive**Many more steps are performed in actuality, to fix up various pesky little artifacts. Read the script if you are interested.
 - Typically this steps involves a high-res anatomical to an anatomical template
 - ► Example: @auto_tlrc -base TT_N27+tlrc. -input anat+orig. -suffix NONE
 - One could also warp an EPI volume to an EPI template.
 - ➡ If you are using an EPI time series as input. You must choose one sub-brick to input. The script will make a copy of that sub-brick and will create a warped version of that copy.

Applying a transform to follower datasets

- Say we have a collection of datasets that are in alignment with each other. One
 of these datasets is aligned to a template and the same transform is now to be
 applied to the other follower datasets
- For Talairach transforms there are a few methods:
 - Method 1: Manually using the AFNI interface (see Appendix C)
 - Method 2: With program adwarp

```
adwarp -apar anat+tlrc -dpar func+orig
```

- → The result will be: func+tlrc.HEAD and func+tlrc.BRIK
- Method 3: With @auto_tlrc script in mode 2
 - ONLY when -apar dataset was created by @auto_tlrc
 - @auto_tlrc -apar SubjectHighRes+tlrc. \
 - -input Subject_EPI+orig. -dxyz 3
 - (the output is named Subject EPI at+TLRC, by default)
- Why bother saving transformed datasets to disk anyway?
 - ◆ Datasets without .BRIK files are of limited use, only for display of slice images

@auto_tlrc Example

- Transforming the high-resolution anatomical:
 - (If you are also trying the manual transform on workshop data, start with a fresh directory with no +tlrc datasets)

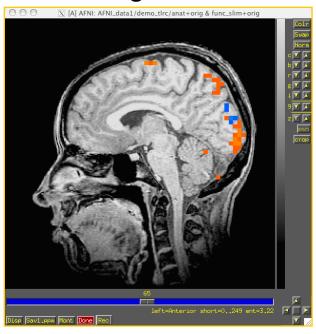
```
@auto_tlrc
   -base TT_N27+tlrc  \
   -suffix NONE  \
   -input anat+orig
```

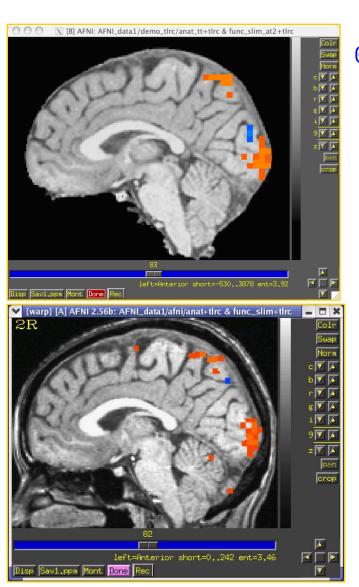
 Transforming the function ("follower datasets"), setting the resolution at 2 mm:

```
@auto_tlrc
-apar anat+tlrc \
-input func_slim+orig \
-suffix NONE \
-dxyz 2
Output:
func_slim+tlrc
```

 You could also use the icbm452 or the mni's avg152T1 template instead of N27 or any other template you like (see @auto_tlrc -help for a few good words on templates)

Original





@auto_tlrc

Manual

Standard Spaces

Why use a standard template space?

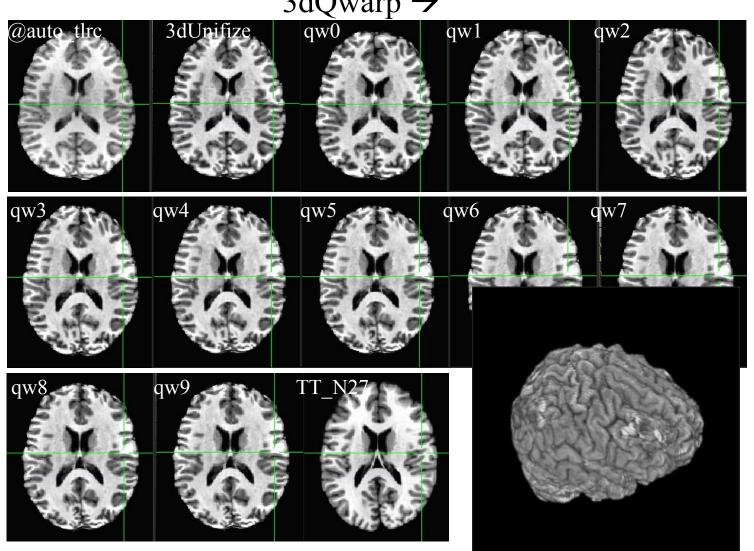
- Compare across subjects and groups easily for every voxel in the brain
- Standardize coordinates with others
- Know where a voxel is automatically from an atlas
- Mostly automated and no specific ROI drawing required

Why not use a standard template space?

- Inconsistency among subjects
- Inconsistency among groups elderly versus younger
- Use consistent anatomical ROIs with good anatomical knowledge
- Lower threshold for multiple comparison adjustments

Nonlinear alignment to template

3dQwarp →



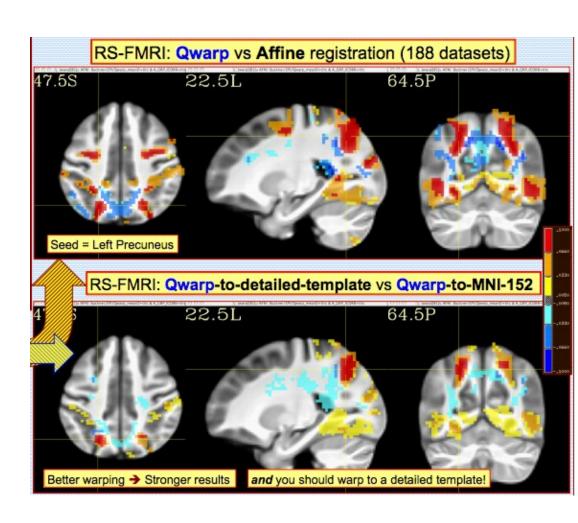
Nonlinear alignment

Advantages:

- Great alignment better spatial correspondence across data →
- Aligned data matches template

Disadvantages:

- Distortion of individual data
- Aligned data matches template.
 Choose template carefully
- End limits?
- Skullstripping must be done much more carefully
- Processing time much slower
- Not yet integrated into AFNI GUI for warp-on-demand



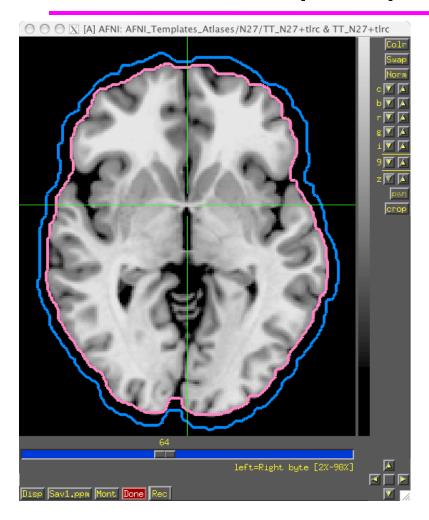
Comparing data

- How can I compare regions/voxels across subjects and groups?
 What works "best"?
 - @auto_tlrc affine registration method to align individual subjects to a template
 - auto_warp.py nonlinear alignment to template better.
 - manual Talairach based on specific markers divides data up based on AC-PC line and brain enclosing boxes. Better for looking at medial structures.
 - 3dTagalign place markers on specific corresponding points among datasets and align with affine transformation
 - ROI creation draw ROI's (Draw Dataset plug-in) for each structure

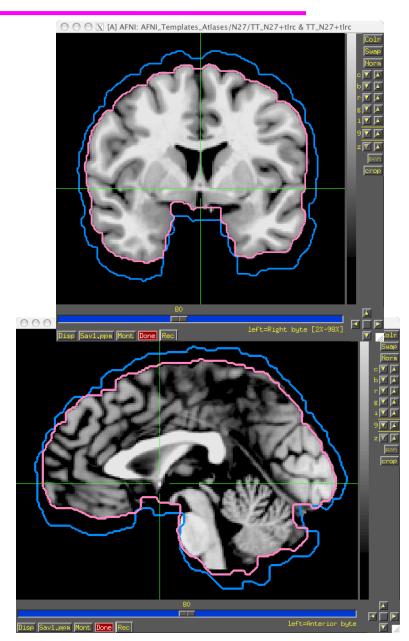
Choosing a template

- Similar to subject group neonates, pediatric, young adults, elderly, macaque, rabbit...
- Same modality, similar coverage
- Relevant atlas segmentation
- Individual or group template
 - Group average or iterative
- Make your own template (and maybe an atlas too)
 - Haskins pediatric atlas research
 - → affine group averages
 - ➡ finding the most "typical" individual in group
 - → nonlinear alignment to typical
 - → iterative nonlinear alignment
 - @toMNI_Awarp, @toMNI_Qwarpar

Atlas/Template Spaces Differ In Size

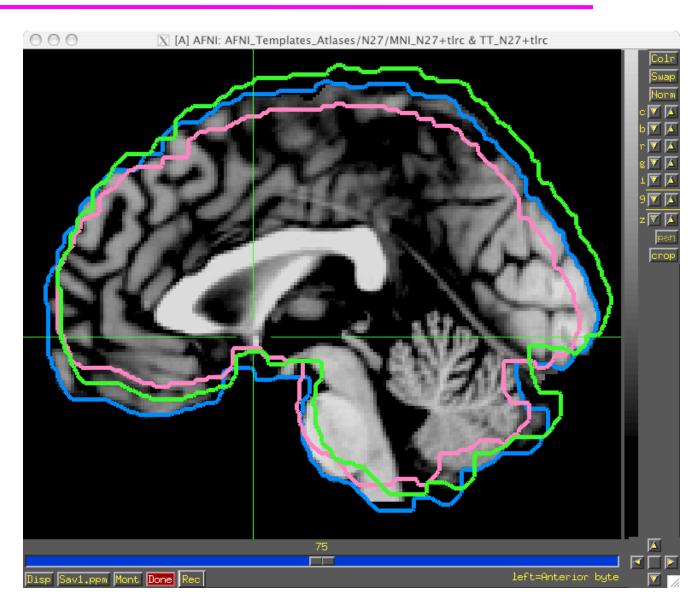


MNI is larger than TLRC space.



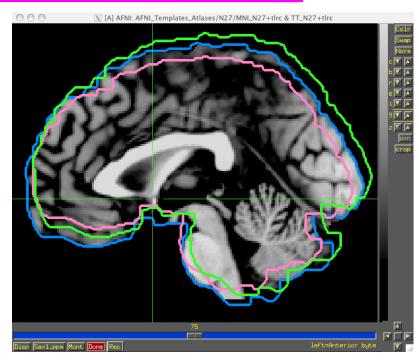
Atlas/Template Spaces Differ In Origin

TLRC MNI MNI-Anat.



From Space To Space

TLRC MNI MNI-Anat.



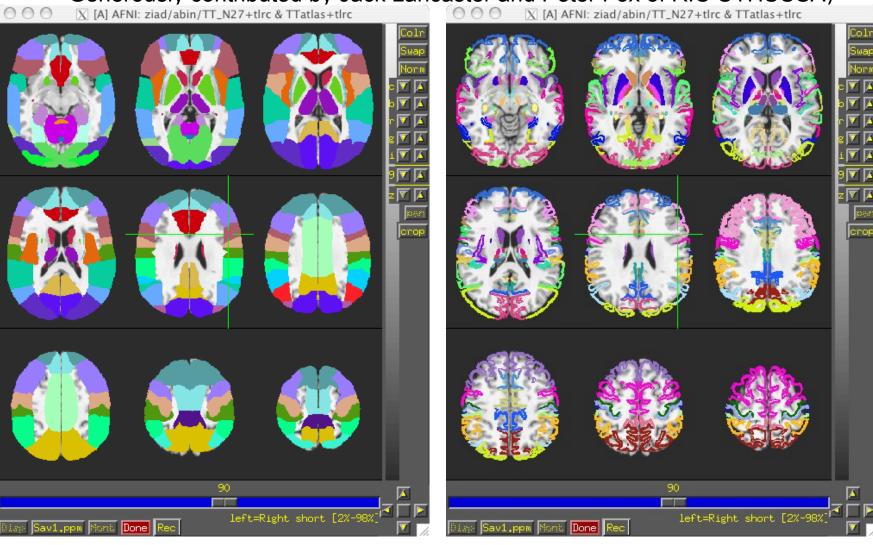
- Going between TLRC and MNI:
 - Approximate equation
 - used by whereami and 3dWarp
 - Manual TLRC transformation of MNI template to TLRC space
 - used by whereami (as precursor to MNI Anat.), based on N27 template
 - Multiple space coordinates reported in whereami output (AFNI_ATLAS_TEMPLATE_SPACE_LIST)
- Going between MNI and MNI Anatomical (Eickhoff et al. Neuroimage 25, 2005):
 - MNI + (0, 4, 5) = MNI Anat. (in RAI coordinate system)
- Going between TLRC and MNI Anatomical (as practiced in whereami):
 - Go from TLRC (TT_N27) to MNI via manual xform of N27 template
 - Add (0, 4, 5)

Atlases/Templates Use Different Coord. Systems

- There are 48 manners to specify XYZ coordinates
- Two most common are RAI/DICOM and LPI/SPM
- RAI means
 - ♦ X is Right-to-Left (from negative-to-positive)
 - ♦ Y is Anterior-to-Posterior (from negative-to-positive)
 - ♦ Z is Inferior-to-Superior (from negative-to-positive)
- LPI means
 - ♦ X is Left-to-Right (from negative-to-positive)
 - Y is Posterior-to-Inferior(from negative-to-positive)
 - Z is Inferior-to-Superior (from negative-to-positive)
- To go from RAI to LPI just flip the sign of the X and Y coordinates
 - Voxel -12, 24, 16 in RAI is the same as 12, -24, 16 in LPI
 - Voxel above would be in the Right, Posterior, Superior octant of the brain
- AFNI allows for all coordinate systems but default is RAI
 - Can use environment variable AFNI_ORIENT to change the default for AFNI AND other programs.
 - See whereami -help for more details.

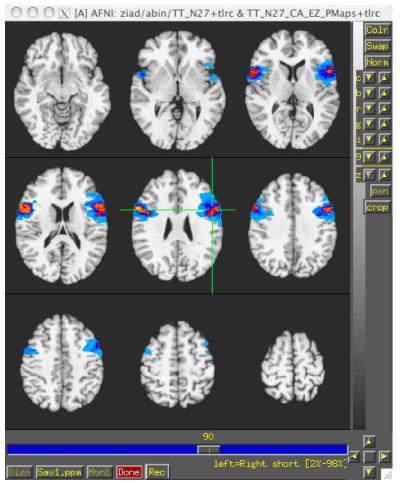
Atlases Distributed With AFNI TT_Daemon

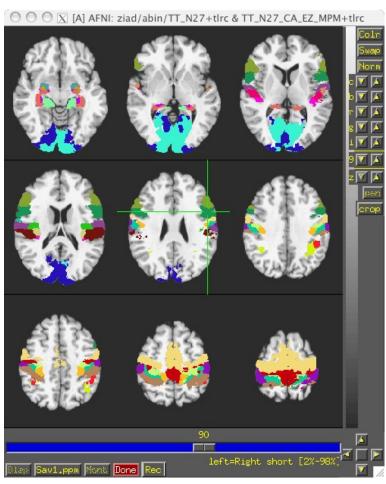
- TT_Daemon : Created by tracing Talairach and Tournoux brain illustrations.
 - Generously contributed by Jack Lancaster and Peter Fox of RIC UTHSCSA)



Atlases Distributed With AFNI Anatomy Toolbox: Prob. Maps, Max. Prob. Maps

- CA_N27_MPM, CA_N27_ML, CA_N27_PM: Anatomy Toolbox's atlases with some created from cytoarchitectonic studies of 10 human post-mortem brains
 - Generously contributed by Simon Eickhoff, Katrin Amunts and Karl Zilles of IME, Julich, Germany



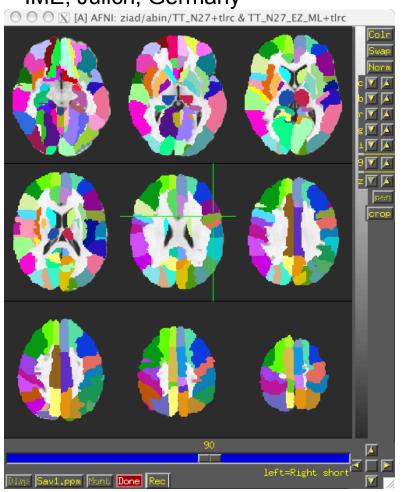


Atlases Distributed With AFNI: Anatomy Toolbox: MacroLabels

 CA_N27_MPM, CA_N27_ML, CA_N27_PM: Anatomy Toolbox's atlases with some created from cytoarchitectonic studies of 10 human post-mortem brains

Generously contributed by Simon Eickhoff, Katrin Amunts and Karl Zilles of

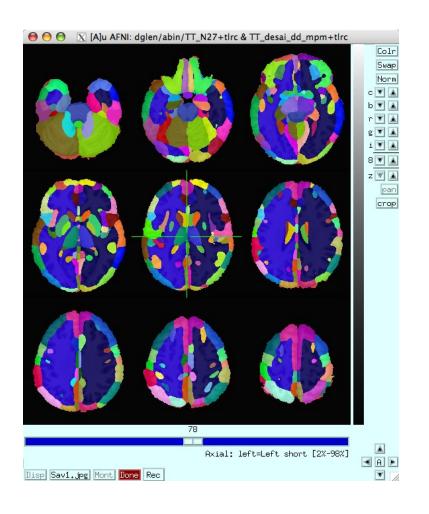
IME, Julich, Germany

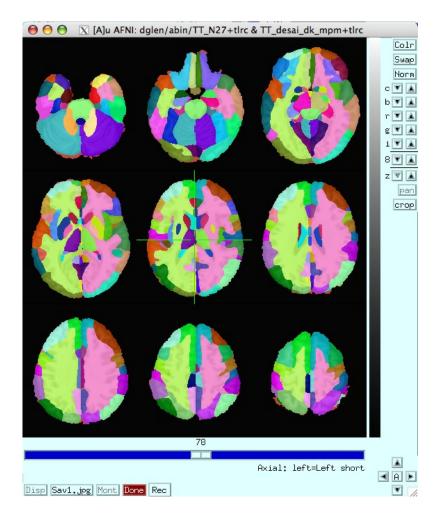


```
Atlas CA ML 18 MNIA: Macro Labels (N27)
      Focus point: Left SupraMarginal Gyrus
      Within 4 mm: Left Superior Temporal Gyrus
      Within 6 mm: Left Middle Temporal Gyrus
Atlas CA_MPM_18_MNIA: Cytoarch. Max. Prob. Maps
      Focus point: IPC (PF)
      Within 2 mm: IPC (PFm)
      Within 3 mm: IPC (PFcm)
      Within 5 mm: IPC (PGa)
      Within 7 mm: TE 3
Atlas CA_PM_18_MNIA: Cytoarch. Probabilistic Maps
      Focus point: IPC (PFm)
      (p = 0.40)
      -AND- IPC (PFcm)
      (p = 0.20)
      -AND- IPC (PF)
      (p = 0.60)
Atlas CA_LR_18_MNIA: Left/Right (N27)
      Focus point: Left Brain
```

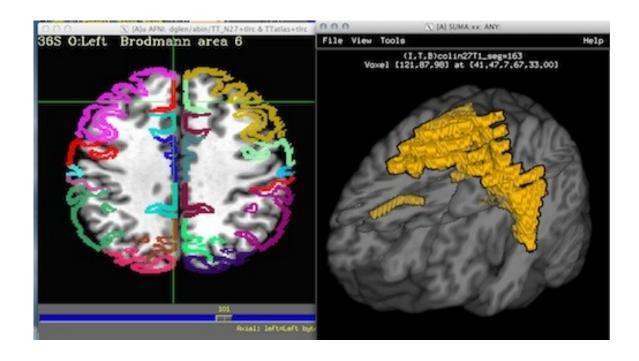
Atlases Distributed With AFNI: Desai PMaps and MPMs

 Atlases generated with typical AFNI pipeline using @auto_tlrc and FreeSurfer segmentation across multiple subjects



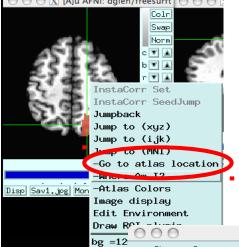


Talairach Daemon (TT_Daemon) problem



Some fun and useful things to do with +tlrc datasets are on the 2D slice viewer

Right click to get menu: [O O N [A]u AFNI: dglen/freesurft [O O D



Go to Atlas Location

Lets you jump to centroid of regions to current default atlas (set by AFNI_ATLAS_COLORS)
Works in +orig too

```
X menu
   -Choose One----
Brain Structure (from DD_Desai_MPM)
ctx_lh_G_and_S_cingul-Mid-Ant [ 3,-13, 32]
ctx_lh_G_and_S_cingul-Mid-Post [ 4, 15, 38]
ctx_lh_G_cingul-Post-dorsal [ 2, 39, 28]
ctx_lh_G_cingul-Post-ventral [ 4, 45, 5]
ctx_lh_G_cuneus [ 1, 81, 14]
ctx_lh_G_front_inf-Opercular [ 49,-12, 13]
ctx_lh_G_front_inf-Orbital [ 46,-28, -5]
ctx_lh_G_front_inf-Triangul [ 49,-30, 8]
ctx_lh_G_front_middle [ 35,-31, 36]
ctx_1h_G_front_sup [ 8,-22, 47]
ctx_lh_G_Ins_lg_and_S_cent_ins [ 37, 8, 5]
ctx_lh_G_insular_short [ 36, -9, 0]
ctx_lh_G_occipital_middle [ 38, 82, 9]
ctx_lh_G_occipital_sup [ 12, 89, 27]
ctx_lh_G_oc-temp_lat-fusifor [ 32, 43,-18]
ctx_lh_G_oc-temp_med-Lingual [ 5, 68, -8]
ctx_lh_G_oc-temp_med-Parahip [ 20, 12,-24]
ctx_lh_G_orbital [ 27,-34,-12]
ctx_lh_G_pariet_inf-Angular [ 43, 66, 35]
ctx_lh_G_pariet_inf-Supramar [ 56, 37, 33]
ctx_lh_G_parietal_sup [ 21, 63, 53]
ctx_lh_G_postcentral [ 44, 28, 52]
ctx_lh_G_precentral [ 41, 10, 49]
ctx_lh_G_precuneus [ 3, 58, 36]
ctx_lh_G_rectus [ 2,-38,-14]
     Quit
                      Apply
Index ▲ ▼ 15
```

Shows you where you are in various atlases and spaces

(works in +orig too, if you have a transformed parent)

For atlas installation, and much, much more, see help in command line version:

whereami -help

Quit AFNI whereami +++++ nearby Atlas structures ++++++ Original input data coordinates in TT N27 space Focus point (LPI)= -54 mm [L], -43 mm [P], 25 mm [S] {TLRC} -58 mm [L], -44 mm [P], 27 mm [S] {MNI} NeuroSynth SumsDB -58 mm [L], -48 mm [P], 32 mm [S] {MNI_ANAT} Atlas HaskinsPeds NL atlas1.0: session atlas Focus point: ctx-lh-superiortemporal Within 4 mm: ctx-lh-supramarginal Within 5 mm: ctx-lh-bankssts Within 7 mm: ctx-lh-inferiorparietal Atlas TT Daemon: Talairach-Tournoux Atlas Focus point: Left Inferior Parietal Lobule -AND- Left Brodmann area 40 Within 2 mm: Left Supramarginal Gyrus Within 3 mm: Left Brodmann area 13 Within 4 mm: Left Superior Temporal Gyrus Within 5 mm: Left Brodmann area 22 Within 6 mm: Left Insula

- whereami can provide the user with more detailed information regarding the output of 3dclust
 - For instance, say you want more information regarding the center of mass voxels from each cluster (from the 3dclust output). I.e., where do they fall approximately within the atlases?

```
3dclust -dxyz=1 -1clip 9.5 1 1000 func_FullF+tlrc > clusts.1D
whereami -coord_file clusts.1D'[1,2,3] -tab | less
```

```
++ Input coordinates orientation set by default rules to RAI
++ Input coordinates space set by default rules to TLRC
++++++ nearby Atlas structures ++++++
Focus point (LPI)
                                       Coord.Space
 42 mm [R], -61 mm [P], -3 mm [I]
                                       {T-T Atlas}
 43 mm [R], -63 mm [P], -7 mm [I]
                                       {MNI Brain}
 45 mm [R], -69 mm [P],
                          2 mm [I]
                                       {MNI Anat.}
Atlas
               Within Label
                                                               Prob.
                                                                       Code
               3.0
                       Right Middle Occipital Gyrus
                                                                       33
TT_Daemon
TT_Daemon
               3.0
                       Right Brodmann area 37
                                                                       113
TT_Daemon
               4.0
                       Right Inferior Temporal Gyrus
                                                                       29
                       Right Middle Temporal Gyrus
                                                                       35
TT_Daemon
               4.0
                       Right Inferior Occipital Gyrus
                                                                       28
TT Daemon
               6.0
                       Right Brodmann area 19
                                                                       96
TT_Daemon
               7.0
CA_N27_MPM
               4.0
                       h0C5 (V5 / MT+)
                                                                MPM
                                                                       110
CA_N27_ML
               0.0
                       Right Inferior Temporal Gyrus
                                                                       90
                                                                       86
CA_N27_ML
               1.0
                       Right Middle Temporal Gyrus
                       Right Inferior Occipital Gyrus
                                                                       54
CA_N27_ML
               5.0
                                                                       52
CA_N27_ML
               6.0
                       Right Middle Occipital Gyrus
****** Please use results with caution!
****** Brain anatomy is quite variable! ******
****** The database may contain errors! ******
```

Center of mass output, columns 1,2,3, from 3dclust output

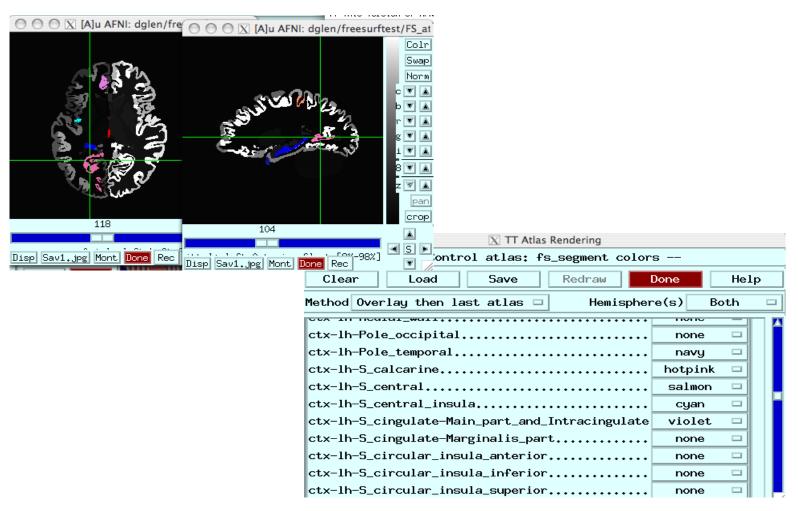
Shown: Cluster #1's coordinates according to various atlases (TT, MNI, etc), as well as the name of the anatomical structure that is located at or near these coordinates (which may vary by atlas)

 whereami can report on the overlap of ROIs with atlasdefined regions

whereami -omask anat_roi+tlrc

```
++ Input coordinates orientation set by default rules to RAI
++ Input coordinates space set by default rules to TLRC
++ In ordered mode ...
++ Have 2 unique values of:
   0 1
++ Skipping unique value of 0
++ Processing unique value of 1
     195 voxels in ROI
     195 voxels in atlas-resampled mask
Intersection of ROI (valued 1) with atlas TT_Daemon (sb0):
  89.2 % overlap with Middle Occipital Gyrus, code 33
  6.7 % overlap with Middle Temporal Gyrus, code 35
  95.9 % of cluster accounted for.
Intersection of ROI (valued 1) with atlas TT Daemon (sb1):
  19.5 % overlap with Brodmann area 37, code 113
  1.5 % overlap with Brodmann area 19, code 96
   21.0 % of cluster accounted for.
      195 voxels in atlas-resampled mask
Intersection of ROI (valued 1) with atlas CA_N27_MPM (sb0):
  1.5 % overlap with hOC5 (V5 / MT+), code 110
  1.5 % of cluster accounted for.
      195 voxels in atlas-resampled mask
Intersection of ROI (valued 1) with atlas CA_N27_ML (sb0):
   61.0 % overlap with Right Middle Occipital Gyrus, code 52
  20.0 % overlap with Right Middle Temporal Gyrus, code 86
  81.0 % of cluster accounted for.
```

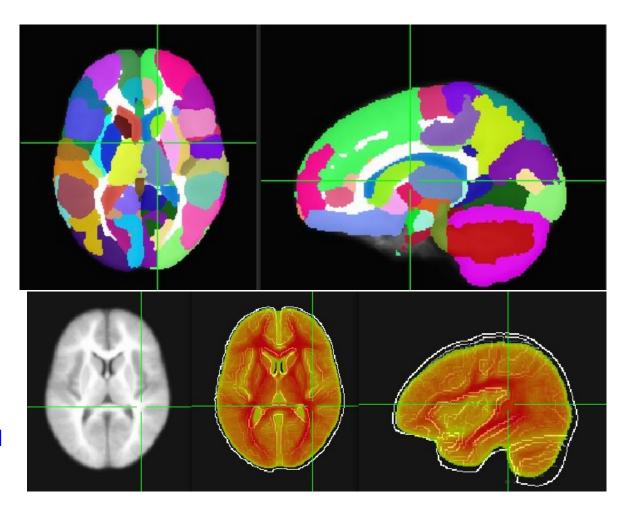
♦ [Atlas colors]



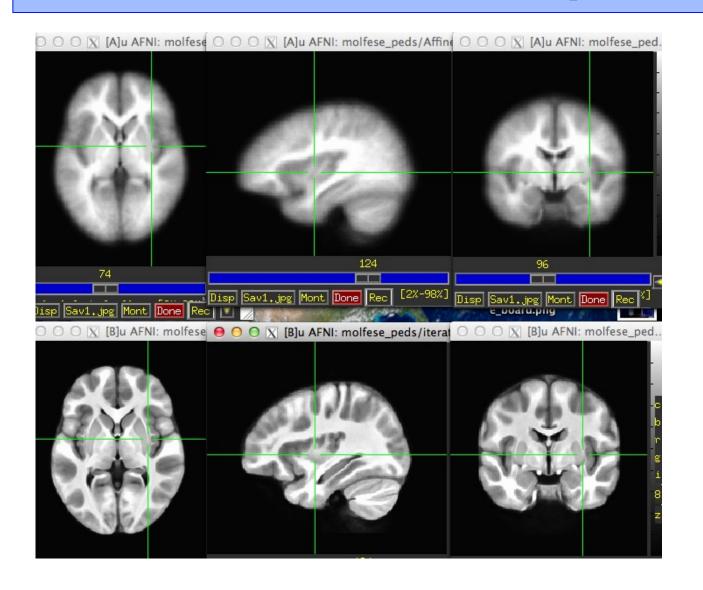
Lets you show atlas regions over your own data (works only in +tlrc).

Haskins Pediatric Atlas

- Pediatric brain atlas and templates (7-12 years old) – Peter Molfese, (formerly Haskins Labs, now at NIH - woohoo!)
- Manually corrected segmentation from Freesurfer.
- Probabilistic, MPM and template
- ~75 subjects -> 500 (ages 6-13)
- Affine, nonlinear averages, ideal/typical subjects, outliers



Haskins Pediatric Atlas - templates

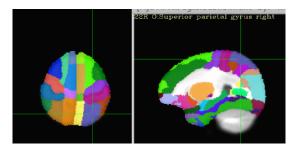


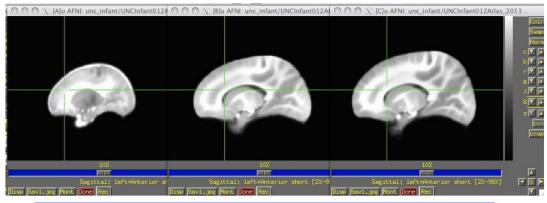
Affine Group

Nonlinear Group I – iterative

Atlases and Templates Available!

 Infant brain atlas and templates – neonate, 1-year, 2-year.
 Contributed by Feng Shi, UNC





UNC infant templates and atlases - neonate, 1 yr, 2 yr old

 Cerebellum atlas and templates – Jorn Diedrichsen, UCL, UK contribution

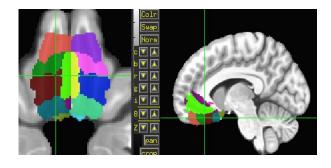


More Atlases and Templates Available!

Ventromedial Prefrontral Cortex (vmPFC, Scott Mackey)

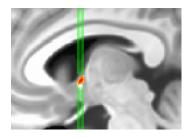
Waxholm Rat Atlas - Papp, et al. Rat brain templates in Paxinos space – Karolinska Institute, Woo Hyun Shim MGH contributions

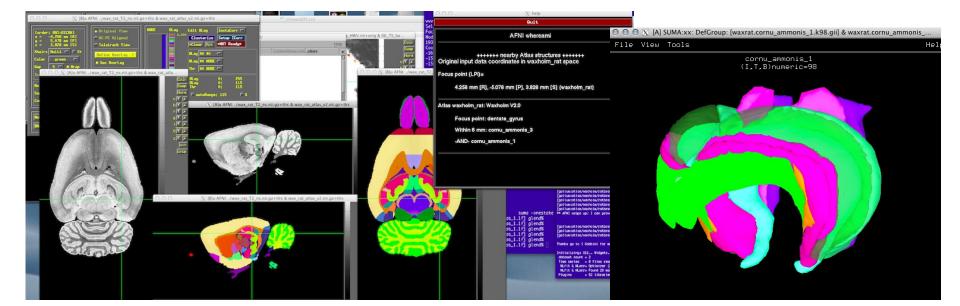
BNST - Torrisi, NIMH



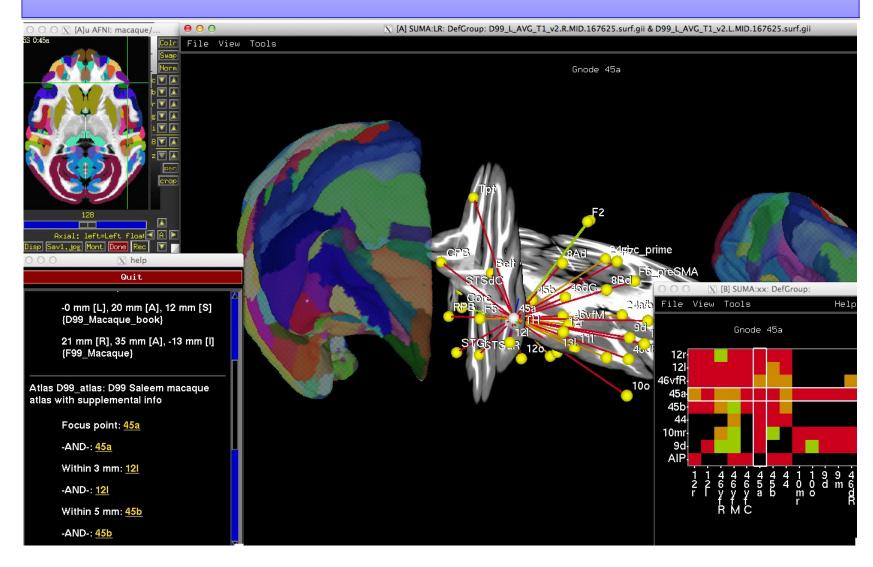
All of these are user requests or contributions!

What do you need?

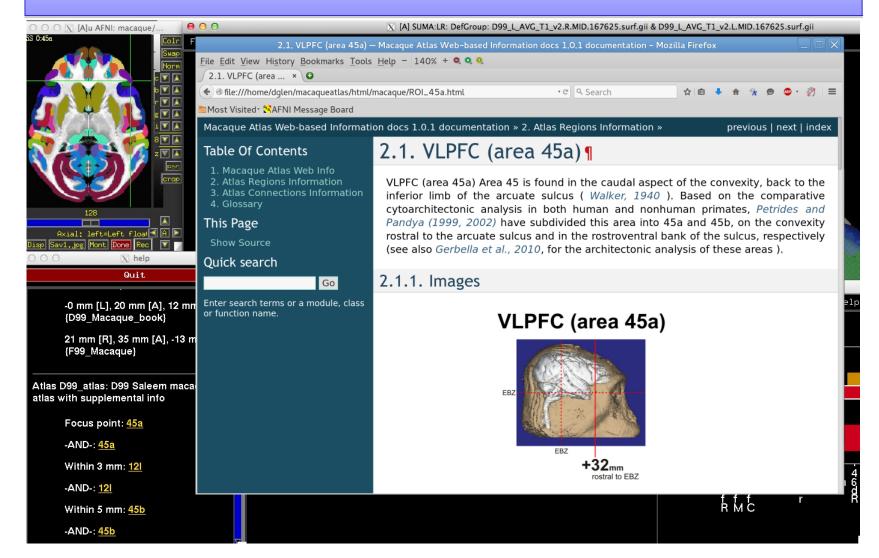




Saleem macaque atlas – MRI, surfaces, connections, supplemental webpages



Saleem macaque atlas – MRI, surfaces, connections, supplemental webpages (in development)

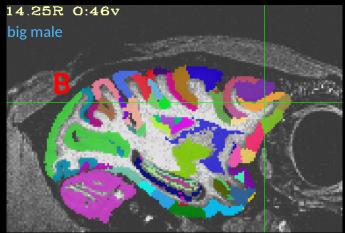


Mapping the digital atlas onto different macaques MRI



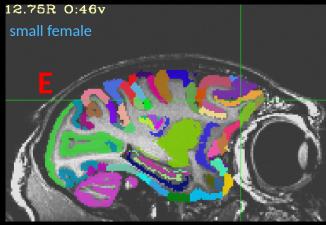
D99 - Digital atlas

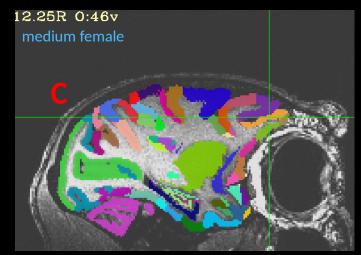
Reveley, Gruslys, Ye, Samaha, Glen, Saad, Seth, Leopold, and Saleem (in preparation)

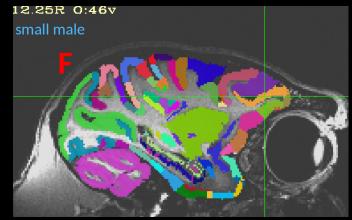


Spatial transformation of the atlas segmentation to each macaque's native space

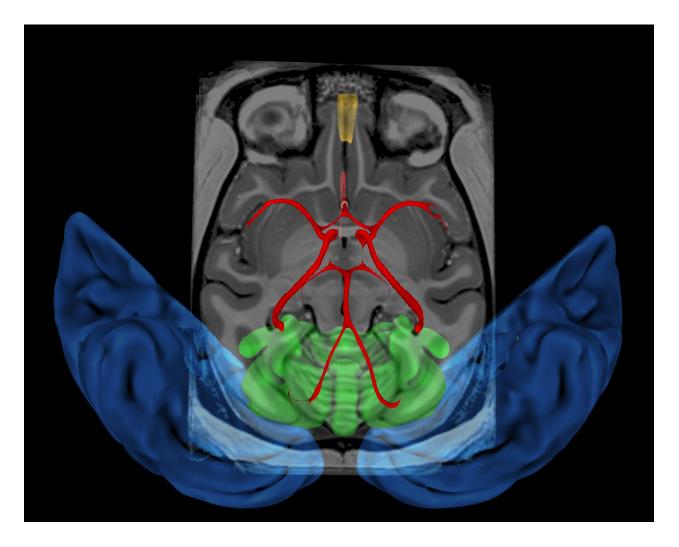






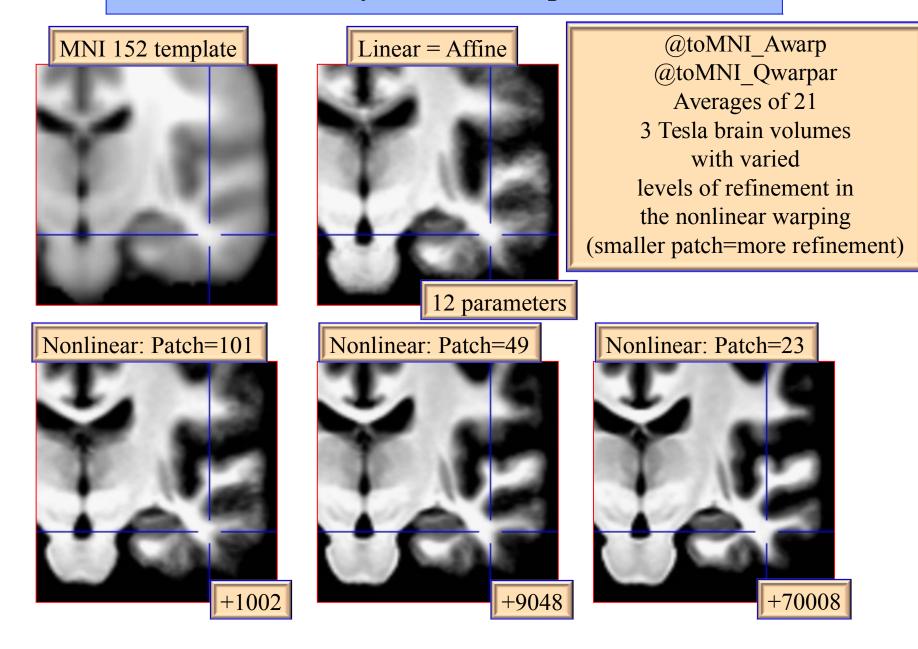


NMT (NIH Macaque Template) – Group template from 31 macaques, surfaces, GM/WM/CSF segmentation

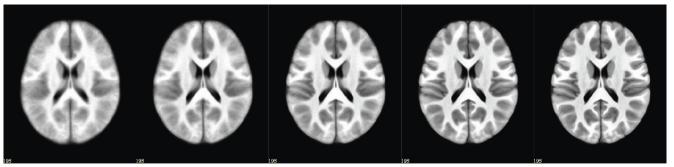


Submitted - with Adam Messinger, Caleb Sponheim, Jakob Seidlitz, Kadharbatcha Saleem,...

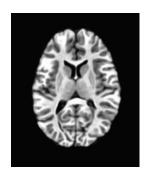
Make your own template



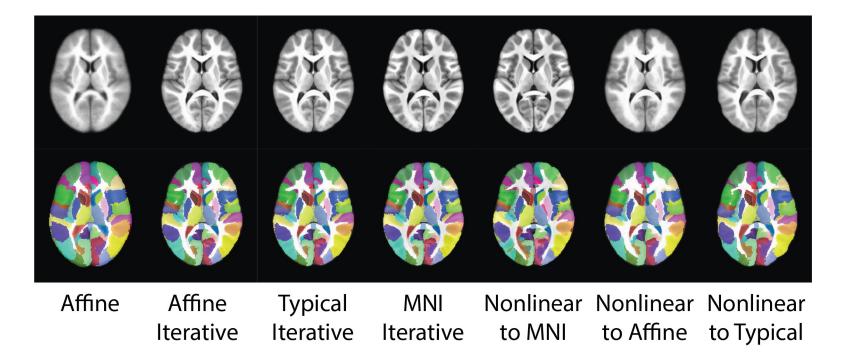
ALTERNATIVE ATLAS CREATION TECHNIQUES: ITERATIVE AND TYPICAL METHODS



Iterative nonlinear alignment to affine template with progressively smaller patch sizes



"Typical" Brain



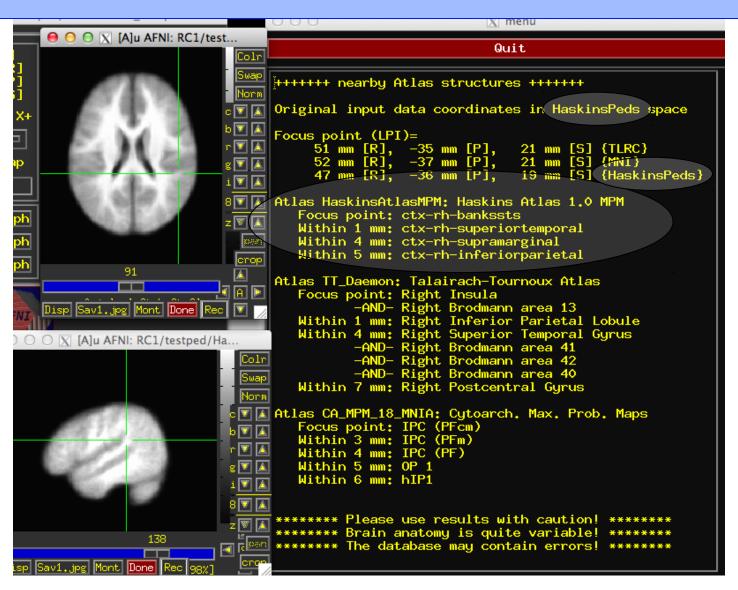
Make your own atlas!

- New atlases easy and fun. Make your own!
 - make available in AFNI GUI and whereami and to other user.

```
@AfniEnv -set AFNI_SUPP_ATLAS_DIR ~/MyCustomAtlases/
Then:
```

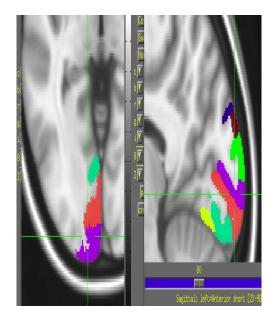
In ~/MyCustomAtlases/ you will now find atlas_for_all.nii along along with a modified CustomAtlases.niml file.

Haskins Pediatric Atlas

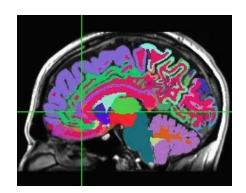


Upcoming atlases

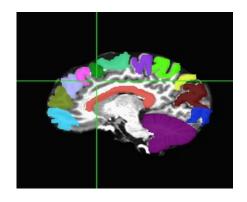
- Eickhoff-Zilles 2.2 cytoarchitectonic atlases
- DTI fiber atlas Susumo Mori
- Princeton Visual Field Map, Kastner, et al.



Individual Subjects

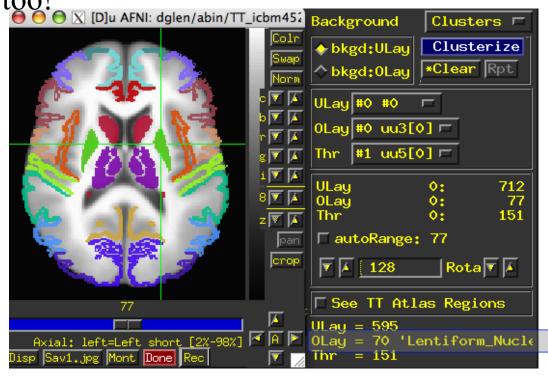


FreeSurfer segmentation



Manual segmentation

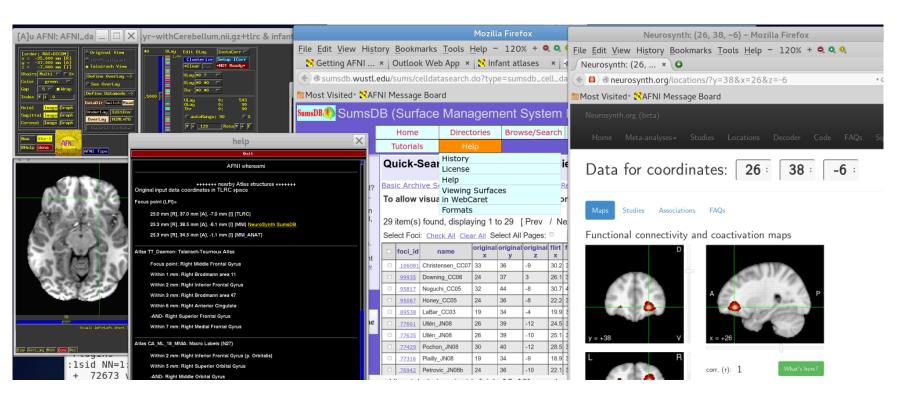




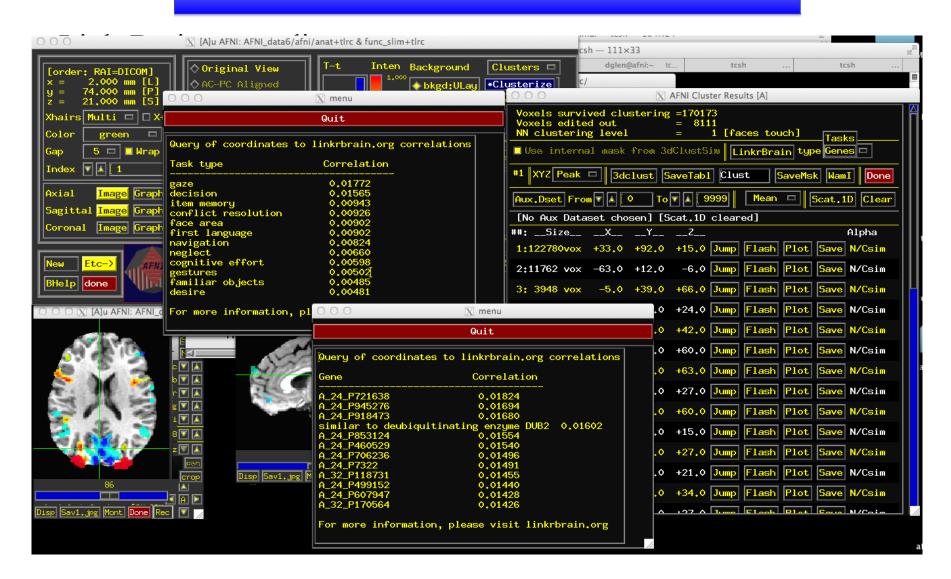
Overlay panel shows structure name. Now FreeSurfer segmentation can also be used in whereami

Web-based atlases

NeuroSynth, LinkrBrain, BrainMap.org, Allen Brain, ...



Web-based atlases



In Development

- New templates and template spaces fully supported in AFNI
 - macaque
 - rat, mouse, human
 - ♦ pediatric, ...
- On-the-fly transformations through all available template spaces
- Extra information about atlas structures
- HAWG standardized format atlases for everyone!



Atlas Conclusions and Questions



Charles Atlas