

# Efficiency of Paramagnetic relaxation enhancement in off-resonance rotating frame

H. Zhang<sup>1,2</sup>, Y. Xie<sup>1</sup>

<sup>1</sup>Center for Basic MR Research, ENH Research Institute, Evanston, IL, United States, <sup>2</sup>Radiology Department, Feinberg Medical School, Northwestern University, Chicago, IL, United States

## Introduction

We have shown recently that the relaxivity loss for Gd-based MR contrast at high magnetic field (>3T) can be regained with the paramagnetic relaxation enhancement in off-resonance rotating frame (1). However, how the enhancement efficiency is related to the molecular structure of paramagnetic agents is unclear. We have derived a complete formalism for the relaxivity of Gd-based contrast agents in the off-resonance rotating frame at high magnetic field. Presented are the theoretical simulation and experimental validation for macromolecule conjugated Gd-DTPA.

## Theory

For a macromolecule conjugated Gd-DTPA at high magnetic field where  $\omega_s \gg \omega_H \gg \omega_e$  with  $T_{1M}, T_{1\rho M} \gg \tau_m$ , the  $R_1$  and  $R_{1\rho}$  for the inner shell water can be simplified as follows,

$$R_{1,in} = Kc(3J(\omega_H)), \quad R_{1\rho,in} = Kc(2f_1(\theta)J(\omega_e) + 3f_2(\theta)J(\omega_H)) \quad [1], [2]$$

Where K is a constant, c is the concentration of gadolinium,  $f_1(\theta) = \sin^2\theta$ ,  $f_2(\theta) = \sin^4(\theta/2) + \cos^4(\theta/2)$ ,  $J(\omega) = \tau_c / (1 + (\omega\tau_c)^2)$ ,  $\theta$  is the tilt angle of off-resonance rotating frame,  $\theta = \tan^{-1}(\omega/\Delta)$ . The  $R_{1\rho}$  for the outer shell water is derived on the basis of Koenig's high field gadolinium model (2,3) as follows,

$$R_{1,out} = K'c \{ 7(1 - (\alpha B_s^2(x)/2))J_{2OS}(\omega_s, \tau_D, \tau_{s2}) + 3[(1 + \alpha)B_s^2(x)J_{1OS}(\omega_H, \tau_D, \tau_{s1 \rightarrow \infty}) + (1 - B_s^2(x))J_{1OS}(\omega_H, \tau_D, \tau_{s1})] \} \quad [3]$$

$$R_{1\rho,out} = K'c [2f_1(\theta)(1 + \alpha B_s^2(x))J_{1OS}(0)] + f_2(\theta)R_{1,out} \quad [4]$$

Where  $K'$  is a constant, c is the concentration of gadolinium,  $J_{nOS}$  are the spectral density functions,  $B_s(x)$  is Brillouin function and  $\alpha = (2S-1)/(2S+1)$ . The total relaxation rate thus equals to  $R_{1\rho} = R_{1\rho,in} + R_{1\rho,out}$ . The experimental enhancement ratio can be extracted from the equilibrium residual z-magnetization according to  $M(z)/M_0 = \cos^2\theta R_1/R_{1\rho}$ .

## Methods

The parameters used in the mathematical simulation are as follows,  $\tau_c = 38$  ps,  $\tau_{s0} = 85$  ps,  $r_{c-H} = 3.0 \text{ \AA}$ ,  $r = 3.6 \text{ \AA}$ ,  $D = 3.16 \times 10^{-5} \text{ cm}^2/\text{s}$ ,  $\tau_m = 0.244 \mu\text{s}$ ,  $\tau_R$  ranges from 80 ps for Gd-DTPA to 3000 ps, and the hydration water number  $q = 1$ . BSA-(Gd-DTPA)<sub>30</sub>, PLS-(Gd-DTPA)<sub>32</sub>, Dendrimer-(Gd-DTPA)<sub>40</sub>, Dextran-(Gd-DTPA)<sub>8</sub> were synthesized and characterized according to the methods reported elsewhere. All NMR experiments were carried with a volume coil on a 9.4 T Bruker Advance micro-imaging spectrometer. The off-resonance rotating frame magnetization profiles were obtained by applying a long pulse with a 5-60 kHz frequency offset followed by a 90° reading pulse. Residual magnetization was plotted as a function of frequency. The applied long off-resonance pulses were 500ms long with RF amplitudes of 2, 4 and 6 kHz.

## Results and discussion

Fig.1(A) shows the relaxivity as a function of  $\log(f)$  in laboratory frame, where f is proton Larmor frequency. With the typical parameters for Gd-DTPA(3), the overall correlation time  $\tau_c$  is determined by the rotational correlation time  $\tau_R$  for the Gd-DTPA unit, and the inner shell water dominates the contributions to the relaxivity enhancement at  $f < 50$  MHz. Fig.1(B) is the same relaxivity as a function of frequency at  $f > 50$  MHz, where all relaxivity enhancement disappears. Fig.1(C) is the rotating frame relaxivity as a function of frequency at the tilt angle  $\theta = 50^\circ$  (i.e.,  $\omega_1 = 6$  kHz,  $\Delta = 5$  kHz), which demonstrates that there is  $\tau_R$ -dependent relaxivity enhancement again. Fig.1(D) shows the enhancement ratio,  $R_{1\rho}/R_1$ , as a function of frequency, which increases as the square of the product  $2\pi f \tau_c$ . The value for the ratio can be as large as 10 to 30 or more, depending on f and  $\tau_c$  (or  $\tau_R$ ).

Fig.2 shows the measured enhancement ratio as a function of off-resonance frequency ( $\Delta$ ) with RF amplitude ( $B_1 = \omega_1/2\pi$ ) of 2, 4 and 6 kHz for four macromolecule conjugated Gd-DTPAs at 9.4 Tesla. The rotational correlation time for these Gd-DTPA units is known and has the order as: dextran  $\sim$  polylysine  $<$  BSA  $<$  dendrimer-g5. The measured enhancement ratio has the magnitude as dendrimer-g5  $>$  BSA  $>$  polylysine  $>$  dextran. The highest  $R_{1\rho}/R_1$  value for dendrimer-g5 is larger than 4, which corresponds to  $\tau_R \sim 1500$ . These measurements show that very high relaxation enhancement efficiency can be achieved in the off-resonance rotating by altering the dynamics of the Gd-DTPA unit.

## Conclusions

We have demonstrated that off-resonance rotating frame technique can substantially enhance the paramagnetic relaxation for  $T_1$ -type contrast agents at high magnetic field. (This work is supported by grant EB02912 from NIH).

## References

- (1) H. Zhang, L. H. Bryant, A. M. Wyrwicz, *Proc. Int. Soc. Magn. Reson.*, **7**, 340 (1999).
- (2) S. H. Koenig, K.E. Keller, *Magn. Reson. Med.*, **34**, 227 (1995).
- (3) K. E. Keller, P. M. Henrichs, M. Spiller, S. H. Koenig, *Magn. Reson. Med.*, **37**, 730 (1997).

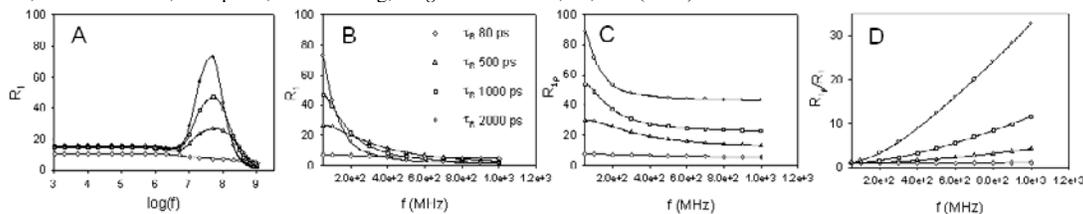


Fig.1 Simulated relaxivities and enhancement ratios.

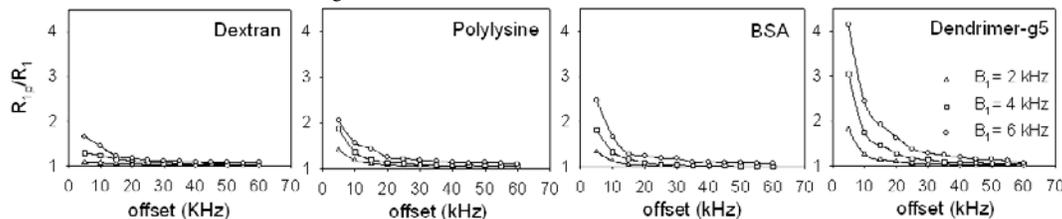


Fig.2 Measured enhancement ratios.